Non-invasive tissue oximetry

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NON-INVASIVE TISSUE OXIMETRY

CURRENT AND PROSPECTIVE APPLICATIONS

NPA VRANKEN

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Non-invasive tissue oximetry:

current and prospective applications

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Nousjka Petra Anna Vranken
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PROMOTOR

Prof. dr. J.G. Maessen

COPROMOTORES

Dr. P.W. Weerwind

Dr. S. Teerenstra

BEOORDELINGSCOMMISSIE

Prof. dr. P.M.H.J. Roekaerts (voorzitter)

Prof. dr. O. Bekers

Prof. dr. C. Boer (VU Medisch Centrum, Amsterdam)

Prof. dr. A.J.J.C. Bogers (Erasmus MC, Rotterdam)

dr. A.J.H.M. Houben

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CHAPTER 1

General introduction

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Comprehensive development of diagnostic and monitoring technologies in modern medicine has helped to better understand the complex pathophysiology of acute circulatory failure in critical cases such as surgical patients or patients admitted to the intensive care unit (ICU). In critical care settings it is vital to assess the patient's hemodynamic status for optimization of end-organ tissue oxygenation to prevent or minimize morbidity and mortality.¹

It is, however, challenging to monitor the state of tissue oxygenation accurately. The use of standard hemodynamic parameters such as blood pressure and pulse oximetry for assessing tissue blood flow is less than accurate.^{2,3} Despite apparently normal macroperfusion (capillary refill, cardiac output, blood pressure), tissue hypoperfusion can persist as a result of microcirculatory perfusion defects.⁴ Various approaches have been introduced to avoid such hypoperfusion - mostly with disappointing or controversial results. As an illustration, a recent study showed that the early goal-directed therapy strategy for septic shock not only proves no survival benefits but also might increase the risk of fluid overload.⁵ Thus, measuring heart rate, cardiac output, arterial blood pressure, and mixed venous oxygen saturation solely provides information regarding the patient's central hemodynamic status, reflecting macroperfusion, and normalization of these hemodynamic variables does not ensure sufficient oxygenation at the peripheral tissue level.⁶

The introduction of near-infrared spectroscopy (NIRS) for assessing the adequacy of regional tissue perfusion was an important landmark in the history of tissue monitoring.⁷ Since then, monitoring regional tissue oxygenation has gained wide interest, and studies began to address the importance of monitoring tissues susceptible to hypoperfusion. This has led to growing interest in non-invasive methods designed to evaluate regional perfusion as a valuable adjunct to standard global parameters to predict or diagnose tissue hypoperfusion.

How common is tissue hypoxia or tissue desaturation during the perioperative period?

Tissue hypoxia and arterial desaturation events in the perioperative period may be more common than is recognized. In a recent blinded study by Sun et al., arterial desaturation events (defined as ≥ 10 min/h with raw pulse oximetry values $< 90\%$) were reported to occur in 21% of non-cardiac surgical patients.⁸ An important finding in their study is that 90% of these hypoxemic events went undetected at the nursing floor. In a comparable patient population, Ehrenfeld et al. showed a prevalence of 6.8% for hypoxemic events (pulse oximetry values $< 90\%$, ≥ 2 minutes in duration) and 3.5% for severe hypoxemic events (pulse oximetry values $\leq 85\%$, ≥ 2 minutes in duration).⁹ In the cardiac surgical popula-

tion, hypoxic events were found to be more common, as illustrated by Ranucci et al. who observed hypoxia in 30.6% of patients (defining hypoxia as a P_{aO_2}/F_{iO_2} ratio <200 mmHg).¹⁰ In another study, Wang et al. reported even higher rates following aortic dissection (49.5%) using the same definition for hypoxia.¹¹ Interventions to correct pulse oximeter-measured oxygen saturation can avert major undesirable outcomes. In a study by Taenzer et al. pulse oximetry monitoring at a medical ward reduced serious adverse outcomes such as ICU admissions.¹² Although pulse oximetry showed clinical benefit in detection of hypoxemia and hypoxia, discordance on the relationship between pulse oximetry monitoring and complication rate remains to exist.¹³

Desaturation events may occur in the operating room or at the post-anesthesia care unit where patients are closely monitored, but frequently these episodes of a dysbalanced regional oxygen supply/demand occur during the postoperative period when patients are less strictly monitored and exposed to the respiratory depressant effects of opioid pain medications. Some of these desaturations occur in the postoperative period¹⁴ and to date it is unknown whether intraoperative or postoperative events are more important for clinical outcome.¹⁵

Physics and principles of near-infrared spectroscopy (NIRS)

The physics and mathematics of NIRS are based on a modified version of the Beer-Lambert law, which states that a proportion of light transmitted through a solution containing a colored compound (chromophore) is absorbed by the compound. As a result, the intensity of the emerging light is reduced.

The relationship between the absorption and concentration of a chromophore is described by the following Beer-Lambert equation:

$$A = \log (I_0 / I) = \varepsilon \cdot c \cdot d,$$

where A is the absorption of light, expressed as optical density (log of the ratio of the intensities of incident (I_0) and transmitted (I) light), c the chromophore concentration, ε its extinction coefficient, and d the width (optical path length) through the solution or medium.¹⁶ The Beer-Lambert law also explains the difference observed when light passes through large versus small blood vessels. If near-infrared light photons pass through a single red blood cell, only a small percentage of photons is absorbed. However, if the photons were to pass through a blood vessel of 1 mm thickness, absorbance would be 0.8 and thus only 10% of the impacting photons would remain unabsorbed.¹⁷

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Tissue oxygenation is the result of a complex interaction of perfusion, arterial oxygen tension, hemoglobin (Hb) level and dissociation conditions, and local oxygen consumption. Consequently, each oxygen-monitoring method involves specific assumptions and limitations. Tissue oximetry with near-infrared light is a non-invasive, optical technique that integrates blood oxygenated hemoglobin (HbO₂) saturation in an anatomical region of interest (Figure 1).

Figure 1. Near-infrared spectra of oxygenated hemoglobin (HbO₂) and hemoglobin (Hb).¹⁸

By nature of the technique, measurement is limited to the intravascular compartment. It combines measurements of arterial, venous, and capillary blood, depending on the absorbance of different wavelengths of near-infrared light. Unlike pulse oximetry, NIRS does not involve detection of a pulsatile tissue component but relies entirely on the Beer-Lambert law that relates the concentration of a substance to its light absorption.¹⁹ The ability to discriminate various types of chromophores varies with the number of wavelengths; for example, a NIRS device using two distinct wavelengths cannot discriminate between the levels of oxyhemoglobin, reduced Hb, oxymyoglobin, and reduced myoglobin.²⁰ This can be a significant issue when, for example, comparing the readings of an NIRS device on the forehead and thenar muscles, with obvious differences in the amount of myoglobin present in the two tissues. For cerebral NIRS devices, the assumption is that myoglobin is only a minor contributor to the signal and that the vascular Hb-oxygen component predominates.²¹ Cerebral oximeters are calibrated by the manufacturer assuming a constant 70% or 75% weighting toward venous blood saturation.^{22,23} Oxygen consumption with insufficient oxygen delivery will lead to an increased concentration of reduced Hb, and since

Hb chromophores dominate the near-infrared absorption spectrum, the estimation of Hb-oxygen saturation is arguably less susceptible to errors and signal-to-noise problems than NIRS-based assessment of cytochrome redox status. An *in vivo* calibration can be accomplished with direct measurement of cerebral venous and arterial saturation in blood samples.²³ This calibration, incorporated into the calculation algorithm that determines the displayed value of regional oxygen saturation (rSO₂), should theoretically reduce the interfering effects of different Hb concentrations and variations in tissue light transmission. However, this calibration approach assumes that all individuals have the same constant ratio of cerebral venous to arterial blood within the tissue where the measurement is performed. Given the great inter- and intrapersonal variations in hemodynamics and anatomy, this assumption is likely incorrect.

NIRS accuracy for measuring brain tissue oxyhemoglobin saturation

Today, physicians can choose from a wide variety of devices for monitoring rSO₂, including INVOSTM (Medtronic, Minneapolis, MN, USA), FORE-SIGHTTM (CAS Medical Systems, Branford, CT, USA), EQUANOXTM (Nonin Medical Inc., Plymouth, MN, USA), CerOxTM (Ornim Medical, Lod, Israel), NIROTM (Hamamatsu Photonics, Hamamatsu City, Japan), and TOS-96TM (Tostec Co., LTD., Tokyo, Japan).

Although spatially resolved spectroscopy can be used to compute a scaled concentration of tissue Hb and relative concentrations of oxy- and deoxyhemoglobin, currently manufactured cerebral oximeters are not designed to provide an “absolute” measurement of regional tissue oxygen saturation.²³ A study evaluating the accuracy of cerebral oximeters by Bickler et al.²³ revealed the between-subject variability and dynamic error of readings that constitute to a challenge in determining absolute thresholds for predicting tissue injury. Furthermore, the measured ratio of venous to arterial blood in brain tissue is variable and about 50:50²⁴, whereas oximeter manufacturers calibrate to fixed venous to arterial volume ratios of 70:30 or 75:25.²³ Moreover, changes in cerebral venous and arterial blood volumes, carbon dioxide or oxygen concentrations will violate assumptions on constancy of arterial to venous blood volume.²⁴ Signal contamination originating from blood in extracranial tissue within the sampled volume of interest also complicates the clinical utility of this technology.²⁵ Administration of peripherally acting vasoconstrictors (e.g. phenylephrine or norepinephrine) is one example that can affect the contribution of extracranial blood and possibly alter tissue oximetry readings.²⁴ In addition, sympathetically-mediated vasoconstriction from pain, hypothermia, and hypovolemia significantly alters peripheral

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tissue oxygenation and may also influence the extracranial component of the reading. Therefore, the measurements are at best relative assessments of tissue oxygenation and are useful as trend monitors, not threshold of injury monitors.

How widespread is the use of tissue oximetry?

Given the diversity of technologies currently available to assess tissue oxygenation status, it is important to consider its various applications in current clinical practices using NIRS.

Brain monitoring

The brain is the organ most commonly directly assessed with regional tissue oximetry using NIRS. Although monitoring cerebral oxygenation to prevent the adverse consequences of acute cerebral hypoperfusion is supportable with current knowledge, the issue of predicting longterm outcomes remains less clear.²⁷ During cardiac surgery with cardiopulmonary bypass (CPB), (undetected) episodes of hypoperfusion predispose the patient to an increased risk of postoperative neurological complications (PNC). Despite this, routine evaluation of cerebral hemodynamics is still not part of standard clinical practice. Non-invasive tissue oximetry has been advocated to minimize and even prevent vulnerable episodes characterized by a disbalance between regional oxygen supply and demand. In one study, Murkin proposed that cerebral oximetry can be used as an organ index, meaning that maintaining adequate rSO_2 levels is beneficial for all vital organs.¹⁹ The technique has been widely applied in clinical centers and multiple studies have been conducted, suggesting that intraoperative optimization of cerebral oximetry-derived values aids in preventing PNC.¹⁹ This contributed to the conclusions drawn in systematic reviews that tissue oximetry is a promising technique for preventing PNC following surgical procedures.²⁸ The evidence linking rSO_2 values and PNC remains doubtful due to the lack of intervention-guided studies that focus on the causality of the proposed relation between rSO_2 and adverse clinical outcome.²⁷ Moreover, studies also failed to prove that intraoperative interventions to correct cerebral rSO_2 lead to improved neurological outcome.²⁷ Part of the explanation can be found in the fact that due to its measurement principle, cerebral oximetry does not take cerebral autoregulatory activity into account. Cerebral autoregulation (CA) is the intrinsic system that maintains adequate cerebral blood flow at a wide range of different perfusion pressures. One example can be found in cerebral hyperperfusion, also referred to as brain luxury perfusion.²⁹ In this case, cerebral oximetry readings can be close to baseline values while the CA is severely dis-

turbed, thereby predisposing the patient to increased risk of cerebral edema and hemorrhage. In order to preserve CA, arterial blood pressure among other factors need to be strictly controlled within certain limits. Together with avoiding large fluctuations in hemodynamic parameters, this may contribute to minimize PNC occurrence in patients undergoing CPB.

Somatic tissue monitoring

Besides brain monitoring, tissue oximetry has also been used in various other clinical applications. Continuous assessment of oxygenation in peripheral tissue or free skin flaps may contribute to early detection of circulatory compromise, as indicated by previous work.³⁰⁻³² Despite this, tissue oximetry is not an integrated part of routine monitoring in surgical or ICU patients susceptible to ischemic tissue damage.

Aims and outline of this thesis

Since the introduction of non-invasive tissue oximetry as a continuous monitor for tissue perfusion, implementation into routine clinical practice has been an ongoing process. For the most part this is due to uncertainties regarding adequate interpretation of rSO_2 values and trends. This thesis focuses on current and prospective applications of non-invasive tissue oxygenation monitoring using NIRS, with the intent to describe the current state of knowledge on non-invasive tissue oximetry and clinical outcome parameters, and to identify the gaps in knowledge and technology that would help to resolve the remaining unknowns.

First, the clinical application of non-invasive tissue oximetry in brain monitoring during CPB is described and discussed in chapter 2. The current evidence of a link between cerebral rSO_2 readings and the occurrence of PNC following cardiac surgery with CPB is systematically reviewed. In addition, elucidation is provided on the role and importance of intact CA as part of brain protection during bypass.

Adequate prevention of ischemic complications contributing to PNC requires knowledge of the modifiable factors that determine the extent of CA functionality in patients during CPB. Among these modifiable factors, hemodynamic stability, arterial carbon dioxide level and hemodilution appeared to play a substantial role in CA efficacy (chapters 3 and 4).

During cardiac surgery with CPB, several actions performed by the cardiothoracic surgeon, clinical perfusionist and anesthesiologist affect oxygen supply to the brain. Non-invasive tissue oximetry could aid in early detection of decreas-

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ing cerebral oxygenation in case of e.g., iatrogenic events, preventing possibly harmful ischemic episodes. It is therefore important to evaluate whether cerebral rSO_2 readings are responsive to certain iatrogenic events and if so, the magnitude of the induced change (chapter 5).

Besides its application in CPB during cardiac surgical procedures, patients admitted to the ICU in need of prolonged cardiopulmonary support may also benefit from tissue oximetry measurements (chapter 6). In the case of femoral access, specifically, concerns regarding variations in oxygenation associated with compromised brain and limb perfusion remain to exist. Continuous monitoring of peripheral tissue as well as brain rSO_2 may contribute in preventing complications. Tissue oximetry may possibly be superior to existing monitoring methods due to the absence of a clear time delay in the representation of impaired tissue perfusion.

In addition to steady-state tissue oxygen saturation monitoring, dynamic assessment of tissue oxygenation may provide valuable information regarding peripheral vascular reactivity (chapter 7). Identification of microvascular dysfunction is of clinical importance due to its relationship with consequential tissue malperfusion. Adequate assessment of vascular reactivity can avert ischemic tissue damage by enabling intervention at the stage where only microvascular dysfunction is apparent, prior to the occurrence of hypoxia.

Another application of tissue oximetry in peripheral tissue monitoring is assessing free flap viability following autologous reconstructive surgery (chapter 8). In the first critical hours following free flap transplantation, the risk of arterial or venous thrombosis is highest and constitutes to risk of partial or complete flap loss as a result of liquefactive fat necrosis. Therefore, extensive and continuous monitoring is warranted to allow timely intervention.

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CHAPTER 2

Cerebral oximetry and autoregulation during cardiopulmonary bypass: a review

NPA Vranken, PW Weerwind, NA Sutedja, EE Ševerdija, PJC Barenbrug, JG Maessen

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CHAPTER 2

Abstract

Postoperative neurological complications (PNCs) following cardiac surgery with cardiopulmonary bypass (CPB) is a detrimental complication, contributing to increased mortality rates and health care costs. To prevent intraoperative cerebral desaturations associated with PNC, continuous brain monitoring using near-infrared spectroscopy has been advocated. However, clear evidence for a defined desaturation threshold requiring intervention during CPB is still lacking. Since cerebral oximetry readings are nonspecific, cerebral tissue oxygenation values need to be interpreted with caution and in the context of all available clinical information. Therefore, maintaining an intact autoregulatory activity during CPB rather than solely focusing on regional cerebral oxygen saturation measurements will collectively contribute to optimization of patient care during CPB.

Introduction

The advancement of extracorporeal circulation techniques in recent decades has played an essential role in minimizing complications following cardiac surgery with cardiopulmonary bypass (CPB).¹ The technical advancements have been, however, partially offset by changes in the patient population. These changes involve a more complex disease at advanced age and significant comorbidities²⁻⁴, resulting in convoluted and lengthier procedures. Moreover, in older patients, the atherosclerotic disease process is farther advanced, which may nourish an increased risk for postoperative complications including perioperative stroke and neurocognitive impairment, including delirium.^{1,4,5} From these, stroke has been reported to be the most detrimental with rates varying from 1.5 to 11%.⁶⁻¹⁰ Furthermore, these postoperative neurological complications (PNC) contribute to prolonged hospital stay, increased mortality rates and health care costs, constituting to an increased burden for health care providers.^{11,12}

The mechanism of cerebral injury following cardiac surgery with CPB is not yet clearly understood. Development of PNC possibly involves embolization or hypoperfusion causing cerebral ischemia.^{5,11,13,14} To prevent intraoperative cerebral desaturations associated with ischemic complications of the brain, continuous brain monitoring using near-infrared spectroscopy (NIRS) has been advocated.^{15,16} Although multiple studies proposed cerebral oximetry as a viable monitoring method to prevent these neurologic complications, clear threshold determinants for acute intervention are still lacking.^{14,17}

Furthermore, there seems to be a link between disturbed intraoperative cerebral autoregulation (CA) and PNC.¹⁸⁻²¹ The neuroprotective autoregulatory system prevents both hypo- and hyperperfusion by reactive vasodilation and constriction following changes in arterial blood pressure (ABP) and arterial partial pressure for carbon dioxide ($P_a\text{CO}_2$), also referred to as modifiable factors.¹³ These factors are mostly based on maintaining a mean ABP of 50-60 mmHg²² and $P_a\text{CO}_2$ is only measured intermittently during CPB. Obviously, there is a lack of optimal control for CA functionality.

Clinical application of cerebral oximetry, its limitations and association with PNC as well as the role of modifiable factors influencing the neuroprotective autoregulatory system during CPB are subsequently reviewed.

Cerebral tissue oximetry

Cerebral oximetry allows clinicians to monitor regional cerebral tissue oxygen saturation (rSO_2) real-time in a non-invasive manner. Cerebral rSO_2 is depend-

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ent on several physiological variables that affect oxygen supply and consumption of the brain, including cardiac output, inspired oxygen concentration, pulmonary function, cerebral metabolism, temperature, and hemoglobin concentration.^{23,24} Cerebral oximetry readings are proposed to reflect the balance between regional oxygen supply and demand and thereby local cerebral metabolism.^{11,25-27} More specifically, a decreasing cerebral rSO_2 due to regional or global ischemia can be explained as an oxygen supply insufficient to meet the metabolic demand caused by, e.g., a decreased cardiac output.^{26,28} Unlike mixed venous oxygen saturation that is measured continuously via a pulmonary artery catheter, cerebral oximetry has shown to reflect alterations in blood pressure real-time.²⁹ This suggests that cerebral oximetry enables prompt assessment of tissue oxygenation, serving as a potential early indicator of neurologic injury.

The technique applied in cerebral oximetry uses NIRS based on the Beer-Lambert law.^{14,30} The elementary particles of near-infrared light are photons that penetrate tissue before reaching the underlying capillary network. Near-infrared light of different wavelengths within the so-called biological spectroscopic window is emitted to penetrate the skin, skull, and dura matter to reach the frontal lobe of either the left or right cerebral hemisphere.¹¹ The photons emitted through a NIRS sensor travel via a banana-shaped pathway before being measured by photodiode detectors positioned at a fixed distance from the light emitter when they resurface. Within tissue, the light is partly reflected, scattered, and absorbed. To minimize residual error, two measurements with different emitter-diode spacings are performed simultaneously, resulting in a shallow-deep detector difference. With the light intensity held constant, the quantity of light absorbed by chromophores varies with the ratio of oxygenated hemoglobin relative to the total concentration of hemoglobin, which is used to estimate local oxygen content.^{14,17} Most clinical devices use one near-infrared light emitter in combination with two near-infrared light detectors, whereas other devices use several detectors per emitter. The latter may contribute to the accuracy of cerebral rSO_2 estimation; however, the measurement principle remains the same. In addition, the algorithm for estimating the oxygen content in cerebral blood requires an assumption on the ratio venous to arterial blood volume, which differs between clinical oximeter devices. The Food and Drug Administration approved four monitoring devices for clinical use in the United States, which include the Fore-sight cerebral oximeter (Cas Medical Systems, Inc., Branford, CT, USA), Equanox (Nonin Medical Inc., Plymouth, MN, USA), INVOS 5100C (Medtronic, Minnesota, MN, USA), and the CerOx (Ornim Medical, Lod, Israel). Both Fore-sight and Equanox use the ratio of 70% venous blood to 30% arterial blood, whereas INVOS 5100C and CerOx use a ratio of 75% venous to 25% arterial

blood.^{29,31} Additionally, cerebral oximeters may provide one or several types of measurement, estimating absolute rSO_2 values (Fore-sight and Equanox), or values intended for trend monitoring (INVOS 5100C and CerOx).

Corresponding to the cerebral oximetry measurement principle, rSO_2 values can only partially reflect oxygen saturation in the anterior circulation of the prefrontal cortex, thereby limiting its monitoring ability to an area of approximately

1 cm³.^{23,29,32} Also extracerebral tissues including skin, bone, and connective tissue may contaminate the estimation of rSO_2 .³³ In addition, tissue oximetry derived values are nonspecific, meaning that a decreasing rSO_2 may be the result of hypoperfusion, relative hypoxemia, and/or an increased metabolic rate.¹⁴ Hence, when interpreting changes in cerebral rSO_2 it is necessary to consider all available clinical information.²³

The algorithm to estimate cerebral rSO_2 takes the predominant venous part of the cerebral blood volume into account that is reflected by a strong correlation between rSO_2 and jugular venous oxygen saturation, an early indicator of brain ischemia.^{34,35} Other studies, however, reported that rSO_2 is unable to reflect changes in jugular venous bulb oximetry in the case of head injury.^{36,37} Nevertheless, a recent observational study has shown that cerebral oximetry is sensitive enough to effectively identify changes in rSO_2 following iatrogenic events including anesthetic induction, aortic cross clamping, and onset and termination of bypass.³⁸ In addition, cerebral oximetry has shown to effectively depict the concomitant decline in cerebral oxygen saturation during cannula malposition³⁹⁻⁴¹, a failing oxygen line to the oxygenator in the CPB circuit⁴² and acute innominate artery dissection.⁴³ These findings indicate that cerebral oximetry may aid in early detection of potential adverse neurologic events and contribute toward preventing PNC by enabling alteration of current patient management.

Although absolute (fixed value for rSO_2) and relative (percentage of baseline rSO_2) desaturation thresholds have been previously applied^{44,45}, to date no consensus has been reached on the use of either an absolute or personalized cut-off value requiring prompt intervention.^{17,46} Nonetheless, it is generally accepted that both the extent and duration of cerebral desaturation are important.^{14,46}

Furthermore, this lack of standardization may be related to the different monitoring devices which use varying numbers and wavelengths of light emitted as well as sensor-emitter spacings, affecting both the measurement itself and the rSO_2 calculation.^{3,30} Differences in applied algorithm between the devices further challenge cerebral oximetry standardization. Moreover, the algorithm itself cannot accommodate for inter-individual differences including variations in cranial anatomy (e.g., asymmetrical brain circulation²³, different percentages of venous cerebral blood circulating in the frontal lobe⁴⁷ and the influence of non-modifiable patient characteristics on baseline rSO_2 readings).²⁵ The algorithm requires the assumption of a constant optical path length that is actually de-

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creased during CPB due to hemodilution, altering the absorbance of near-infrared light by chromophores. This may introduce an error in the estimation of the local oxygen content.³⁰ In summary, focusing on an rSO₂ threshold as suggested by Douds et al.⁴⁸ would be a provocative step towards the use of cerebral oximetry as a preemptive marker for perioperative morbidity to optimize postoperative recovery.

Cerebral tissue oximetry and PNCs

Since the widespread clinical application of tissue oximetry, several studies investigated the relationship between cerebral oximetry readings and PNC. The current evidence on the relationship between cerebral desaturations as identified by cerebral oximetry and PNC following cardiac surgery with CPB is systematically reviewed in this section.

To identify relevant publications, PubMed and MEDline databases were searched for articles originating from January 2006 to August 2016. Two researchers searched and screened articles on title, abstract, and full text independently. Additional studies were identified by screening the references in the retrieved papers to capture articles that might have been missed.

The articles included were studies that focused on the relationship between cerebral oximetry readings and cognitive decline following cardiac surgery with CPB in adults. The search was limited to publications in English. Studies that were not published as a full-length article or did not discuss PNC outcome in relation to cerebral oximetry readings were excluded. Free search terms were divided in two main groups, the first representing cerebral oximetry and the second representing cardiac surgery with CPB. The cerebral oximetry category included the search terms “near infrared spectroscopy”, “infrared spectroscopy”, “NIRS”, “cerebral oximetry” and “cerebral oxygen saturation” while the cardiac surgery with CPB category included the search terms “cardiac surgery”, “CPB”, “coronary artery bypass grafting” (CABG), “CABG”, and “coronary bypass graft”. For each search, one of the aforementioned search terms from both groups was combined.

Results

The initial search focusing on cerebral oximetry resulted in 507 publications using all combinations of free search terms. Review of the title and abstract led to inclusion of 21 out of 507 articles. A total of 13 observational and 7 interventional studies were identified as depicted in Table 1.

Several studies found a relationship between cerebral desaturations and neurological complications, including a study by Colak et al. who showed an increased occurrence of stroke in patients with cerebral desaturations, defined by both absolute (area under the curve of >50 minutes·% under 50% absolute rSO_2) and relative (area under the curve >150 minutes·% under 20% of baseline rSO_2) thresholds.⁴⁵ Similarly, Slater et al. and de Tournay-Jetté et al. found a significant relationship with early postoperative neurocognitive decline when the absolute desaturation threshold of 50% rSO_2 was exceeded.^{50,63} In patients undergoing aortic arch surgery, Fischer et al. noted more conservative absolute desaturation thresholds of 65% and 60% to indicate an increased risk of adverse outcome.⁵¹ Contrastingly, Kok et al. in a pilot study failed to show a relationship between cerebral desaturation and PNC.⁶⁴

Moving forward to interventional-guided studies, Slater et al. through a prospective randomized interventional trial found a positive relation between cerebral desaturations and PNC using the mini-mental state examination (MMSE).⁶³ In another prospective randomized interventional trial, Murkin et al. studied cerebral desaturations and postoperative morbidity in cardiac surgical patients undergoing CPB.⁶² More patients in the control group ($n=96$), (i.e., no intervention based on normalization of intraoperative rSO_2 within 75% of baseline) underwent prolonged cerebral desaturation episodes compared to the intervention group ($n=98$). Stroke rate, however, did not significantly differ between groups. The authors attributed this finding to the fact that their study lacked adequate statistical power for assessment of stroke ($n=4$ in the control group, versus $n=1$ in the intervention group), as the a priori power analysis was based on major organ morbidity and mortality. Nevertheless, they conclude that intraoperative monitoring and management using cerebral oximetry may have a clinical benefit for the cardiac surgical patient.

Table 1. Overview of the studies included in the systematic literature search.

author	year	type of study	device used	n	rSO ₂ -PNC relation	rSO ₂ threshold	outcome measured	measuring complications
Negargar ⁴⁹	2007	PO	INVOS	72	no	absolute decrease <40% and 50%, >20% absolute desaturation from baseline	neuropsychological state	MMSE
De Tournay-Jette ⁵⁰	2011	PO	INVOS	61	yes	absolute decrease <50%, >30% decrease from baseline	early (4-7 days) and late (1 month) POCD (drop of 1SD from baseline (the day before surgery) on ≥ 2 more neuropsychologic indices)	Trail Making Test part A and B, Verbal Fluency Test, Ray's Auditory Verbal Learning Test, Logical Memory Subtest (Rivermead battery), digit symbol, Stroop Test
Fischer ⁵¹	2011	PO	Fore-sight	30	yes	absolute decrease <50%, <55%, <60%, <65%	severe adverse outcome, including stroke	not specified
Schoen ⁵²	2011	PO	INVOS	231	yes	absolute decrease <50% absolute, >80% decrease	delirium	MMSE, CAM-ICU
Hong ⁵³	2008	PO	INVOS	100	no	absolute decrease <40%, 50%, >20% decrease from baseline	POCD	MMSE, Trail-Making Test (Part A), Grooved Pegboard Test
Fudickar ⁵⁴	2011	PO	Niro	35	yes	absolute decrease <65%	postoperative cognitive deficit	Trail Making Test, Verbal Learning Test, Ray's Auditorial Verbal Fluency Test, Digit Symbol Substitution Test, Digit Span Test
Olsson ⁵⁵	2006	RO	INVOS	46	yes	none	stroke	new neurologic deficit that did not resolve before discharge confirmed by CT and/or specialist neurologic assessment

author	year	type of study	device used	n	relation rSO ₂ -PNC	rSO ₂ threshold	outcome measured	measuring complications
Urbanski ⁵⁶	2013	PO	Niro	122	no	absolute decrease ≤55%, <80% change from baseline	adverse neurological outcome (permanent focal neurological deficit or temporary neurological dysfunction)	permanent focal neurological deficit: confirmed by a neurologist and CT or MRI. Temporary neurological dysfunction: confusion, delirium, agitation or temporary focal deficits without evidence on CT or MRI.
Kakihana ⁵⁷ Hassan ⁵⁸	2012 2010	PO POP	Hamamatsu Fore-sight	10 1	yes yes	none absolute decrease <55%	stroke neurocognitive deficit	MMSE not reported
Greenberg ⁵⁹	2013	PO	Fore-sight	53	no	absolute decrease <60% ≥60 seconds in ≥1 hemisphere	delirium	not reported
Senanayake ⁶⁰	2012	PO	INVOS	27	yes	none	permanent or temporary neurological deficit	Permanent neurological deficit: any new postoperative neurological deficit that included new focal stroke or global coma which did not resolve by discharge, and confirmed by a new cerebral infraction on CT. Temporary neurological deficit: any postoperative neurological deficit that included motor deficit, confusion, agitation, or transient delirium that resolved spontaneously before discharge with no new cerebral infarction on CT.
Kamenskaya ⁶¹	2015	PO	INVOS	61	yes	absolute decrease <40%	neurological complications (encephalopathy, stroke)	MMSE, GCS
Murkin ⁶²	2007	PRI	INVOS	194	no	AUC<70% of baseline >150 min-%, desaturation AUC <40% absolute	stroke	focal neurologic deficit persisting >24hrs and confirmed by CT

author	year	type of study	device used	n	relation rSO ₂ -PNC	rSO ₂ threshold	outcome measured	measuring complications
Colak ⁴⁵	2015	PI	INVOS	200	yes	absolute decrease <50%, AUC >150%·min <20% of baseline, AUC >50min·%	cognitive decline	MMSE, Color Trail Test 1, Grooved-Pegboard Test
Slater ⁶³	2009	PI	INVOS	240	yes	desaturation score >3000	early POCD	neurocognitive test battery
Kok ⁶⁴	2014	PIP	INVOS (but both INVOS and Foresight were measured)	60	no	AUC 40% >10 min·%	postoperative cognitive decline (4 days (early) and 3 months (late))	CogState brief computerised cognitive test battery
Mohandas ⁶⁵	2013	PI	Equanox	100	yes	>20% decrease from baseline	PNC	MMSE, ASEM
Colak ⁶⁶	2012	PI	INVOS	58	yes	AUC>150 min·% for <20% of baseline or >50 min·% for <50% of absolute value	stroke, coma, stupor	Coma: profound state of unconsciousness without response to verbal call, pain or any other stimulus. Stupor: state of unconsciousness from which patient can be aroused only by vigorous physical stimulation. Stroke: acute onset of a neurologic deficit that persists for at least 24 hours and reflects focal involvement of the central nervous system. Delirium/encephalopathy: confusion, agitation, disorientation, decreased alertness, sleep disturbances, memory deficit or seizure without obvious focal neurological deficit.

author	year	type of study	device used	n	relation rSO ₂ -PNC	rSO ₂ threshold	outcome measured	measuring complications
Murkin ⁶⁷	2011	PI	INVOS	57	no	rSO ₂ decrease <75% of baseline >15 seconds.	new-onset stroke, major-organ morbidity and mortality	unclear

ASEM: antisaccadic eye movement, AUC: area under curve, CAM-ICU: confusion assessment method on the intensive care unit, CT: computed tomography, GCS: Glasgow coma scale, MMSE: mini mental state examination, MRI: magnetic resonance imaging, PI: prospective interventional, PIP: prospective interventional pilot, PNC: postoperative neurological complications, PO: prospective observational, POCD: postoperative cognitive dysfunction, POP: prospective observational pilot, PRI: prospective randomized interventional, RO: retrospective observational, rSO₂: regional cerebral tissue oxygen saturation.

Interpretation

Several studies suggest that cerebral oximetry is a valuable monitoring tool and implicate that early intervention based on cerebral oximetry monitoring can potentially prevent or decrease the occurrence of PNC. Murkin even proposed that cerebral oximetry can be applied as an index organ, indicating that maintaining adequate cerebral rSO₂ values is beneficial for all vital organs.¹⁵ Despite these findings it remains unclear if this is part of a causal relationship or just a reflection of overall morbidity.¹⁴

In a recent systematic review, data on the specificity of rSO₂ monitoring to ensure cerebral perfusion could not be established, i.e., the absence of acute reductions in rSO₂ did not ensure adequate cerebral blood flow (CBF).¹⁷ Furthermore, Kok et al. reported no relationship between cerebral desaturations and PNC, which can be explained by the fact that low rSO₂ occurred only sporadically in their patient population.⁶⁴ This suggests that factors other than intraoperative hypoxic episodes contribute to the development of PNC. Moreover, the incidence of PNC following cardiovascular procedures is relatively low, which affects the ability of studies to demonstrate a significant association with cerebral desaturations.^{3,4,68} A plausible explanation for the low PNC occurrence can be found in the applied perfusion protocol, which includes maintaining the mean ABP within a certain range (70-90 mmHg), maintaining normoxia (partial arterial oxygen pressure between 11.0-14.0 kPa or 83-105 mmHg) and normocapnia (P_aCO₂ 4.5-5.5 kPa or 34-41 mmHg), with a hematocrit level >28% throughout the intraoperative period.⁶⁹ Further, it has been shown that avoiding large fluctuations in hemodynamic parameters during CPB decreases the risk of postoperative neurologic complications.⁷⁰

Besides perfusion protocols, additional factors that likely alter the risk of PNC occurrence include patient and surgery-related parameters. Previous studies identified the factors advanced age, a history of neurologic events, insulin-dependent diabetes mellitus, congestive heart failure, peripheral vascular disease, prolonged CPB time, and a more complex surgical procedure to be linked to PNC occurrence.^{6-9,17,20,45,68,71-74} In contrast, Fink et al. in a recent review state that the evidence linking cardiovascular procedures to cognitive outcome is scarce, and persistent postoperative cognitive impairment may solely reflect the presence of cognitive impairment prior to surgery.³

Moreover, the lack of standardization in the diagnosis of PNCs makes comparison between studies focusing on its determinants challenging. In the current literature, different cognitive assessment methods are applied to identify cognitive decline, of which the MMSE is most frequently used.¹² These tests require measurements to be performed at different time points prior to and following surgical intervention. For diagnosis of stroke additional computed tomography

scanning or magnetic resonance imaging is required.⁷⁵ Furthermore, the MMSE does not account for frontal lobe abnormalities, which is the typical area for cerebral rSO₂ measurement⁷⁶, possibly causing a false-negative test result. In summary, there is a lack of intervention-guided trials linking disturbances in cerebral oxygen saturation to occurrence of PNC. It is therefore doubtful whether regional rSO₂ can be used as a specific brain monitor.

Cerebral autoregulation

Besides intraoperative cerebral desaturations, disturbances in the neuroprotective cerebral autoregulatory system are known to result in adverse neurological outcome.^{18,77,78} The definition of CA is the intrinsic ability of the cerebral vasculature to provide a constant CBF despite changes in cerebral perfusion pressure.⁷⁹ In case of an intact CA, the cerebral perfusion pressure is coupled with the cerebral metabolic demands, preventing both ischemia and hyperemia.⁷⁷ The central homeostatic system of CA provides neuroprotection against hypo-, hyperperfusion, and ischemia through vasodilation and vasoconstriction of the cerebral vasculature. Proportionate alterations in CBF and subsequent maintenance of brain metabolism ensure adequate oxygen saturation and removal of carbon dioxide and other metabolites. The cerebral vasculature receives its postganglionic sympathetic innervation from the superior cervical ganglion containing neuropeptide Y and norepinephrine. This vascular response is dependent on vessel size and mostly initiated by the pial arteries extending from the circle of Willis.⁸⁰ In case of a sudden increase in blood pressure, the cerebral autoregulatory response prevents cerebral hyperemia and disruption of the blood-brain barrier.⁸¹ This is reflected by the fact that when the CA fails, worsened clinical outcome can be expected, including an increased risk of PNC.⁸² According to previous studies, cerebral oximetry reflects CA by close association with a determinant of autoregulation, i.e., the cross-correlation between middle cerebral artery blood flow velocity and mean ABP.^{83,84} Likewise, the positive association of a change in rSO₂ with a change in ABP is thought to reflect the absence of CA, also referred to as pressure passive cerebral perfusion.^{85,86} On the other hand, in the case of hyperperfusion (also referred to as luxury brain perfusion⁸⁷, cerebral rSO₂ values can be close to baseline while the CA is severely disturbed. This can be explained by the fact that the cross-correlation between middle cerebral artery blood flow velocity and mean ABP is merely an intermediate indicator of CA, as the phase relationship in the autoregulatory response is not taken into account.⁸⁸ For assessing cerebral autoregulatory activity, either its efficiency or its efficiency combined with the time necessary for cerebrovascular resistance to adapt

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can be determined. These two methods are also referred to as steady-state CA or static CA and dynamic CA, respectively.⁸⁹ In both static and dynamic assessment of CA, ABP as well as CBF velocity (CBFV) need to be taken into account. Mostly transcranial Doppler is used for quantification of CBFV, utilizing high-frequency sound waves to penetrate the acoustic temporal window of the cranium. One commonly used method validated for determining the current state of CA using transcranial Doppler is transfer function analysis that estimates phase shift, coherence, and gain. The phase shift is the time difference observed between ABP (input) signal and the CBFV (output) signal, whereas coherence reflects the strength of the the magnitude of the transfer function between CBFV and ABP.⁹⁰ The result of the transfer function analysis is an autoregulation index ranging from 0 (absence of autoregulatory activity) to 9 (strongest autoregulatory activity).⁹¹ In patients, fluctuations in ABP and thereby CBFV need to be initiated to provoke adaptation in cerebrovascular resistance. In awake subjects, this can be achieved through metronome-triggered breathing while during CPB the indexed pump flow can be varied in a cyclic manner.⁶⁹ Although the association between cerebral desaturations and PNC remains inconclusive, the link between disturbances in the intrinsic autoregulatory system and PNC occurrence is well recognized.^{18,21,77,82,92-94} Despite this fact, disturbances in the CA are reported to occur relatively frequently, in 20% of patients undergoing CPB.¹⁸ The primary requisite to maintain an intact CA is targeting a mean ABP within a certain range, i.e., the lower and upper autoregulatory limits. A range of 60-150 mmHg has been recommended to attain intact CA, although these pressures can be affected by sympathetic nervous activity⁹⁵, which is the case in chronic hypertension.⁸¹ Also, the lower limit of CA has a wide inter-individual range, and thereby poses a challenge to predict an intact CA based on preoperative measurements.⁸⁴ Within the autoregulatory range, CBF velocity appears unaffected by CPB pump flow.⁹⁶ However, when ABP falls below the lower limit of CA, cerebral hypoperfusion and ischemia can result, as the cerebral vasculature cannot compensate any further for the reduction in perfusion pressure.⁹⁷ Low CBF increases the risk of ischemic brain lesions leading to functional neuronal impairment or possibly even permanent neuronal injury.⁷⁷ This has been confirmed by multiple studies reporting a positive relationship between a lowered mean ABP and the occurrence of adverse neurologic events.^{18,92,94} More specifically, a >15 mmHg reduction in ABP caused a 10% cerebral desaturation.⁹⁸ In addition, a lowered perfusion pressure during bypass (60-70 mmHg) has been previously associated with an increased occurrence of postoperative delirium, while no differences in intraoperative cerebral oximetry values were found between a low and high systemic perfusion pressure group.⁹⁹ On the other hand, an ABP above the upper limit leads to cerebral hyperperfusion and possibly even edema, swelling, and hemorrhag-

es^{77,78,100}, predisposing the patient to an increased risk of postoperative delirium.⁹⁴ Thus, maintenance of an adequate target ABP is important to enable autoregulatory vascular compensation¹⁷ and thereby minimizing thrombotic and hypoxic events contributing to PNC.^{101,102} A recent study by Moerman et al. described several patterns of autoregulatory activity in response to a 20% change in blood pressure by administration of vasoactive drugs.²⁹ One would expect that when CA is intact, CBF and rSO₂ remain constant despite changes in perfusion pressure. However, Moerman et al. observed a paradoxical response in some of the patients, i.e., a decrease in rSO₂ when the perfusion pressure was increased and an increase in rSO₂ when the perfusion pressure was decreased under normocapnic conditions. The authors contributed this phenomenon to an overcompensation of CA and considered it part of the normal physiologic response. Since multiple reaction patterns in cerebral autoregulatory activity were observed, they concluded that individualization of ABP targets might be the optimal approach in order to prevent hypo- and hyperperfusion. For example, in traumatic brain injury patients, CA may vary within a short time scale, underlining the importance of continuous CA monitoring.⁸²

Presumably this may prove beneficial in terms of PNC risk. Although carbon dioxide reactivity has shown to influence CBF and thus CA, all measurements in the study of Moerman et al. were performed at normocapnia, thereby precluding analysis of individual patterns of CA at different levels of P_aCO₂.

Apart from the influence of mean ABP, several studies showed elevated levels of P_aCO₂ to be accompanied by a decreased level of CA^{69,87,103}, affecting hemoglobin saturation and CBF.²³ The report by Ševerdija et al. illustrated that hypercapnia is associated with a decreased autoregulatory activity (compared to normocapnia), whereas under hypocapnic conditions the level of CA is relatively close to baseline values.⁶⁹ This effect has been elucidated through several studies and can be explained by the phenomena of hypocapnia causing an expansion of the autoregulatory plateau, resulting in improved CA functionality.¹⁰⁴⁻¹⁰⁶ In other words, both ABP and P_aCO₂ influence cerebral CBF and are still not tightly controlled within the autoregulatory limits during CPB (mean ABP between 60 and 150 mmHg and P_aCO₂ between 4.7 and 5.3 kPa or 35 and 40 mmHg).^{69,107}

Additionally, the extent of hemodilution (hematocrit level ≤18% or <19%) showed to be related to PNC and possibly an increased risk of mortality.^{108,109}

Mathew et al. even had to prematurely terminate their study due to the occurrence of adverse events attributed to profound hemodilution.¹⁰⁸ Specifically, hemodilution has been associated with perioperative stroke in cardiac surgical patients.¹¹⁰ This relation can be partially explained by its adverse effects on CA.¹¹¹ Ševerdija et al. showed that patients with a reduced hematocrit (<28%) during bypass have decreased levels of CA⁶⁹, whereas Karkouti et al. reported

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that a 12% decrease in hematocrit is associated with neurocognitive decline.¹¹⁰ Hemodilution combined with hypercapnia even resulted in the largest decrease in autoregulatory activity during CPB.⁶⁹ These studies, therefore, emphasize the adverse effects of nadir hemodilution during CPB.

In conclusion, disturbances in CA are associated with cerebral malperfusion, contributing to adverse neurological outcome following cardiac surgery with CPB. Therefore, tight control of mean ABP within the autoregulatory range, avoiding hypercapnia and minimizing hemodilution and hemodynamic fluctuations during CPB will collectively contribute to preservation of CA and a further decrease in PNC occurrence. Although the literature linking cerebral oximetry readings and PNC remains inconclusive, clinicians should prioritize maintaining an intact CA rather than solely focusing on maintaining rSO_2 values above a certain threshold. Future studies should aim at determining personalized values of mean ABP and P_aCO_2 in order to preserve an intact CA.

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CHAPTER 3

Hemodilution combined with hypercapnia impairs cerebral autoregulation during normothermic cardiopulmonary bypass

EE Ševerdija*, NPA Vranken*, AP Simons, ED Gommer, JH Heijmans, JG Maessen, PW Weerwind

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*These authors contributed equally to this study.

CHAPTER 3

Abstract

Objective: To investigate the influence of hemodilution and arterial PCO_2 on cerebral autoregulation and cerebral vascular CO_2 reactivity.

Design: Prospective interventional study.

Setting: University hospital-based single-center study.

Participants: Forty adult patients undergoing elective cardiac surgery using normothermic cardiopulmonary bypass.

Interventions: Blood pressure variations induced by 6/minute metronome-triggered breathing (baseline) and cyclic 6/min changes of indexed pump flow at 3 levels of arterial PCO_2 .

Measurements and main results: Based on median hematocrit on bypass, patients were assigned to either a group of a hematocrit $\geq 28\%$ or $< 28\%$. The autoregulation index was calculated from cerebral blood flow velocity and mean arterial blood pressure using transfer function analysis. Cerebral vascular CO_2 reactivity was calculated using cerebral tissue oximetry data. Cerebral autoregulation as reflected by autoregulation index (baseline 7.5) was significantly affected by arterial PCO_2 (median autoregulation index amounted to 5.7, 4.8, and 2.8 for arterial PCO_2 of respectively 4.0, 5.3, and 6.6 kPa, $p \leq 0.002$) respectively. Hemodilution resulted in a decreased autoregulation index; however, during hypocapnia and normocapnia, there were no significant differences between the two hematocrit groups. Moreover, the autoregulation index was lowest during hypercapnia when hematocrit was $< 28\%$ (autoregulation index 3.3 versus 2.6 for hematocrit $\geq 28\%$ and $< 28\%$, respectively, $P = 0.014$). Cerebral vascular CO_2 reactivity during hypocapnia was significantly lower when perioperative hematocrit was $< 28\%$ ($P = 0.018$).

Conclusions: Hemodilution down to a hematocrit of $< 28\%$ combined with hypercapnia negatively affects dynamic cerebral autoregulation, which underlines the importance of tight control of both hematocrit and P_aCO_2 during CPB.

Introduction

Cardiopulmonary bypass (CPB) enables complex cardiac surgery. Neurologic complications, however, still remain a major concern and may be linked to altered brain perfusion.¹ In general, reduced vasomotor reactivity has been associated with an increased risk of death.² In cardiac surgical patients, impaired cerebral autoregulation has been associated with an adverse cognitive outcome.¹ Others found a clear relationship between perioperative stroke risk and nadir hematocrit values.³ An interventional study by Mathew et al. on hemodilution with subsequent decreased levels of hematocrit during hypothermic CPB had to be preliminarily terminated, because of significant occurrence of adverse events in the low hematocrit group.⁴ Moreover, increased levels of arterial CO₂ have shown to decrease cerebral autoregulation.⁵ To the best of the authors' knowledge, however, there is no literature available that combines cerebral autoregulation and/or cerebral vasomotor reactivity with both hematocrit level and arterial partial gas pressure of CO₂ (P_aCO₂).

The aim of this study was to investigate cerebral autoregulation and cerebral vascular reactivity with respect to hemodilution and arterial CO₂ levels during normothermic CPB.

Methods

Study population

To study dynamic cerebral autoregulation and cerebral vascular reactivity for CO₂, 40 random male patients scheduled for elective coronary bypass surgery in the time period July 2009 through July 2012 were included in this prospective explorative study. Presence of an adequate temporal acoustic window was the main inclusion criterion, along with absence of neurologic, renal, liver, or severe pulmonary disorders, diabetes, and severe atherosclerosis of carotid and/or middle cerebral arteries.

The study was approved by the medical ethical committee of the Maastricht University Medical Center (Dutch trial registration: NTR1723). All patients gave written informed consent.

Patient management and conduct of CPB

General anesthesia was induced with infusion of 1.0 µg/kg of sufentanil (Hamel Pharmaceuticals, Hameln, Germany), 2.0 mg/kg of propofol (Fresenius Kabi, Zeist, The Netherlands) and 1.0 mg/kg rocuronium bromide (Fresenius

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Kabi, Zeist, The Netherlands). A subsequent propofol infusion (Fresenius Kabi, Zeist, the Netherlands) was set to 5.0 mg/kg/h.

During normothermic nonpulsatile CPB using central cannulation, the centrifugal pump bypass flow rate was targeted at 2.4 l/min/m² body surface area. Mean arterial blood pressure was kept near the preoperative baseline value (between 70 mmHg and 90 mmHg) using phenylephrine titration (pharmacy of Radboud UMC, Nijmegen, The Netherlands) via an infusion pump if necessary. Arterial partial gas pressure of O₂ was kept between 13 and 20 kPa. Cardiac arrest was induced using crystalloid cardioplegia (St. Thomas II, St. Thomas Hospital, Exeter, United Kingdom).

Radial arterial blood pressure (ABP) was measured continuously using a patient monitoring system (Philips Healthcare, Eindhoven, The Netherlands). Pump flow was measured using an ultrasonic flow monitor (Transonic Systems Inc., Ithaca, NY). Cerebral blood flow velocity (CBFV) was measured from the left and right middle cerebral arteries at a depth ranging from 45 to 56 mm using two 2 MHz transcranial Doppler probes (ST3, Spencer Technologies, Seattle, WA) respectively. Data signals of ABP, pump flow, and CBFV were collected and recorded using a data acquisition system (IDEEQ, Maastricht Instruments, Maastricht, The Netherlands). Cerebral tissue oxygen saturation (S_{ct}O₂) was monitored continuously using near-infrared spectroscopy (ForeSight, Casmed, Branford, CT). Hematocrit, P_aCO₂ and pH were measured inline continuously (CDI500, Terumo, Tokyo, Japan).

Dynamic assessment of cerebral autoregulation

Cerebral autoregulation was assessed dynamically prior to administration of preoperative medication in the patient ward at rest (baseline) and in the operating room during CPB. On the ward, hematocrit was determined using a blood sample and autoregulation was assessed analogous to Diehl et al. using metronome-triggered 6/minute breathing to vary cardiac preload and resultant cardiac output.⁶ CBFV was measured using transcranial Doppler sonography, and ABP was measured noninvasively via Portapres (Finapres Medical Systems, Amsterdam, The Netherlands). The cerebral autoregulation index (ARI) was estimated using the resulting step response function in ABP and CBFV.^{7,8} In the operating room during CPB, autoregulation was assessed with the aorta cross clamped and after cardioplegia administration. In contrast to the baseline measurement that used manipulations in cardiac output, during CPB the indexed pump flow was changed in a cyclic manner. During a time frame of 300 seconds, flow was varied with a frequency of 6 cycles/min and 2.5 s per indexed flow rate (from 2.4 L/min/m² to 2.0 L/min/m² and back to 2.4 L/min/m², and from 2.4 L/min/m² to 2.8 L/min/m² and back to 2.4 L/min/m², etc.), as described el-

sewhere.⁹ ARI then was estimated using the recordings of pump flow, ABP, and CBFV.

Assessment of cerebral vascular reactivity

Cerebral vascular reactivity for CO₂ (CO₂R) was assessed using the recordings of S_{ct}O₂ and P_aCO₂. The P_aCO₂ at start of extracorporeal circulation was maintained at 5.3 kPa. For measurement purposes, P_aCO₂ was varied stepwise from 4.0 kPa to 5.3 kPa to 6.6 kPa by adjusting sweep gas flow to the oxygenator and brought back to 5.3 kPa at the end of the measurements. The induced hypocapnic and hypercapnic conditions lasted for 5 minutes each. Subsequently, absolute cerebral CO₂R (CO₂R_{abs}) and relative cerebral CO₂R (CO₂R_{rel}) were calculated for each change in P_aCO₂ using the following formulae:

$$\text{cerebral CO}_2\text{R}_{\text{abs}} = \Delta S_{\text{ct}}\text{O}_2 / \Delta P_{\text{a}}\text{CO}_2$$

and

$$\text{cerebral CO}_2\text{R}_{\text{rel}} = (\text{cerebral CO}_2\text{R}_{\text{abs}} / S_{\text{ct}}\text{O}_{2;5.3 \text{ kPa}}) * 100\%$$

where $\Delta S_{\text{ct}}\text{O}_2$ represents the difference in S_{ct}O₂ measured before and after an alteration of p_aCO₂, during CPB ; $\Delta p_{\text{a}}\text{CO}_2$ represents the difference in P_aCO₂. S_{ct}O_{2;5.3 kPa} represents S_{ct}O₂ measured at a P_aCO₂ of 5.3 kPa.

Data processing and statistical analysis

Depending on the on-bypass hematocrit level after aortic cross-clamping and after induction of cardiac arrest, patients were assigned to a group with a hematocrit value during CPB $\geq 28\%$ (high hematocrit group) or $< 28\%$ (low hematocrit group), with 28% corresponding to the median hematocrit value calculated from all patients. For data of CBFV, ARI and S_{ct}O₂, average values of the left and right cerebral hemispheres were calculated and used for statistical analysis. Data distribution was assessed by performing the Shapiro-Wilk test and visual assessment of histograms. Depending on data distribution, numerical parameters are depicted either in mean and standard deviation or median and interquartile range. Values for CBFV, ARI, and S_{ct}O₂ acquired from both left and right hemispheres were averaged. The independent samples Mann-Whitney U test was used for comparison of numerical variables between the 2 groups of hematocrit. Cerebral autoregulation was tested between different levels of P_aCO₂ by the related samples of Friedman's two-way analysis of variance by ranks. If significant, the related samples of Wilcoxon signed rank test was used as a post-hoc test.

Cerebral autoregulation was tested between the 2 levels of hematocrit for each level of P_aCO₂ by using the independent samples of Mann-Whitney U test. A P-value < 0.05 was considered statistically significant for all tests.

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Results

Patient demographics and preoperative data for all patients divided according to perioperative hematocrit level are shown in Table 1. Analysis revealed no significant difference between the high ($\geq 28\%$) and low hematocrit ($< 28\%$) groups except for preoperative hematocrit ($P=0.002$).

Table 2 shows CPB time, aortic cross-clamp time, difference in perioperative hematocrit, and the effect of hematocrit on cerebral CO_2R . Hematocrit during hypercapnia affected neither absolute nor relative cerebral CO_2R . During hypocapnia, in contrast, hematocrit was noted to have a significant effect on cerebral CO_2R (cerebral $\text{CO}_2\text{R}_{\text{abs,hypo}}$ and $\text{CO}_2\text{R}_{\text{rel,hypo}}$, $P=0.018$ for both).

Table 1. Patient demographics and preoperative data, specified for all ($n=40$) and per perioperative hematocrit group.

hematocrit	$n=40$	$\geq 28\%$, ($n=21$)	$< 28\%$, ($n=19$)	P-value $\geq 28\%$ vs $< 28\%$
age (years)	60.1 [55.8-68.6]	58.9 [55.4-68.6]	61.2 [56.4-68.7]	0.566
BSA (m^2)	2.1 [1.9-2.2]	2.1 [1.9-2.2]	2.0 [1.8-2.1]	0.624
preoperative haematocrit (%)	44.0 [42.3-46.0]	46.0 [43.0-47.0]	43.0 [40.8-44.3]	0.002
ABP (mmHg)	86.0 [78.9-97.0]	86.0 [79.3-98.7]	85.7 [78.1-95.7]	0.578
S_{ctO_2} (%)	71.9 [70.0-73.9]	72.0 [70.4-74.7]	71.0 [68.8-72.3]	0.098
CBFV (cm/s)	40.3 [34.5-47.6]	39.3 [34.4-47.7]	41.8 [36.5-49.7]	0.561
ARI	7.5 [7.0-8.0]	7.4 [6.5-8.0]	7.5 [7.1-8.0]	0.671

Data presented as median [interquartile range].

Abbreviations : BSA, body surface area; ABP, arterial blood pressure; S_{ctO_2} , cerebral tissue oxygen saturation; CBFV, cerebral blood flow velocity; ARI, autoregulation index.

Comparing cerebral autoregulation at the 3 levels of P_aCO_2 for all 40 patients, regardless of hematocrit, showed autoregulation to be significantly affected by P_aCO_2 level compared to both baseline (7.5 [7.0-8.0]) and to the other P_aCO_2 levels ($P \leq 0.002$); for $\text{P}_a\text{CO}_2 = 4.0, 5.3$, and 6.6 kPa, the median ARI was 5.7 [4.8-6.4], 4.8 [4.0-5.7], and 2.8 [2.3-3.8], respectively. Compared to baseline and regardless of hematocrit, ARI proved lowest during hypercapnia ($P < 0.001$).

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Table 2. Perioperative data and cerebral vascular reactivity for CO₂ for the high and low hematocrit group.

	≥28% (n=21)	<28% (n=19)	P-value
CPB time (min)	71.0 [58.5-82.5]	82.0 [62.0-93.0]	0.231
aortic cross clamp time (min)	49.0 [41.0-58.5]	47.0 [38.0-66.0]	0.585
perioperative hematocrit (%)	30.0 [28.5-31.0]	23.0 [22.0-25.0]	<0.001
cerebral CO ₂ R _{abs,hypo} (%S _{ct} O ₂ /kPa)	1.5 [1.2-2.3]	0.8 [0.4-1.9]	0.018
cerebral CO ₂ R _{rel,hypo} (%S _{ct} O ₂ /kPa)	2.3 [1.7-3.3]	1.2 [0.6-3.1]	0.018
cerebral CO ₂ R _{abs,hyper} (%S _{ct} O ₂ /kPa)	2.3 [1.7-3.5]	2.7 [1.9-3.1]	0.856
cerebral CO ₂ R _{rel,hyper} (%S _{ct} O ₂ /kPa)	3.6 [2.4-5.4]	4.1 [2.9-4.7]	0.705

Data presented as median [interquartile range]. S_{ct}O₂, cerebral tissue oxygen saturation; CPB, cardiopulmonary bypass; CO₂R_{abs,hypo}, absolute change of cerebral vascular reactivity for CO₂ when altering P_aCO₂ from 5.3 kPa to 4.0 kPa; CO₂R_{rel,hypo}, relative change of cerebral vascular reactivity for CO₂ when altering P_aCO₂ from 5.3 kPa to 4.0 kPa; CO₂R_{abs,hyper}, absolute change of cerebral vascular reactivity for CO₂ when altering P_aCO₂ from 5.3 kPa to 6.6 kPa; CO₂R_{rel,hyper}, relative change of cerebral vascular reactivity for CO₂ when altering P_aCO₂ from 5.3 kPa to 6.6 kPa.

Table 3 shows intraoperative variables at different levels of both P_aCO₂ and hematocrit. Analyzing cerebral autoregulation with respect to hematocrit only showed a significant difference at hypercapnia, during which ARI was lowest in the <28% group (3.3 versus 2.6 for hematocrit ≥28% and <28% respectively, P=0.0014). A more illustrative presentation is provided by Figure 1. None of the authors' study patients experienced any adverse neurological complications as expressed by delirium, cerebral vascular accident, and transient ischemic attack during the surgical procedure or in a 30 day follow-up.

Table 3. Perioperative variables.

	hematocrit $\geq 28\%$ (n=21)			hematocrit $< 28\%$ (n=19)		
	4.0 kPa	5.3 kPa	6.6 kPa	4.0 kPa	5.3 kPa	6.6 kPa
$p_a\text{CO}_2$						
ARI	6.1 [5.5-6.5]	5.6 [4.6-6.2]	3.3 [2.5-4.2]	5.5 [4.1-6.2]	4.4 [3.9-5.1]	2.6 [1.6-3.7]
CBFV (cm/s)	22.7 [16.7-29.9]	27.6 [22.7-34.7]	46.2 [30.0-56.6]	29.1 [23.1-30.2]	39.3 [32.5-41.4]	52.8 [45.5-57.2]
ABP (mmHg)	80.8 [70.4-85.6]	81.2 [74.0-90.3]	83.0 [76.6-93.5]	70.7 [63.4-79.6]	78.6 [69.4-89.0]	79.2 [69.9-85.8]
$S_{a}\text{O}_2$ (%)	64.5 [63.0-67.3]	67.0 [65.0-69.5]	70.5 [68.3-73.0]	64.5 [62.0-66.5]	66.0 [65.0-70.0]	69.5 [67.0-72.0]

Data presented as median [interquartile range].

Abbreviations : $P_a\text{CO}_2$, arterial partial gas pressure of CO_2 ; ARI, autoregulation index; CBFV, cerebral blood flow velocity; ABP, arterial blood pressure; $S_{a}\text{O}_2$, cerebral tissue oxygen saturation.

Figure 1. Cerebral autoregulation as indicated by the autoregulation index (ARI) at baseline, at 3 levels of P_aCO_2 , and at 2 levels of hematocrit during cardiopulmonary bypass.

Discussion

This study investigated dynamic cerebral autoregulation (dCA) during normothermic nonpulsatile CPB. Autoregulation proved to be lower compared to preoperative values and was affected by intraoperative hematocrit and P_aCO_2 . With impaired cerebral autoregulation being reflected by decreased ARI⁷, efforts have been made to assess normal values for ARI in both awake and anesthetized patients.^{10,11} In the authors' study, the preoperative median ARI in awake patients at rest was 7.5 (Figure 1). Tiecks et al. found ARI to amount to 5 ± 1 in patients at rest during light propofol anesthesia⁷, to which our results closely correspond. The authors measured in normocapnic ($P_aCO_2 = 5.3$ kPa) patients a median ARI of 4.8 for the overall study population even though our patients were on full bypass and propofol anesthetized. Engelhard et al. found mean values for ARI to be 5.4 and 5.9 in awake patients prior to induction of anesthesia¹¹, which are lower compared to the authors' baseline ARI of 7.5. Gommer et al.⁸ showed an average ARI of 6.7 in young healthy volunteers using paced breathing at a 6/min frequency, an ARI higher compared to that for spontaneous breathing. Additionally, Engelhard et al. reported a mean ARI of 4.9 in abdominal surgical patients during anesthesia with combined propofol and remifentanyl,

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which closely correlated to the authors' results, showing a median of 4.8 in normocapnic anesthetized patients. Although the hematocrit of the patients in that study was not mentioned, it may be expected that those patients were not exposed to such a relatively high level of hemodilution with resulting low hematocrit as our patients undergoing CPB (hematocrit_{median}=28%). The patients in the study of Engelhard et al., however, showed ARI values relatively similar to those of the authors' patients, therefore suggesting these values to be representative for a normal ARI in the average normocapnic propofol-anesthetized cardiac surgical patient on bypass. In addition, propofol is known to decrease CBFV by reducing the cerebral metabolic rate of oxygen.^{12,13} Nevertheless, cerebral autoregulation has shown to be unaffected by propofol anesthesia, which implies that normal cerebral circulation and metabolism are maintained.¹⁴ With literature and the authors' data showing comparable values for ARI, their baseline and perioperative normocapnic measurements of ARI may be considered clinically representative for unimpaired (intact) values for cerebral autoregulation. This suggests that their baseline values measured in awake unanesthetized patients also may be applicable to surgical patients in general.

In surgical patients, impaired cerebral autoregulation (i.e., in the authors' data represented by decreased ARI levels) has been associated with increased occurrence of perioperative stroke.¹⁵ Additionally, a low hematocrit during CPB is known to contribute to postoperative morbidity and mortality.^{3,4,16} The authors' study investigated the effect of perioperative hematocrit on dCA, and found ARI to be decreased at a hematocrit level <28% (at a P_aCO₂ level of 6.6 kPa). The relation between hemodilution and impaired dCA previously was elucidated by Ogawa et al., but they studied awake subjects and did not include measurements of P_aCO₂.¹⁷ Karkouti et al. found hemodilution to be associated with perioperative stroke.³ Roach et al. found that impaired cerebral autoregulation is associated with adverse neurological outcome.¹ As a result of lowered perioperative hematocrit negatively influencing both cerebral autoregulation and postoperative neurological outcome, low hematocrit levels due to excessive hemodilution should be avoided, and techniques limiting hemodilution could prove beneficial.^{18,19}

Arterial CO₂ level has been demonstrated to affect cerebral blood flow by altering cerebral vasomotor reactivity.²⁰ The authors' data also show that ARI decreases with increasing P_aCO₂. For P_aCO₂=4.0, 5.3, and 6.6 kPa, the index amounted 5.7, 4.8, and 2.8, respectively. A study conducted by Henriksen et al. showed a negative effect on cerebral autoregulation when P_aCO₂ level was increased.⁵ Moreover, Henriksen et al. found cerebral autoregulation to be near-absent at a P_aCO₂ level >50 mmHg (>6.7 kPa). Although the authors used such

a high $P_a\text{CO}_2$ level as well, results indicated a decreased but still present level of cerebral autoregulation, as depicted by a 35% reduction ($\text{ARI}=2.6$) and 44% reduction ($\text{ARI}=3.3$) of autoregulation for the low and high hematocrit group, respectively, compared to baseline in awake subjects ($\text{ARI}=7.5$). With decreased cerebral autoregulation being associated with impaired or adverse neurological outcome, these data underline the importance of tight control of $P_a\text{CO}_2$ during CPB.¹

Cerebral autoregulation is a complex physiological mechanism, which is influenced by several factors including hematocrit and $P_a\text{CO}_2$.^{21,22} Ono et al. studied cerebral autoregulation during CPB and found increased $P_a\text{CO}_2$ levels to be a factor of negative influence.¹⁵ As indicated by the authors' data, dCA was reduced with a lower hematocrit (Table 3). The data also showed that increased levels of $P_a\text{CO}_2$ resulted in decreased ARI as well. Combining hypercapnia with low hematocrit ($<28\%$) showed the largest decrease in ARI compared to baseline (median $\text{ARI}_{\text{baseline}}=7.5$ (Fig 1). Summarized, the difference in ARI between patients with higher ($\geq 28\%$) and lower ($<28\%$) hematocrit ($\Delta\text{ARI}=4.2$ and $\Delta\text{ARI}=4.9$, respectively) was most pronounced at the lower limit of cerebral autoregulation (2.8 [2.3 - 3.8]), which is found at a $P_a\text{CO}_2$ level of 6.6 kPa. A possible explanation for the authors' finding is that hemodilution induces a reduction in viscosity and compensatory vasodilatation, therefore increasing CBFV, which results in a decreased autoregulatory capacity.²³ The detrimental effect of combined hypercapnia and hemodilution underlines, once more, the importance of adequate $P_a\text{CO}_2$ monitoring and tight perioperative $P_a\text{CO}_2$ control while avoiding extreme hemodilution in order to diminish the risk of cognitive complications and adverse neurologic clinical outcome.

Cerebral CO_2R plays an intricate part in the vascular autoregulatory system of the brain and aims at minimizing the effects of fluctuations in arterial blood pressure on cerebral perfusion.²⁴ The authors' study showed that in hypocapnia there was a significant positive relationship between cerebral CO_2R and hematocrit (Table 2). Tu et al. found similar results, reporting a decreased cerebral CO_2R with isovolemic hemodilution.²⁵ In contrast to Tu et al's study, however, the authors included alterations of $P_a\text{CO}_2$ and showed that both hemodilution and arterial CO_2 level affect cerebral CO_2R . Henriksen also found that decreased cerebral CO_2R during hypocapnia is related to distinct changes in hematocrit.⁵ This is in line with the authors' findings of a significant difference in cerebral CO_2R between the 2 hematocrit groups at a $P_a\text{CO}_2$ level of 4.0 kPa (Table 2). This can be explained by the fact that although cerebral autoregulation is suppressed during hypercapnia, cerebral blood flow as such is present. Blood

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flow even can be increased due to lowered viscosity as a result of hemodilution and increased cerebral CO₂R.

This study investigated cerebral autoregulation and found low hematocrit (<28%) combined with hypercapnia to significantly decrease ARI. None the authors' study patients, however, experienced any adverse neurological complications as expressed by delirium, cerebral vascular accident, and transient ischemic attack during the surgical procedure or in a 30-day follow-up. This could be attributed to the short duration of 5 minutes in which hypercapnia was induced. Another explanation can be found in the authors' protocol of keeping mean arterial blood pressure in the 70 mmHg-to-90 mmHg range, which is close to the baseline values of their patients and in which cerebral autoregulation is generally considered present.²⁶

In the authors' study, CBFV was measured using transcranial Doppler, a method that presumes the assumption of a constant vessel diameter.²⁷ As previously elucidated, both P_aCO₂ and hemodilution significantly affect cerebral CO₂R and thereby blood flow, two factors that were altered in the authors' study subjects. However, several studies have exemplified that the diameter of larger arteries change minimally during hemodilution and hypercapnia.^{28,29} Therefore, changes in CBFV in the middle cerebral artery measured by Doppler legitimately reflect changes in cerebral blood flow.

Cerebral autoregulation is estimated by measuring CBFV at the middle cerebral artery using transcranial Doppler via the temporal window.²⁴ The authors' study showed preoperative CBFV in resting conditions to be around 40 cm/s (Table 1). Liboni et al. found CBFV to amount to approximately 67 cm/s³⁰, whereas Lindegaard et al. found CBFV to vary between 32 to 78 cm/s.³¹ Lindegaard et al. and the authors' study, however, included male patients, whereas Liboni et al. measured CBFV in women. In women, a proper acoustic optical temporal window frequently is absent, which impedes measurement of cerebral autoregulation.³² Although the authors' study did not include female patients, women show comparable or higher CBFV values^{30,33} and their results on cerebral autoregulation may be applicable to the full cardiac surgical population, including both genders.

Conclusion

Hemodilution down to a hematocrit of <28% combined with hypercapnia negatively affects dynamic cerebral autoregulation, which underlines the importance

of tight control of both hematocrit and $P_a\text{CO}_2$ during CPB. Perioperative cerebral monitoring proves a valuable tool for future studies evaluating cerebral autoregulation during CPB to, hopefully, clarify optimal perfusion strategies.

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CHAPTER 4

Cerebral autoregulation during cardiopulmonary bypass

NPA Vranken, PW Weerwind

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CHAPTER 4

Dear Editor,

Postoperative cognitive dysfunction (POCD) accompanied by short- and long-term effects remains a major burden for patients' recovery and quality of life following cardiac surgery with cardiopulmonary bypass (CPB). Several patient- and procedure-related factors have shown to affect the risk of POCD, as discussed by Messerotti Benvenuti et al. in a recent issue of *Perfusion* (2015;30:514-516).¹ They conclude that pre-existing cognitive status and not the duration of CPB is associated with POCD at middle-term postoperative evaluation. However, the authors did not elaborate on the CPB protocol that was used. For adequate interpretation of POCD risk, it is necessary also to take the cerebral autoregulation (CA) into account, as the neuroprotective autoregulatory system prevents both hypo- and hyperperfusion by reactive vasodilation and constriction following changes in arterial blood pressure (ABP) and arterial carbon dioxide tension.² To maintain an intact CA during CPB, it is, therefore, important to target a mean ABP within the autoregulatory range (60-150 mmHg)² and to maintain normocapnia (4.5-5.5 KPa).³ Moreover, it has been shown that avoiding large fluctuations in hemodynamic parameters during CPB results in a decreased risk of postoperative neurologic complications.⁴

In summary, for middle-term evaluation of POCD, it would be interesting to include intraoperative data on hemodynamics and arterial carbon dioxide tension. Taking this into account, apart from the role of patient-related factors, will add to a better understanding of the contributors involved in POCD risk.

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CHAPTER 5

Impact of intraoperative events on cerebral tissue oximetry in patients undergoing cardiopulmonary bypass

EE Ševerdija*, NPA Vranken*, S Teerenstra, YM Ganushchak, PW Weerwind

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*These authors contributed equally to this study

Abstract

Previous studies showed that decreased cerebral saturation during cardiac surgery is related to adverse postoperative outcome. Therefore, we investigated the influence of intraoperative events on cerebral tissue saturation in patients undergoing cardiac surgery with cardiopulmonary bypass (CPB).

A total of 52 adult patients who underwent cardiac surgery using pulsatile CPB were included in this prospective explorative study. Cerebral tissue oxygen saturation ($S_{ct}O_2$) was measured in both the left and right cerebral hemisphere. Intraoperative events, involving interventions performed by anesthesiologist, surgeon, and clinical perfusionist, were documented. Simultaneously, in-line hemodynamic parameters (partial oxygen pressure, partial carbon dioxide pressure, hematocrit, arterial blood pressure, and CPB flow rates) were recorded.

Cerebral tissue saturation was affected by anesthetic induction ($P<0.001$), placement of the sternal retractor ($P<0.001$), and initiation ($P<0.001$) as well as termination of CPB ($P<0.001$). Placement ($P<0.001$) and removal of the aortic cross-clamp ($P=0.026$ for left hemisphere, $P=0.048$ for right hemisphere) led to changes in cerebral tissue saturation. In addition, when placing the aortic cross clamp, hematocrit ($P<0.001$) as well as arterial ($P=0.007$) and venous ($P<0.001$) partial oxygen pressures changed.

Cerebral tissue oximetry effectively identifies changes related to surgical events or vulnerable periods during cardiac surgery. Future studies are needed to identify methods of mitigating periods of reduced cerebral saturation.

Introduction

Despite impressive improvements in the overall safety of cardiac surgery, perioperative cerebral injury remains a major concern.¹ The two major causative factors for neuropsychological dysfunction after cardiac surgery are global brain hypoperfusion and cerebral emboli generated by either surgical or perfusion-related interventions.²⁻⁶ Furthermore, worsened control of cerebral blood flow due to hypertension, diabetes, or other conditions imposes patients intraoperatively to increased risk of neurological complications.^{7,8} However, evaluation of cerebral hemodynamics may still not be part of routine practice.⁹

Intraoperative cerebral monitoring to identify vulnerable periods during cardiac surgery that require prompt intervention (e.g., adjusting the partial carbon dioxide gas pressure or fraction of inspired oxygen) should be a major goal in the fields of cardiac anesthesia, surgery, and perfusion.^{10,11} In a randomized, blinded, prospective study of 200 patients, Murkin et al.¹² demonstrated that non-invasive regional cerebral saturation monitoring is associated with a significant improvement in overall outcome after cardiac surgery.

Moreover, using a protocol-based interventional strategy to maintain cerebral saturation within 75% of baseline values during cardiopulmonary bypass (CPB) may improve both neurological and multi-organ dysfunction outcomes in cardiac surgery.^{12,13} Using the brain as an index organ for adequate tissue perfusion may therefore be beneficial for all vital organs.¹⁴ Routine monitoring of cerebral saturation during cardiac surgical interventions may therefore detect early signs of post-surgery neurological deficits.

In this study, intraoperative events were recorded in order to qualify the effects on cerebral tissue oxygen saturation ($S_{ct}O_2$) in patients undergoing cardiac surgery with pulsatile CPB.

Materials and methods

Patients

This prospective, explorative non-randomized clinical study included 52 adult patients (38 male and 14 female) that underwent elective cardiac surgery using pulsatile CPB between November 2011 and May 2012. No restrictions or inclusion criteria were applied. Institutional approval was received for this evaluation and since the study did not influence the routine care of the patient, informed consent was waived.

Non-invasive absolute ($S_{ct}O_2$) was routinely measured via near-infrared spectroscopy (FORE-SIGHT; CAS Medical Systems, inc., Branford, CT) by placing a fiber optic sensor on each side of the patient's forehead. Cerebral oximetry was

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measured in both the left and right hemisphere. $S_{ct}O_2$ data were simultaneously recorded every 2 seconds. All intraoperative events from anesthetic induction to discharge from the operating room were marked including the corresponding time in the data file. No interventions based on $S_{ct}O_2$ changes were applied intraoperatively and data used for analysis were routine measurements.

Anesthesia

After establishing standard anesthetic monitoring including electrocardiogram, oxygen saturation, and invasive arterial blood pressure (ABP) measurement, general anesthesia was induced with 0.5 $\mu\text{g/kg}$ sufentanil, 1.5 mg/kg propofol, and 0.6 mg/kg rocuronium. After endotracheal intubation, the patients were ventilated with volume-controlled ventilation with tidal volumes of 7-8 mL/kg , positive end-expiratory pressure of 5 $\text{cm}\cdot\text{H}_2\text{O}$, respiratory rate of 12/min, and a fraction of inspired oxygen of 0.4, which resulted in normocapnia and normal oxygen oxygen saturation. Anesthesia was maintained with sevoflurane at a minimal alveolar concentration of approximately 0.8. Perioperative analgesic regime contained continuous intravenous administration of (S)-ketamine, lidocaine, and boluses of sufentanil.

Prior to surgery a warming blanket (3M Bair Hugger, 3M Health Care, Delft, The Netherlands) was positioned to maintain normothermia.

Cardiopulmonary bypass

The CPB system included a standard hollow-fiber membrane oxygenator (Capi-ox SX18R; Terumo Medical Corps., Tokyo, Japan), a roller pump (S5; Sorin Group S.p.A, Mirandola, Italy), a cardiotomy reservoir (Capi-ox CXCRXA, Terumo), a collapsible venous reservoir (JVR 1900; Maquet Cardiopulmonary AG, Rastatt, Germany), and an arterial line filter (Leukogard-6, Pall, East Hills, NY). The standard priming of the CPB circuit consisted of 1500 mL of 4% gelofusin (B. Braun Melsungen AG, Melsungen, Germany), 200 mL of 20% mannitol (Viaflo; Baxter BV, Utrecht, The Netherlands), 100 mL of 20% human albumin (Albuman; Sanquin, Utrecht, The Netherlands), 50 mL of 8.4% NaHCO_3 , and 20 mL of 10% calcium gluconate (B. Braun Melsungen AG). The total volume of the CPB priming amounted to 1870 mL clear fluid, containing 7500 IU heparin (Leo Pharmaceutical Products BV, Weesp, The Netherlands). The activated coagulation time was kept >400 seconds during bypass. Myocardial preservation was provided via the aortic root or selectively via the coronary ostia by a single dose of cardioplegic solution (800 ± 200 mL; St. Thomas' hospital No.1) at 4°C . Depending on the patients' body surface area, the ascending aorta was cannulated using either a 22- or 24-Fr cannula (Maquet Cardiopulmonary AG). A dual-stage venous cannula (32/40 or 36/51 Fr; Edwards Lifesciences BV, Breda, The Netherlands) was used for gravity drainage during coronary artery

bypass grafting and aortic valve surgery. In case mitral or tricuspid valve surgery was involved, the venae cavae were cannulated separately using a DLP single-stage metal tip cannula (28 and 31 or 24 and 28 Fr; Medtronic, Inc., Minneapolis, MN).

Target flow rates of ≥ 2.6 L/min/m² body surface area were maintained throughout normothermic (36.3°C) CPB. Pulsatile flow (radial artery pulse pressure ≥ 25 mmHg) was used only during the period of cross-clamping with a frequency of 70 beats per minute, a base flow of 28% (1.4 L/min), and a pulse width of 50% (0.42 seconds). Mean ABP was maintained at 80 ± 10 mmHg by titration of phenylephrine (0.4 mg/mL) via an infusion pump if necessary. The sweep gas and fraction of inspired oxygen settings for the oxygenator were titrated to maintain normocapnia (arterial partial carbon dioxide pressure - $P_a\text{CO}_2$ 4.5 - 5.5 kPa) and normoxia (partial arterial oxygen pressure - $P_a\text{O}_2$ 11.0 - 14.0 kPa). All patients received tranexamic acid (2 mg) during CPB. The transfusion trigger during CPB was set at a hematocrit level $< 25\%$. Pericardial blood was drained and washed with a cell saver device.

During valve and aortic root procedures carbon dioxide flooding was routinely used. By maintaining in-line normocapnia, no episodes of high $P_a\text{CO}_2$ that could have potentially influenced the cerebral saturation occurred.

Near-infrared spectroscopy

Cerebral tissue oximetry is measured non-invasively as described by Murkin and Arango.¹⁴ In short, oxygen content in the frontal lobes is measured by near-infrared light penetrating the skin, skull, and other protective tissues. Near-infrared light (660-940 nm) is partly scattered by chromophores within the tissue, absorbed by oxyhemoglobin or deoxyhemoglobin. The fiber optic sensors used in this study emit light at four different wavelengths to obtain greater precision for estimation of oxygen content.

Data processing

To be able to relate changes in cerebral saturation to occurring events, several hemodynamic parameters were recorded continuously during CPB: pump flow, ABP, as well as continuous in-line $P_a\text{CO}_2$ and $P_a\text{O}_2$, venous saturation, and electrolytes measurement via an optical fluorescence and reflectance-based system (CDI-500, Blood Parameter Monitoring System; Terumo, Japan). Pump flow was recorded by an ultrasonic flow monitor (Transonic Systems Europe BV, Maastricht, The Netherlands). All in-line measurements except for $S_{ct}\text{O}_2$ were collected using a data acquisition system (M-PAQ; Maastricht Instruments, Maastricht, The Netherlands). To combine all data, sample frequencies had to be equalized in all files. To achieve this, data were either averaged (decreasing the frequency of measuring), or the same data point was duplicated and added

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after its original data point (increasing the frequency of measuring). Subsequently, data synchronization was performed. For further data analysis, samples of 5 minutes were selected. One time sample was selected prior to the event, and the other one during the event.

Statistical analysis

Data are shown as mean $\pm$ SD or median (interquartile range), depending on data distribution. A P-value of $<.05$ was considered statistically significant.

For events occurring before or after CPB, only cerebral $S_{ct}O_2$ and ABP were compared between samples prior and during the event. For placement and removal of the aortic cross-clamp, cerebral $S_{ct}O_2$, mean ABP, pump flow, and blood parameters (P_aCO_2 , P_aO_2 , P_vO_2 and hematocrit) were compared. If one or more parameters differed significantly between the two samples, a possible cause of the difference in $S_{ct}O_2$ could be determined.

Statistical analysis was performed using the Statistical Package for Social Sciences version 15.0 (SPSS inc., Chicago, IL). Distribution of data was tested using the Shapiro-Wilk test. The paired student's t test or Wilcoxon signed-rank test was used to compare cerebral saturation measurement before and during events.

Results

Demographic and baseline data for the 52 enrolled patients are listed in Table 1. Surgical- and perfusion-related data are presented in Table 2.

During the entire intraoperative period, cerebral $S_{ct}O_2$ showed comparable values for both left and right hemisphere. Left and right mean $S_{ct}O_2$ values of $71\pm4\%$ and $70\pm4\%$ were found prior to CPB, $66\pm4\%$ and $65\pm4\%$ during CPB, and $70\pm4\%$ and $69\pm5\%$ after CPB, respectively. Since the difference between the left and right hemisphere can be neglected, the influence of intraoperative events on $S_{ct}O_2$ are depicted in Figure 1 using mean values.

Onset of CPB, placement and removal of the aortic cross-clamp (difference in significance between hemispheres, $P=.026$ for the left and $P=.048$ for right hemisphere) resulted in a decrease in $S_{ct}O_2$, whereas anesthetic induction ($P<.001$), placement of the sternal retractor ($P<.001$), and termination of CPB ($P<.001$) showed to be related to an increase in $S_{ct}O_2$ (Figure 1). Furthermore, phenylephrine infusion ($P=.356$), hemofiltration ($P=.892$) and removal of the sternal retractor ($P=.692$ for the left hemisphere, $P=0.123$ for the right hemisphere) did not result in a significant $S_{ct}O_2$ change. Aortic cross-clamping showed to have a statistically significant impact on cerebral saturation as shown in Figure 1, which may in part be explained by differences in arterial and venous blood gas pa-

rameters and hematocrit. During placement of the aortic cross-clamp, hematocrit decreased significantly ($P<.001$), as well as arterial ($P=.007$) and venous ($P<.001$) oxygen levels (Table 3). The changes in hematocrit, arterial, and venous PO_2 did not occur during removal of the aortic cross-clamp.

In all cases, the postoperative period was uneventful and no intraoperative cerebral ischemic episode occurred.

Table 1. Demographic and baseline data.

gender (male/female)	38/14
age (years)	68 (59.3-75.8)
BMI (kg/m^2)	26.0 (24.4-27.8)
diabetes Mellitus (yes/no)	7/45
peripheral vascular disease (yes/no)	4/48
mean ABP pre CPB (mmHg)	102.1 $\pm$ 11.3
$S_{ct}O_2$ mean pre CPB (%)	70 (66-71)
mean Hct pre CPB (%)	41.0 $\pm$ 3.9

ABP, arterial blood pressure; BMI, body mass index; CPB, cardiopulmonary bypass; Hct, hematocrit; $S_{ct}O_2$, cerebral tissue oxygen saturation.

Parameters in italics are shown as median (interquartile range), and remaining parameters are shown as absolute numbers or mean $\pm$ SD.

Table 2. Surgical and perfusion data.

isolated CABG surgery	59.7% (n=31)
isolated valve surgery	23.1% (n=12)
CABG + valve surgery	13.5% (n=7)
ascending aorta replacement	3.8% (n=2)
CPB time (minutes)	80 (69-105)
aortic cross clamp time (minutes)	55 (43-70)
mean Hct (%) during CPB	28 (25-29)
mean pump flow (L/min)	4.3 $\pm$ 0.5
mean ABP (mmHg) during CPB	75 (71-80)

ABP, arterial blood pressure; CABG, coronary artery bypass grafting; Hct, hematocrit.

Data for mean pump flow is presented as mean $\pm$ SD. Data for CPB time, aortic cross-clamp time, Hct and ABP are presented as median (interquartile range).

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Table 3. Influence of aortic cross clamping on hemodynamic parameters.

Aortic cross-clamp on	Prior to cross-clamping	During cross-clamping	P-value
Mean ABP (mmHg)	72.4 (63.4-80.3)	73.9 (63.5-79.2)	0.420
P _a CO ₂ (kPa)	5.5 (5.1-5.6)	5.4 (5.0-5.6)	0.792
P _a O ₂ (kPa)	14.9 (12.6-18.0)	13.0 (12.3-16.5)	0.007
p _v O ₂ (kPa)	5.9±1.0	5.3±0.6	<0.001
Hct (%)	28.7 (26.5-31.6)	26.4 (24.6-29.0)	<0.001
CPB flow (L/min)	4.3 (3.8-4.7)	4.4 (4.0-4.7)	0.680
Aortic cross-clamp off	Prior to cross-clamp removal	After cross-clamp Removal	P-value
Mean ABP (mmHg)	74.4 (68.7-80.7)	71.6 (67.2-77.7)	0.196
P _a CO ₂ (kPa)	5.5 (5.2-5.7)	5.5 (5.3-5.7)	0.017
P _a O ₂ (kPa)	14.0±2.9	14.4±2.7	0.255
P _v O ₂ (kPa)	5.1±0.5	5.1±0.6	0.535
Hct (%)	27.4 (24.0-29.0)	27.5 (23.7-29.6)	0.761
CPB flow (L/min)	4.1 (2.0-4.7)	3.7 (0.1-4.6)	0.093

ABP, arterial blood pressure; CPB, cardiopulmonary bypass; Hct, hematocrit; p_aCO₂, arterial carbon dioxide level; p_aO₂, arterial oxygen level; p_vO₂, venous oxygen level.

Figure 1. Influence of intraoperative events on mean cerebral S_{ct}O₂. CPB, cardiopulmonary bypass; HF, hemofiltration; S_{ct}O₂, cerebral oxygenation; SR, sternal retractor; X-clamp, aortic cross clamp.

Discussion

Intraoperative events showed to affect cerebral oximetry in patients undergoing cardiac surgery with CPB. Since previous studies suggest that a fall in cerebral saturation is related to adverse neurological outcome, routine measurement of cerebral saturation warrants early detection of brain ischemia during surgery.¹²⁻¹⁴

Our results showed subtle changes in $S_{ct}O_2$ readings following several events that appeared statistically significant while absolute differences were relatively small and far from the suggested 20% decrease when intervention is required.¹⁴ Presumably the events did not provoke any therapeutically relevant changes in cerebral tissue saturation in our study. One can speculate that maintaining normocapnia, normoxia, and a tight blood pressure control led to minimized fluctuations in cerebral saturation. Iatrogenic events i.e., placement of the aortic cross-clamp can still induce changes in cerebral saturation, which do not necessarily require intervention. On the other hand, the extent of cerebral desaturation requiring an intervention may vary between different sensors, implying that no fixed thresholds have been set.¹⁵ Nonetheless, cerebral oximetry enables clinicians to observe slight changes in cerebral saturation, which may help to prevent further desaturations.

Induction of general anesthesia resulted in a steep increase in cerebral $S_{ct}O_2$, which may be explained by pre-oxygenation with a high-inspired fraction of oxygen and unchanged cardiac output.¹⁶ Conversely, a significant decrease in mean $S_{ct}O_2$ occurred with onset of CPB, which can presumably be explained by acute hemodilution, as the hematocrit dropped from approximately 41% to 28% (Tables 1 and 2). These findings are in line with the study of Han et al.¹⁷ who showed that acute normovolemic hemodilution is associated with a fall in cerebral saturation. Rapid initiation of CPB mostly provoked a drop in $S_{ct}O_2$ as resultant of assanguinous priming solution passage through the cerebral vasculature with inadequate oxygen delivery to the brain.

Placement of the sternal retractor is another factor influencing the cerebral saturation as measured by near-infrared spectroscopy. One could hypothesize that the change in cerebral saturation is caused by strong pain signals transported via the spinal cord during the event. In theory, this causes an immediate elevation in ABP. However, this effect is not observed in this study, which is potentially due to adequate anesthesia and analgesia.

Another theory is that opening the thoracic cavity influenced intrathoracic pressures and venous return, resulting in an increased cerebral saturation. On the

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other hand, removal of the sternal retractor did not show a significant difference in $S_{ct}O_2$. A plausible explanation for this observation is that the hypothesized pain signals were not activated or not in an extent large enough to cause a significant difference. Also, instead of generating pressure on the site of the sternum and surrounding tissue (as in placement of the sternal retractor), the opposite effect could have taken place i.e., relaxation.

Another event that showed to affect cerebral saturation is aortic-cross clamping, which may in part be explained by differences in arterial and venous blood gas parameters and hematocrit (Table 3). Placement of the aortic cross-clamp resulted in sudden excessive withdrawal of blood volume from patient to the heart-lung machine by lowering the CPB flow. This resulted in loss of cardiac output and a drop in ABP with concomitant negative consequences on oxygen delivery to the brain, as reflected by significantly lowered values of PO_2 in both arterial and venous blood. CPB flow was not significantly different between samples of placement and removal of the cross-clamp, most likely because the duration of lowered flow was too short and the heart-lung machine was at optimal flow before and after both these events. In contrast, the decrease in arterial and venous PO_2 did not appear while removing the cross-clamp as by routine during removal of the aortic cross-clamp the CPB flow and ABP are not actively lowered.

Vasoconstriction using phenylephrine infusion did not appear to affect cerebral saturation, which is in contrast with the results of a previous study by Moerman et al.¹⁸ However, Brassard et al.¹⁹ recently showed that the negative effect might only be present in diabetic patients.

Finally, a study limitation is the lack of an intervention-guided design. Physiologic parameters are kept within a certain range, preventing major fluctuations in cerebral tissue saturation during the intraoperative period. Furthermore, data synchronization involving the equalization of the sample frequency led to data (pump flow and ABP) to be leveled out and small fluctuations to be diminished compared to the raw data.

In conclusion, cerebral tissue oximetry by near-infrared spectroscopy effectively identifies subtle changes in cerebral saturation related to surgical events or vulnerable periods during cardiac surgery. Future studies in larger cohorts are required to identify therapeutically relevant changes in cerebral saturation as measured by cerebral oximetry.

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CHAPTER 6

Cerebral and limb tissue oxygenation during peripheral veno-arterial extracorporeal life support

NPA Vranken, AAMA Lindelauf, AP Simons, MJH Ariës, JG Maessen,
PW Weerwind

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Abstract

Femoral access in extracorporeal life support (ECLS) has been associated with regional variations in arterial oxygen saturation, potentially predisposing the patient to ischemic tissue damage. Current monitoring techniques, however, are limited to intermittent bedside evaluation of capillary refill among other factors.

The aim of this study was to assess whether cerebral and limb regional tissue oxygen saturation (rSO_2) values reflect changes in various patient-related parameters during venoarterial ECLS (VA-ECLS).

This retrospective observational study included adults assisted by femorofemoral VA-ECLS. Bifrontal cerebral and bilateral limb tissue oximetry was performed for the entire duration of support. Hemodynamic data were analyzed parallel to cerebral and limb rSO_2 .

A total of 23 patients were included with a median ECLS duration of 5 [1-20] days. Cardiac arrhythmias were observed in 12 patients, which was associated with a decreased mean rSO_2 from $61\pm11\%$ to $51\pm10\%$ during atrial fibrillation and $67\pm9\%$ to $58\pm10\%$ during ventricular fibrillation ($P<0.001$ for both). A presumably sudden increase in cardiac output due to myocardial recovery ($n=8$) resulted in a significant decrease in mean cerebral rSO_2 from $73\pm7\%$ to $54\pm6\%$ and from $69\pm9\%$ to $53\pm8\%$ for the left and right cerebral hemisphere, respectively ($P=0.012$ for both hemispheres). Also, right radial artery partial gas pressure for oxygen decreased from 15.6 ± 2.8 to 8.3 ± 1.9 kPa ($P=0.028$). No differences were found in cerebral desaturation episodes between patients with and without neurologic complications. In six patients, limb rSO_2 increased from on average 29.3 ± 2.7 to 64.0 ± 5.1 following insertion of a distal cannula in the femoral artery ($P=0.027$). Likewise, restoration of flow in a clotted distal cannula was necessary in four cases and resulted in increased limb rSO_2 from 31.3 ± 0.8 to 79.5 ± 9.0 ; $P=0.068$.

Non-invasive tissue oximetry adequately reflects events influencing cerebral and limb perfusion and can aid in monitoring tissue perfusion in patients assisted by ECLS.

Introduction

Despite the increasing experience and continuously improving technology applied in extracorporeal life support (ECLS), femoral access is still associated with regional variations in arterial saturation driven by an impaired oxygen delivery.¹ Specifically, femoral artery cannulation may compromise perfusion of the lower limbs, causing limb ischemia and concomitant tissue damage.^{2,3} Besides impaired limb perfusion, veno-arterial ECLS (VA-ECLS) is linked with the delivery of hypoxic blood to the brain (i.e., differential hypoxia or two-circulation syndrome), resulting in an increased risk of brain damage.⁴ Although maintaining adequate tissue oxygenation is vital in critically ill patients, current monitoring techniques are often limited to bedside observation of capillary refill, limb temperature, and limb color. Continuous non-invasive tissue oximetry could be of added value to monitor regional tissue oxygen saturation (rSO₂) in patients supported by ECLS. This monitoring method is based on the Beer-Lambert law and uses near-infrared spectroscopy (NIRS) to assess local tissue oxygenation.⁵ Tissue oximetry readings are proposed to reflect hemodynamic parameters in real-time, serving as a potential early marker for distal limb and cerebral ischemia.⁵⁻⁷ The literature describing the application of this monitoring technique in patients supported by VA-ECLS, however, remains scarce.⁸⁻¹⁰

The aim of this study was to assess the efficacy of cerebral and limb tissue oximetry during VA-ECLS.

Materials and Methods

Patients

In this retrospective study, data from adult patients assisted by peripheral femoro-femoral VA-ECLS were consulted. Institutional approval was granted based on a retrospective quality analysis of our patient database (trial number 14-4-194). Due to the retrospective nature of the study, informed consent was waived.

Patients were fully sedated and on mechanical ventilation. Support was provided by either a Permanent Life Support system (Maquet Cardiopulmonary AG, Hirrlingen, Germany) or a CardioHelp-mounted HLS Advanced 7.0 module (Maquet Cardiopulmonary), both Bioline-coated. Extracorporeal cardiopulmonary resuscitation patients were actively cooled to a rectal temperature of 33°C for 24 hours and thereafter gradually rewarmed to 37°C using a heater-cooler unit (HCU 30, Maquet Cardiopulmonary). Arterial cannulation was performed

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using a 19Fr. or 21Fr. HLS cannula (Maquet Cardiopulmonary), whereas venous cannulation was performed using a 26Fr. or 29Fr. multi-stage HLS cannula (Maquet Cardiopulmonary). An additional 8Fr. or 10Fr. cannula (Super Arrowflex percutaneous sheath introducer set, Teleflex Medical Europe Ltd, Westmeath, Ireland) was used to provide distal limb perfusion via antegrade cannulation of the femoral artery if necessary. Heparinization was monitored by activated partial thromboplastin time (targeted between 50 and 70 seconds) and at a hematocrit value less than 25% patients received transfusion of packed red blood cells (PRBCs).

Data collection

Bi-frontal cerebral and bilateral limb rSO_2 were routinely monitored using non-invasive tissue oximetry using NIRS (INVOS 5100C Cerebral/Somatic Oximeter, Medtronic, Minneapolis, MN, USA). Immediately upon initiation of VA-ECLS, patients' forehead (left and right side) as well as the medial site of the musculus gastrocnemius (of both limbs) were fitted with a disposable self-adhesive sensor. All sensors were replaced once every seven days during the entire period of ECLS.

Data concerning systolic, diastolic and mean radial artery blood pressure, pulse pressure, cardiac rhythm, pulse oximetry, limb temperature, blood loss and number of transfused PRBCs were retrieved from a critical care and anesthesia data system (Philips ICIP Intellispace version F.00.01, Philips, Eindhoven, the Netherlands). Arterial blood gas analyses were executed using blood samples drawn from the right radial artery during the full period of intensive care unit stay according to hospital protocol. Pulse oximetry was performed at the left index finger. All data acquisition and analyses were performed anonymously and in accordance with the Dutch law for approving medical research.

Data processing

Raw data files retrieved from the clinical oximeter contain one data point every six seconds, i.e. ten data points per minute. The output files were exported to Microsoft Excel (Microsoft Office 2010) for further analysis.

To assess the effect of cardiac rhythm (sinus rhythm, atrial fibrillation (AF), and ventricular fibrillation (VF)) on cerebral rSO_2 , data were analyzed as follows: first, all cerebral rSO_2 data points per patient were clustered in successive groups of 300 data points (30 minutes). For every group, a mean rSO_2 value was calculated. A relative difference of 5% between two subsequent data points was marked as an event. Second, cardiac rhythm and rSO_2 data were aligned. In case of an event identified in the cerebral rSO_2 data, the cardiac rhythm was

consulted to see if any arrhythmias occurred. In case of a cardiac arrhythmia, the lowest mean cerebral rSO_2 value was derived for the duration of the particular arrhythmia. Also a mean cerebral rSO_2 was derived from a 300 data point sample during normal sinus rhythm, resulting in a rhythm-specific mean cerebral rSO_2 per patient. When a difference of $\geq 5\%$ was found between the left and right cerebral hemisphere rSO_2 , values of both hemispheres were used for data presentation. In case of no difference between the left and right cerebral hemisphere, rSO_2 data were presented as one mean value for both hemispheres.

The effect of distal limb perfusion on limb tissue oxygenation was determined by comparison of mean rSO_2 values before (pre-event) and after (event) placement of a distal cannula in the femoral artery. Mean rSO_2 values were determined by averaging 300 data points before and after placement of the distal cannula. The latter sample was selected immediately following limb rSO_2 stabilisation. For comparison of tissue oxygenation values prior to (pre-event) and following (event) distal cannula clot removal, mean rSO_2 values were calculated in a similar fashion using 300 data points per sample.

To investigate the difference in cerebral desaturation between patients who did and did not suffer from neurologic complications, a mean cerebral rSO_2 was calculated for 30-minute intervals in both cerebral hemispheres for the entire duration of ECLS. A desaturation episode was defined as a mean unilateral cerebral rSO_2 below 50% over a period of 30 minutes. Consecutively, the sum of desaturation episodes was compared between patients with and without neurologic complications.

Statistical analysis

Numerical variables are depicted either in mean $\pm$ standard deviation or as median [interquartile range] depending on data distribution. Comparison of rSO_2 values between the different cardiac rhythms, pre-event samples and event samples was performed using the related samples Wilcoxon signed-rank test. A P-value <0.05 was considered statistically significant. All analyses were performed using the Statistical Package for Social Sciences version 22.0 (SPSS Inc., Chicago, IL, USA).

Results

Twenty-three adult patients assisted by femorofemoral VA-ECLS were included in this retrospective study. Mean age was 59 ± 13 years and a total of 18 females

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and 5 males were included. The median duration of ECLS support was 5 [1-20] days with a mean full ECLS pump flow of 4.5 ± 0.9 L/min.

Of the 23 patients, 16 were assisted by femorofemoral VA-ECLS upon resuscitation following an out-of-hospital cardiac arrest. Assistance by VA-ECLS was provided in three postcardiotomy cases. In the remaining four cases, life support was initiated following detection of, for example, pulmonary embolism. Distal cannulation was provided in six cases. Nine patients developed AF, whereas in three patients VF was observed. Development of abnormal cardiac rhythm was immediately followed by a decrease in mean rSO_2 from $61 \pm 11\%$ to $51 \pm 10\%$ during AF and from $67 \pm 9\%$ to 58 ± 10 during VF ($P < 0.001$ for both). No significant differences were found between the left and right cerebral hemisphere rSO_2 ($P = 0.750$). An example of a decrease in bifrontal cerebral rSO_2 during AF is shown in Figure 1.

In case of a presumably increased cardiac output resulting from myocardial recovery during full ECLS ($n=8$, mean flow 4.45 ± 0.6 L/min), a decrease in cerebral rSO_2 was observed from 73% to 54% and from 69% to 53% for the left and right cerebral hemisphere, respectively ($P = 0.012$ for both), as depicted in Table 1.

Table 1. Cerebral tissue oxygen saturation values in case of an im promptu increase in cardiac output while on extracorporeal life support.^{a,b}

		before increased CO	during increased CO	P-value
cerebral rSO_2 (%)	left	73 ± 7	54 ± 6	0.012
	right	69 ± 9	53 ± 8	0.012
arterial oxygen saturation (%)		99 ± 1	85 ± 8	0.028
arterial PO_2 (kPa)		15.6 ± 2.8	8.3 ± 1.9	0.012
pulse oximetry (%)		99 ± 1	97 ± 5	0.075
mean pressure (mmHg)		70 ± 7	80 ± 15	0.012

Abbreviations: CO, cardiac output; Left, left cerebral hemisphere; right, right cerebral hemisphere; rSO_2 , regional tissue oxygen saturation; PO_2 , partial gas pressure for oxygen.

^a $n=8$

^bValues presented as mean $\pm$ standard deviation.

Figure 1. Example of a decrease in bi-frontal cerebral oxygen saturation during consecutive periods of atrial fibrillation and sinus rhythm. AF, atrial fibrillation; ECLS, extracorporeal life support; rSO_2 , regional tissue oxygen saturation; rSO_2 -left, regional tissue oxygen saturation left cerebral hemisphere, rSO_2 -right, regional tissue oxygen saturation right hemisphere; SR, sinus rhythm.

Concomitant partial gas pressure for oxygen (PO_2) decreased from 15.6 ± 2.8 to 8.3 ± 1.9 kPa ($P=0.012$). Arterial saturation values derived from blood gas analyses showed a significant decrease from $99 \pm 1\%$ to $85 \pm 8\%$ ($P=0.028$), while pulse oximetry decreased from $99\% \pm 1\%$ to $97\% \pm 5\%$ ($P=0.075$). In Figure 2 the change in cerebral rSO_2 values is shown in case of a sudden increased cardiac output during ECLS without concomitant adjustment of ventilator settings. After approximately one hour, the ventilatory settings were adjusted, resulting in gradual rSO_2 normalization.

In the current study, a total of 11 patients (47.8%) died while on VA-ECLS due to neurologic complications, deep cardiogenic shock, sepsis, pneumonia, lung edema, myocarditis, multi-organ failure, or intestinal ischemic damage. The total number of cerebral desaturation episodes did not differ between patients who did or did not survive until ECLS weaning (19 versus 12 episodes, respectively, $p=0.695$). Five patients (21.7%) developed neurological complications while on VA-ECLS, which included intracerebral hematoma or extensive ischemic dam-

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age diagnosed with computed tomography imaging, critical illness neuropathy, and absence of the direct light pupil reflex.

Figure 2. Example of a decrease in bi-frontal cerebral tissue oxygen saturation with an im promptu increase in cardiac output during full extracorporeal life support. rSO_2 , regional tissue oxygen saturation; rSO_2 -left, regional tissue oxygen saturation left cerebral hemisphere; rSO_2 -right, regional tissue oxygen saturation right hemisphere.

Three out of five patients died due to the consequences of neurologic complications while in the remaining two cases one patient died due to lung edema and another survived weaning from ECLS. In the five patients with neurological complications, a median of 13 cerebral desaturation episodes (sum of left and right hemisphere) were observed, while in patients without neurological complications a median of 14.5 desaturation episodes were found ($P=1.000$). In patients with neurologic complications, the median number of desaturation episodes per day on VA-ECLS was 6.5, while the median number of desaturation episodes in patients without neurologic complications amounted to 3.0 ($P=0.914$).

Regarding tissue oximetry performed at the distal limb, rSO_2 values of the non-cannulated limb amounted to $65\pm6\%$ (mean value) and remained constant throughout the entire duration of ECLS. In six patients (26%), additional cannulation of the femoral artery proved necessary to ensure adequate blood flow to

the limb. Following insertion of a distal cannula in the femoral artery, limb rSO_2 increased from 29.3 ± 2.7 to 64.0 ± 5.1 ($P=0.027$) as shown in Table 2. An example of a limb rSO_2 pattern is provided in Figure 3.

Figure 3. Example of an increase in limb tissue oxygen saturation after restoring blood flow by inserting a distal cannula in the femoral artery. rSO_2 , regional tissue oxygen saturation; rSO_2 -left, regional tissue oxygen saturation left limb; rSO_2 -right, regional tissue oxygen saturation right limb.

Complications with distal cannulation of the femoral artery were observed in four patients (17.4%) following insertion of the distal cannula, including bleeding and thrombus formation. Due to clotting of the distal cannula, which was the most common complication associated with distal cannulation, limb rSO_2 values decreased (Table 2). Blood flow in the distal cannula restored following clot removal by aspiration using a syringe, as reflected by the increase in limb rSO_2 (from 31.3 ± 0.8 to 79.5 ± 9.0 , $P=0.068$). Furthermore, a decrease in temperature was noted in the cannulated limb. Notably, changes in limb temperature became evident after a clear time delay as compared to changes observed in limb rSO_2 (Figure 4).

All patients received PRBC transfusion or infusion of fluids (e.g., Ringer lactate and/or Gelofusin 4%). Transfusion of 38 PRBC units (275 mL per unit) for 13 anemic patients did not result in a significant change in cerebral rSO_2 . In contrast, rSO_2 levels increased $>10\%$ after infusion of >1000 mL of fluids within one hour ($P<0.001$, Table 3).

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Table 2: Restoring limb tissue oxygen saturation by inserting a distal cannula in the femoral artery (n=6) and clotting of the distal cannula (n=4).^a

patient #	limb rSO ₂ prior cannulation (%)	limb rSO ₂ post cannulation (%)	limb rSO ₂ clotted cannula (%)	limb rSO ₂ after clot removal (%)
4	24±2	63±3	32±3	66±4
5	28±1	60±3	31±2	89±5
10	32±2	70±4	-	-
11	30±1	59±2	30±1	86±1
16	31±2	72±2	-	-
28	31±3	60±5	32±2	77±3

Abbreviation: rSO₂, regional tissue oxygen saturation.

^aData presented as mean±standard deviation. rSO₂, regional tissue oxygen saturation. Difference between limb rSO₂ prior to distal cannulation and limb rSO₂ post cannulation (n=6): P=0.027. Difference between limb rSO₂ in case of a clotted distal cannula and limb rSO₂ after clot removal (n=4): P=0.068.

Table 3: Effect of transfusion of PRBC and fluid infusion on mean bi-frontal cerebral tissue oxygen saturation.^a

	pre transfusion	post transfusion	P-value
PRBC (n=13)	60±13	60±13	0.686
infusion <1000 mL fluids (n=11)	62±13	63±13	0.102
infusion >1000 mL fluids (n=10)	60±15	70±10	<0.001

Abbreviation: PRBC, packed red blood cells.

^aFluid infusion concerns Ringer lactate or Gelofusin. Data are presented as mean±standard deviation.

Figure 4. Example of a decrease in limb tissue oximetry values in case of a clotted distal cannula positioned in the left femoral artery. rSO₂, regional tissue oxygen saturation; rSO₂-left, regional tissue oxygen saturation left limb; rSO₂-right, regional tissue oxygen saturation right limb.

Discussion

This observational study focused on the application of continuous non-invasive tissue oximetry in patients supported by peripheral VA-ECLS. Our results showed cerebral and limb tissue oximetry readings adequately reflect both hemodynamic instability and compromised limb perfusion.

Fluctuations in mean arterial pressure, pulse oximetry values, arterial pO₂, and oxygen saturation reflect variations in cardiac output and are often the first signs of hemodynamic instability in patients on ECLS.^{11,12} Maintaining adequate cardiac output is important to prevent ischemic episodes, which can potentially result in complications such as congestive heart failure, neurocognitive impairment, renal dysfunction, infections, and irreversible multi-organ failure.¹²⁻¹⁶ A decreased cardiac performance resulting in lowered cardiac output has been associated with decreased cerebral and microvascular perfusion, which is reflected by lowered rSO₂ values.¹⁷ As a compensatory mechanism, brain oxygen extraction has shown to increase in case of reduced cardiac performance with concomitant lowered rSO₂.^{18,19} A possible cause of reduced cardiac perfor-

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mance can be an abnormal cardiac rhythm such as AF.²⁰ In the current study, AF was noted in nine patients, whereas in three patients VF was observed. Our results confirm that cerebral tissue oxygenation is lowered during episodes of AF and VF. These results indicate a high positive predictive value, suggesting that tissue oximetry can aid in timely recognition of hemodynamic instability in VA-ECLS patients, contributing to early detection of impaired cerebral perfusion.

Femoro-femoral cannulation is a common access technique for VA-ECLS procedures.²¹ A consequence of this cannulation method specifically is the development of so-called “differential hypoxia” or “isolated hypoxia” in the upper body.^{22,23} The phenomenon of differential hypoxia can be explained as follows: during full ECLS, the right heart is fully unloaded, the resultant lung circulation is minimal, and mechanical lung ventilation is reduced accordingly. If under these circumstances an increase in cardiac output occurs due to, for example, cardiac recovery, blood ejected by the left ventricle remains hypoxic as a result of the reduced ventilatory settings. Blood pumped by the ECLS system via the arterial femoral cannula retrograde into the aorta is fully saturated with oxygen and encounters the desaturated blood ejected by the left ventricle. When both blood flows meet in the near descending aorta, hypoxic blood will flow through the cervical arteries, whereas fully saturated blood will be diverted to, for example, the left subclavian artery. Subsequently, the brain suffers from an inadequate oxygen delivery, reflected by lowered cerebral rSO_2 .^{9,22,23} One may assume that the phenomenon of differential hypoxia occurred in eight of our patients in whom a presumably sudden increase in cardiac output occurred without timely adjustment of mechanical lung ventilation settings (Table 3). In line with this hypothesis, a significant decrease in cerebral rSO_2 and right radial artery pO_2 values were found, while pulse oximetry values (measured at the left index finger) remained unaffected. However, due to the retrospective nature of this study, this could not be confirmed by echocardiographic imaging. Nonetheless, these results suggest that cerebral oximetry enables early identification of differential hypoxia in patients on ECLS. When cardiac recovery is confirmed and a patient becomes candidate for weaning from ECLS, immediate adjustment of mechanical lung ventilation is warranted to prevent differential hypoxia and minimize the risk of neurological complications resulting from cerebral desaturation. The current results indicate that increased lung perfusion without accompanying adapting ventilator settings might be detected by careful (multimodal) monitoring with tissue oximetry. After multidisciplinary discussion, additional treatments might be planned such as fluid unloading or inotropic support to further improve myocardial and lung recovery. In addition, an observed decrease in rSO_2 may indicate an increased oxygen extraction and thereby a relative decrease in cer-

erebral perfusion, increasing the risk of poor neurologic outcome.²⁴ Future studies should therefore focus on neurological outcome of patients weaning from VA-ECLS.

The number of desaturation episodes did not differ between patients with or without a diagnosis of neurologic complications. Although this finding might seem contradictory, one must take into account that the evidence for a causal relationship between cerebral oximetry derived measurement values and neurologic outcome is still lacking.²⁵ Obviously, the development of neurologic complications is a very complex process and not in all cases reflected by clear reduction in rSO_2 values. One explanation can be found in the fact that the cerebral autoregulatory activity is not considered when measuring regional rSO_2 . In the case of cerebral hyperperfusion, for example, cerebral rSO_2 values may appear normal while the intrinsic neuroprotective mechanism of cerebral autoregulation is severely affected, predisposing the patient to an increased risk of neurologic complications.

Moreover, patients on VA-ECLS are subject to complex physiologic interactions including a whole-body inflammatory response, translating into high morbidity and mortality rates. This, in combination with the limitations inherent to the measurement technique of tissue oximetry using NIRS may be part of the explanation why a clear link between rSO_2 and clinical outcomes could not be established. Nevertheless, the results clearly indicate that cerebral tissue oximetry adequately reflects episodes of hemodynamic instability which is also a known factor contributing to postoperative morbidity and mortality.

A possible adverse effect of femoral cannulation is inadequate perfusion of the cannulated limb caused by occlusion of the femoral artery cannula. The limited antegrade flow in the distal artery is exacerbated due to delayed use of a distal artery perfusion cannula.²⁶ This may result in lower extremity ischemia, fasciotomy, or even limb amputation.²⁷ In the current practice, capillary refill as well as temperature and color of the limb are systematically evaluated for detection of ischemia. Changes in these parameters, however, are subjective with a possible risk of delayed intervention in the case of circulatory compromise. The current study showed that limb rSO_2 adequately reflected distal cannula clotting as well as restoration of blood flow (Figure 4). Hence, tissue oximetry aids in early recognition of compromised limb perfusion and contributes to timely intervention by identifying the need for an additional distal cannula. This exemplification underlines the clinical benefit of using noninvasive tissue oximetry in patients assisted by VA-ECLS.

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Packed red blood cell transfusion increases the oxygen content and improves tissue oxygen saturation.²⁸ Based on the fact that tissue oximetry enables rapid evaluation of tissue oxygenation, one can expect that transfusion of PRBCs result in an immediate increase in rSO_2 values.²⁸⁻³⁰ However, our data did not support this hypothesis. A possible explanation can be found in the critical hemodynamic conditions of our patients who received PRBC transfusion, since twelve patients suffered from severe bleeding. In this case, transfusion of RPBCs may have compensated for the decrease in cardiac output due to blood loss, resulting in a restored cardiac output and thereby preserving bi-frontal cerebral rSO_2 (Table 3). Another explanation for the lack of an increase in cerebral rSO_2 following PBRC transfusion can be found in the use of vasopressors, considering a study by Brassard et al. showing a decreased cerebral rSO_2 due to phenylephrine administration.³⁰ Nine of our patients received a relatively high dose of norepinephrine (1.94 $\mu\text{g/kg/min}$ at maximum) that could have led to a decrease in cerebral rSO_2 , masking the effect of PRBC transfusion on rSO_2 readings. The study of Brassard et al., in contrast, included young (26 ± 7 years) and healthy subjects. Our patients had co-morbidities including Q-fever, liver ischemia, pulmonary emboli, and an adenine nucleotide transporter deficiency. In addition, three patients in whom rSO_2 was unaffected by PRBC transfusion were diagnosed with either endocarditis or pericarditis. The limited effect of PRBC transfusion in infective patients has been described by Creteur et al. who attributed this effect to diminished microcirculation.³¹ Therefore, it remains debatable whether tissue oximetry is appropriate for assessing the effects of PRBC transfusion on tissue oxygenation in patients assisted by VA-ECLS. On the other hand, when fluid suppletion exceeded 1000 mL/h, cerebral rSO_2 did increase, which was most likely due to a concomitant increase in cardiac output together with timely adjustment of the ventilator settings.

One study limitation that needs to be considered when interpreting the current study results is the relatively small sample size. Despite this fact, the authors were able to show alterations in cerebral and limb rSO_2 as a reflection of changes in several patient-related factors including hemodynamic stability and limb perfusion. In addition, due to the retrospective design of the study, it was not possible to include data regarding blood flow in the distal perfusion cannulae and hemoglobin.

In conclusion, non-invasive tissue oximetry is a viable monitoring method for assessing cerebral and distal limb tissue perfusion in patients assisted by ECLS and should therefore be part of routine monitoring.

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CHAPTER 7

Vascular occlusion test to dynamically assess microcirculation during normothermic pulsatile cardiopulmonary bypass

NPA Vranken, YM Ganushchak, HM Willigers, JG Maessen, PW Weerwind

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Abstract

Objective: To evaluate parameters of the vascular occlusion test (VOT) before, during, and after pulsatile cardiopulmonary bypass (CPB).

Design: Prospective, observational study.

Setting: Single-center university hospital.

Participants: Adult patients undergoing elective cardiac surgery with pulsatile CPB.

Interventions: An oximeter sensor and adult-sized pneumatic tourniquet were positioned at the right forearm. A VOT with a predefined ischemic time of 3 minutes was performed before, during, and after CPB. Changes in tissue oxygen saturation were recorded.

Measurements and main Results: Thirty-four patients who underwent cardiac surgery were enrolled in the study. The lowest tissue oxygen saturation measured during the ischemic challenge differed between all 3 stages of surgery, with median values of 62.9% before, 57.5% during, and 59.3% after perfusion ($P<0.05$). Both occlusion ($P<0.001$) and reperfusion ($P<0.05$) slopes were steeper after bypass compared to before initiating bypass, whereas the reperfusion time remained constant between the different time points.

Conclusions: The microcirculatory function as demonstrated by changes in VOT parameters was enhanced during and after normothermic pulsatile CPB. Clinical relevance, however, needs to be further explored.

Introduction

Microvascular alterations after cardiac surgery with cardiopulmonary bypass (CPB) and impaired tissue oxygen saturation (S_tO_2) have been associated with adverse patient outcome.¹⁻⁵ Shear stress and contact with foreign surfaces cause transient microcirculatory dysfunction by activation of inflammatory and hemostatic systems.^{6,7} Tissue trauma and anesthesia also influence microcirculation,^{8,9} which may be aggravated by severe total blood volume shifts during surgery. Although the microcirculation is shown to be adversely affected by surgery with CPB¹⁰, monitoring of the microcirculatory function is still not part of routine practice. Continuous real-time monitoring may aid in early detection of tissue malperfusion. Measuring S_tO_2 using near-infrared spectroscopy with a reproducible ischemia-reperfusion challenge (ie, vascular occlusion test [VOT]) has shown to be a non-invasive method suitable for assessment of microcirculation.^{9,11,12} The VOT is an application in functional hemodynamic monitoring in which the response to an artificially induced ischemic stress can be followed. This method highly correlates to strain gauge plethysmography, which has been used extensively for measuring vascular function.^{13,14} Furthermore, to the best of the authors' knowledge, only a few reports combining near-infrared spectroscopy and VOT in patients undergoing nonpulsatile CPB have been published to date.^{9,15-17} On the other hand, pulsatile CPB has been shown to preserve microvascular function associated with improved patient outcome.^{2,18,19} Therefore, the aim of this study was to assess dynamic microcirculatory function using the VOT during cardiac surgery in patients undergoing pulsatile CPB.

Methods

Patients

After approval by the local ethical committee (reference number 1-4-087), a prospective explorative study was conducted. A total of 34 adult patients were included after they provided written informed consent. The inclusion criterion was elective cardiac surgery with CPB. Exclusion criteria were a body mass index $>30 \text{ kg/m}^2$, chronic advanced peripheral vascular disorders (including subclavian artery stenosis, Diabetes Mellitus, Raynaud's disease, and Raynaud's syndrome), a state of cardiogenic shock (emergency procedures), or patients diagnosed with New York Heart Association class IV.

Anesthesia

General anesthesia was induced using 0.5 to 1.0 $\mu\text{g/kg}$ of sufentanil (Hameln Pharmaceuticals, Hameln, Germany), 0.6 to 1.0 mg/kg rocuronium bromide

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(Fresenius Kabi Nederland, Zeist, The Netherlands), and 0.1 mg/kg of midazolam (Roche Nederland BV, Woerden, The Netherlands). After endotracheal intubation, patients were ventilated with volume-controlled ventilation with tidal volumes of 7 to 8 mL/kg and a positive end-expiratory pressure of 5 cmH₂O. The respiratory rate was adjusted to maintain normocapnia. Oxygen saturation measured from a pulse oximeter was maintained between 95 and 100%. Anesthesia was maintained with 0.5 to 0.8 minimum alveolar concentration of sevoflurane (AbbVie BV, Hoofddorp, The Netherlands) and continuous intravenous administration or boluses of sufentanil. During bypass, sevoflurane was replaced by infusion of 4 to 6 mg/kg/h of propofol (Fresenius Kabi), which was continued until patient arrival at the intensive care unit. Inotropes and vasoconstrictors were administered according to the hemodynamic status of the individual patient.

Patients were kept normothermic throughout the entire cardiac surgical procedure using a warming blanket (Bair Hugger 505; 3M Deutschland GmbH, Neuss, Germany).

Cardiopulmonary bypass

Target flow rates of ≥ 2.6 L/min/m² body surface area were maintained throughout normothermic (36.3°C) CPB. Pulsatile flow (radial artery pulse pressure ≥ 25 mmHg) was used only during the period of cross-clamping, with a frequency of 70 bpm, a base flow of 30%, and a pulse width of 50%. Mean arterial blood pressure (ABP) was maintained between 70 and 95 mmHg by titration of 0.4 mg/mL phenylephrine (pharmacy of Radboud UMC, Nijmegen, The Netherlands), if necessary. The sweep gas and fraction of inspired oxygen settings for the oxygenator were titrated to maintain normocapnia (partial pressure of carbon dioxide, 4.5 - 5.5 kPa) and normoxia (partial pressure of oxygen, 11.0 - 14.0 kPa). All patients received 2 mg of tranexamic acid (Pfizer BV, Capelle a/d IJssel, The Netherlands) during CPB. The transfusion trigger during CPB was set at a hematocrit level $< 25\%$.

Vascular occlusion test

The Fore-Sight tissue oximeter sensor (CAS Medical Systems Inc., Branford, CT) was used for assessing local tissue oxygen saturation, providing absolute S_tO₂ data, which was measured continuously. This device utilizes laser light of 4 different wavelengths (690, 780, 805, and 850 nm) to estimate the oxygen content.²⁰ A medium-sized sensor (emitter/diode spacing 15 and 40 mm for the first and second light path, respectively) was placed at the internal surface of the proximal third of the right forearm, and an adult-sized pneumatic tourniquet was positioned at the right brachial artery. After S_tO₂ signal stabilization ($< 2\%$ variation in 30 seconds), the cuff was inflated until pressure reached 30 mmHg

above the patient's systolic blood pressure. Inflation took 3 to 4 seconds after which the cuff was kept inflated for 3 minutes. Then the cuff was deflated rapidly (within 0.5 seconds), and the response in S_tO_2 was monitored. The VOT was performed at the following 3 predefined time points: after induction of anesthesia and prior to initiation of bypass (T_0), after initiation of bypass and aortic cross-clamping (T_1), and after termination of bypass (T_2).

Tissue oximetry readings were recorded and stored locally using the Fore-Sight oximeter before the data were transferred and saved in Microsoft Office Excel (Microsoft, Redmond, WA) format. The following VOT parameters were calculated: S_tO_2 before occlusion (%), occlusion slope ($S_tO_2\%/min$), lowest S_tO_2 in VOT (%), reperfusion slope ($S_tO_2\%/min$), reperfusion time (min), S_tO_2 at end of recovery (%), hyperemic area ($S_tO_2\%/min$), and S_tO_2 at end of hyperemia (%). As a baseline measurement for every VOT, S_tO_2 before occlusion was determined by calculating the average S_tO_2 over a 30-second interval prior to tourniquet inflation. Occlusion and reperfusion slopes were calculated over the entire slope between occlusion to the lowest S_tO_2 value in VOT and the complete slope between the lowest S_tO_2 value during occlusion and the first data point of S_tO_2 back at baseline level, respectively (Fig 1). After the reperfusion phase, the hyperemic area was determined using integration of the area under the curve (see Fig 1).

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Fig 1. Example of a vascular occlusion test performed in an individual patient.

1, start of the occlusion phase; 2, lowest oxygen saturation observed after 3 minutes of occlusion; 3, end of reperfusion phase; 4, hyperemic area; 5, end of hyperemic area where the oxygen saturation has reached pre-VOT values.

The occlusion slope was calculated as the change in oxygen saturation for the interval between data points 1 and 2 divided by 3 minutes. Time for recovery was calculated using the interval between data points 2 and 3. Calculating the reperfusion slope required dividing the change in oxygen saturation for the interval between data points 2 and 3 by the time for recovery. The hyperemic area was calculated as the area under the curve between datapoints 3 and 5.

S_tO_2 : tissue oxygen saturation.

Statistical analysis

Continuous variables are depicted as mean $\pm$ standard deviation or median (interquartile range) depending on data distribution. Statistical analysis was performed using the Statistical Package for Social Sciences, version 22.0 (IBM Corp, Armonk, NY). Distribution of data was tested using the Shapiro-Wilk test. To analyze for differences in VOT parameters before, during, and after CPB, the related-samples Friedman 2-way analysis of variance by ranks was computed. If statistically significant, the related-samples Wilcoxon signed rank test was performed to test pairwise comparisons. A P-value of <0.05 was considered statistically significant.

Results

Patient demographics and surgery-related variables are summarized in Table 1. In two patients no recognizable VOT curves could be obtained before and after perfusion; therefore, only data points at T_1 were taken into analysis for these patients. Intraoperative hemoglobin and ABP data are depicted in Table 2. Hemoglobin values differed significantly at every predefined time point and every other time point ($P<0.001$), with the lowest value recorded at T_1 (4.8 mmol/L). The median ABP was higher at both T_0 (83 mmHg, $p<0.001$) and T_2 (80 mmHg, $P=0.003$) compared with T_1 (69 mmHg).

VOT parameters at different time points are presented in Table 3. Values for S_tO_2 at the end of the occlusion phase the lowest at T_1 (57.5%). The occlusion slope was steeper at both T_1 (4.7%/min, $p<0.001$) and T_2 (5.1%/min, $P<0.001$) compared with T_0 (3.8%/min). Analyzing reperfusion slopes revealed a steeper slope at T_2 (36.8%/min) compared with T_0 (32.8%/min, $P<0.05$). Changes in S_tO_2 values prior, during, and after bypass are presented in Figure 2.

Table 1. Patient demographics and surgery-related variables.

demographic variables		
type of surgery	gender (F/M), n (%)	10(29.4%)/24(70.6%)
	age (years)	68.6 $\pm$ 10.7
	BMI (kg/m ²)	26.0 $\pm$ 3.5
	CABG	14 (41.2%)
	CABG+valve replacement	8 (23.5%)
	valve replacement	9 (26.5%)
	other*	3 (8.8%)
	CPB time (min)	82.0 (71.8-106.0)
	aortic occlusion time (min)	54.0 (49.5-75.0)

NOTE. Numerical values are depicted either as mean $\pm$ standard deviation or median (interquartile range), unless specified otherwise.

Abbreviations: BMI, body mass index; CABG, coronary artery bypass grafting; CPB, cardiopulmonary bypass.

*Other types of surgery include ascending aorta replacement with or without CABG or valve surgery.

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Table 2. Overview of perioperative hemoglobin and blood pressure data.

	T ₀ (n=32)	T ₁ (n=34)	T ₂ (n=32)
hemoglobin (mmol/L)*	8.5(7.8-9.0)	4.8 (4.1-5.4)	5.8 (5.2-6.6)
mean ABP (mmHg) ^{†,‡}	83 (76-94)	69 (62-76)	80 (71-92)
systolic pressure (mmHg) ^{†,§}	117 (101-132)	84 (76-93)	115 (107-126)
diastolic pressure (mmHg) [†]	62 (58-79)	56 (49-63)	60 (54-68)
pulse pressure (mmHg) ^{†,§}	53 (39-62)	26.9 (23-37)	54 (49-61)

NOTE. Numerical values are depicted as median (interquartile range).

Abbreviations: ABP, arterial blood pressure; T₀, before onset of bypass; T₁, during bypass; T₂, after cessation of bypass.

* Values all differ from each other (P<0.001).

† Difference between before and during perfusion (P<0.001).

‡ Difference between during and after perfusion (P=0.003).

§ Difference between during and after perfusion (P<0.001).

Table 3. Vascular occlusion test-derived parameters before, during, and after cardiopulmonary bypass.

	T ₀ (n=32)	T ₁ (n=34)	T ₂ (n=32)
S _t O ₂ before occlusion (%)*	76.4 (72.8-79.4)	74.1 (72.1-78.6)	76.2 (74.1-78.8)
occlusion slope (S _t O ₂ %/min) ^{†,‡}	3.8 (3.3-5.4)	4.7 (3.3-6.6)	5.1 (3.8-6.2)
lowest S _t O ₂ in VOT (%) ^{*,§,}	62.9 (55.8-68.6)	57.5 (53.1-64.3)	59.3 (53.2-66.2)
reperfusion slope (S _t O ₂ %/min)	32.8 (20.0-47.6)	35.3 (23.6-47.0)	36.8 (27.9-57.1)
reperfusion time (min)	0.43 ([0.33-0.49)	0.43 (0.33-0.51)	0.37 (0.32-0.52)
S _t O ₂ at end of recovery (%)	76.2 (72.3-78.6)	73.8 (71.0-77.2)	75.4 (74.1-77.2)
hyperemic area (S _t O ₂ %/min)	7.3 (3.6-14.3)	6.0 (4.7-8.7)	8.0 (5.1-9.9)
S _t O ₂ at end of hyperemia (%) ^{*,§}	76.3 (73.7-80.1)	74.0 (71.8-77.9)	77.0 (73.9-78.5)

Numerical values are depicted as median (interquartile range).

Abbreviations: T₀, before bypass; T₁, during bypass; T₂, after cessation of bypass; S_tO₂, tissue oxygen saturation; VOT, vascular occlusion test.

* Difference between T₁ and T₂; P<0.05.

† Difference between T₀ and T₁; P<0.01.

‡ Difference between T₀ and T₂; P<0.001.

§ Difference between T₀ and T₁; P<0.005.

|| Difference between T₀ and T₂; P<0.05.

Fig 2. Results of tissue oxygen saturation in the right forearm during the ischemic challenge before, during, and after bypass.

Median values were calculated from all 34 patients (32 during bypass). S_tO_2 , tissue oxygen saturation; T_0 , prior to bypass; T_1 , during bypass; T_2 , after cessation of bypass.

Discussion

Intraoperative monitoring of peripheral microvascular reactivity enables detection of alterations in microcirculatory function and thereby may contribute to preventing impaired tissue perfusion.^{3,4,17,21} This prospective study showed significant changes in VOT parameters between the different stages of cardiac surgery, implying altered vascular reactivity in patients undergoing cardiac surgery with CPB.

The occlusion slope (also referred to as the desaturation slope or rate of deoxygenation) is one of the parameters that reflects the current state of microcirculation and ought to represent the rate of mitochondrial oxygen consumption and local tissue metabolism.²² A steeper occlusion slope therefore would be indicative of a relatively high local metabolic rate, as reflected by the rapid local decrease in oxyhemoglobin concentration. The results of this study showed a significantly steeper occlusion slope at both T_1 and T_2 compared to T_0 , indicating increased oxygen consumption during and after CPB compared with before initiation of CPB. This effect has been previously described and represents the effect of general anesthesia with propofol on oxygen delivery and extraction as well as capillary blood flow.^{9,23-25} Contrastingly, Smith et al. found the occlusion

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slope to be similar across different stages of surgery,¹⁷ which may be explained partially by methodologic differences that consequently affect the values of VOT-derived parameters. For example, their study did not apply any exclusion criteria, such as Raynaud's disease, which may logically may affect S_tO_2 .

Another VOT-derived parameter is the lowest value found during the ischemic period, which provides information regarding the absolute oxygen reserve in the microcirculatory system. The observed decline in the lowest S_tO_2 value at T_1 suggested that the absolute oxygen reserve was affected during perfusion, probably in part due to hemodilution. This also was reflected by the decreased hemoglobin values during bypass (see Table 2).

Since the time required for recovery did not change, it can be speculated that perfusion recovery occurred in a more efficient manner while the patient was on bypass. This observed effect can be attributed to an increased blood flow velocity in minor hemodilution by a decrease in systemic vascular resistance.²⁶⁻²⁷ In addition, reduced blood viscosity adds to the increase in blood flow in the capillaries and thereby compensates for the effect of dilution, contributing to maintaining adequate tissue oxygenation.²⁷

The reperfusion slope (also referred to as the recovery slope or rate of reperfusion) represents the time required to wash out stagnant blood from the microvasculature and the local reperfusion reserve.^{9,22} Our results did show an increased reperfusion slope at T_2 compared to T_0 , suggesting altered peripheral microvascular reactivity. The duration of reperfusion remained unchanged, possibly indicating enhanced reperfusion efficiency. It has been proposed that the reperfusion slope is directly proportional to tissue perfusion while that reperfusion time is inversely proportional to tissue perfusion.¹¹ Therefore, it can be speculated that the observed changes reflect an enhanced tissue perfusion when the patient is on bypass. Hence, our results could not confirm that CPB worsens microcirculatory function. Smith et al., in contrast, reported a decreased reperfusion slope at T_1 compared with T_0 , implying impaired peripheral microvascular reactivity.¹⁷ They also found a successive decline in reperfusion slopes with increasing duration of CPB, denoting worsened microcirculatory function. Possible factors contributing to these discrepancies are measurement site and CPB protocol. S_tO_2 measurements in the study presented here were performed at the internal surface of the forearm, which may result in different values for VOT-derived parameters compared with positioning the measurement probes at the thenar eminence.

Another VOT-derived parameter considered to reflect vascular reactivity is the hyperemic area,^{4,17} which is reflective of tissue oxygen consumption.²⁸ Dorschug et al. reported a significantly lowered reactive hyperemic response in

septic patients and attributed this finding to a dysregulated microvascular oxygen balance.²⁸ In the current study, the hyperemic area did not differ between time points, which was in concordance with previous studies and adds to the notion of preserved peripheral microcirculation during and after CPB.^{9,17}

Discrepancies between previously published studies and the results of this study could be the result of differences in the ischemic challenge protocol. The choice of probe, probe positioning, and duration of ischemia affect the values of VOT-derived parameters.²⁹ However, a standardized protocol of VOT is not yet established. One method is the application of a fixed target S_tO_2 for termination of the ischemic period (absolute value for S_tO_2 of 40%).⁹ Because a target tissue saturation level may be difficult to reach due to decreased metabolic rate and increased oxygen content during surgery, the study presented here used a fixed interval of 3 minutes occlusion time, similar to another study.¹⁷ Moreover, position of sensors and probe spacing affect the values of VOT-derived parameters. It was described previously that baseline as well as reperfusion and occlusion slopes were affected by probe placement.²⁹ Both this study and the study by Smith et al. used medium-sized probes placed on the brachial artery.¹⁷ Previous studies report VOT protocols with placement of oximetry sensors at either the forearm or the thenar eminence.^{9,15-17} However, S_tO_2 measured at the thenar muscle may be subject to the body-finger temperature difference in a larger extent than S_tO_2 measured at the forearm.³⁰ Inconsistent probe sizing and placement in prior studies make interpretation and comparison of data challenging, and future studies therefore should aim at developing a standardized protocol.

Another source of variation in the reported results could be differences in calculation methods. For example, in the study presented here, data of the entire downward slope were used for calculation of the desaturation slope, whereas others selected a 1-minute interval commencing with S_tO_2 decreasing below baseline¹⁷ or defined the occlusion slope as the first 25% of S_tO_2 descent.⁹ Regarding the reperfusion slope, other studies used either solely S_tO_2 values from the first 14 seconds of reperfusion,⁴ values from the release of occlusion to 85% S_tO_2 recovery,¹⁷ or values of the entire reperfusion interval, similar to this study.⁹

Although differences in protocol apparently influence the values of VOT-derived parameters, it is unlikely that the observed changes between the different phases of surgery are affected. Nonetheless, it remains unclear whether these differences significantly contribute to the seemingly opposite physiologic effects described in published reports, underlining the importance of standardizing the VOT in future research. In addition, both baseline and dynamic VOT parameters may be affected by patient-related factors, including differences in subcutane-

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ous adipose tissue depth.^{31,32} High interindividual variability makes comparison among patients challenging, hence the study presented here focussed on differences between time points.

The influence of propofol on the microcirculatory responsiveness and metabolic rate was precluded in the analysis, which potentially could influence VOT results.^{9,23-25} However, in the study presented here, the focus predominately was on the effect of CPB rather than the anesthesia protocol. In addition, the use of an α 1-antagonist (eg, phenylephrine) also may affect VOT-derived parameters because it causes vasoconstriction, thereby reducing capillary blood flow. In the study presented here, however, the administered dose of phenylephrine was considerably lower compared with the study by Maier et al. that described the effects of phenylephrine on sublingual microcirculation in patients undergoing CPB.³³ Therefore, it may be assumed that the effects of phenylephrine on the microcirculation in the current study were limited.

Conclusion

The microcirculatory function as demonstrated by changes in VOT parameters was enhanced during and after normothermic pulsatile CPB. Clinical relevance, however, needs to be further explored.

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Non-invasive tissue oximetry following unilateral DIEP-flap reconstruction: a pilot evaluation

NPA Vranken, PW Weerwind, MA van Onna, EAC Bouman, RRWJ van der Hulst

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Abstract

Introduction: Post-operative monitoring of a free flap transplant in the form of a deep inferior epigastric perforator flap (DIEP-flap) is crucial for early detection of vascular compromise. The aim of the current study, therefore, is to gain insight whether non-invasive tissue oximetry is suitable for assessment of tissue perfusion following DIEP-flap surgery and whether it can serve as an early marker for vascular compromise.

Methods: Patients (n=29) undergoing secondary unilateral DIEP-flap surgery were included in this prospective explorative study. Non-invasive tissue oxygen saturation (StO₂) measurements were performed using one sensor positioned on the DIEP-flap and another positioned on the native breast. Measurements were performed directly after the surgical procedure until 24 h post-operatively.

Results: Tissue oxygenation response was swift in the native breast (on average 11.9%/h for 84 min, n=28), whereas the DIEP-flap showed a lower and more extended tissue recovery phase of approximately 7.5%/h for 6 h (n=23). In some of these latter cases (n=14), an acute and second more prolonged response was observed in the DIEP-flap. The average difference between the DIEP-flap and native breast StO₂ was 4% across the entire measurement (P=0.043). Two patients underwent post-operative re-exploration of the DIEP-flap, in which an immediate and constant enlarged difference between DIEP-flap and native breast StO₂ ($\geq 38\%$), and a decreased DIEP-flap StO₂ ($\leq 43\%$) was observed.

Conclusion: Continuous non-invasive tissue oxygen saturation is suitable for postoperative monitoring of DIEP-flaps, and StO₂ pattern may aid in early identification of vascular compromise in DIEP-flaps.

Introduction

Increasing awareness of complications associated with silicone breast implants (haematomas, infections, sensory changes, peri-implant capsule formation/contraction and implant perforation or contracture) has generated high interest in breast reconstruction following mastectomy using solely autologous tissue.¹ Success or failure of a particular free skin transplant, however, is dependent on continuous arterial and venous outflow through patent microvascular anastomoses.² Therefore, postoperative monitoring of a DIEP-flap is crucial for early detection of vascular compromise to maximise chances of flap salvage.³ Loss of free flaps due to vascular compromise is a detrimental complication and has been reported to occur in 3.6-6% of cases, while re-exploration is performed in 5-25% of cases.^{4,5}

In daily practices, clinical observation of skin colour, temperature and capillary refill are used to assess flap perfusion and viability, as well as results obtained by Doppler ultrasonography.⁶ However, these monitoring methods are only performed intermittently and are rather subjective, relying on the experience of the evaluator. Additionally, the results of a literature review conducted by Smit and colleagues implicate that solely performing clinical evaluation for postoperative flap monitoring is unfavourable due to the time needed for clinical signs to become evident.⁷

Non-invasive tissue oximetry using near-infrared spectroscopy (NIRS) is a method that could be used for continuous monitoring of tissue perfusion in free skin flaps. Previous studies suggest that tissue oximetry is capable of early detection of tissue hypoxia in free skin flaps.^{3,8-10} However, these studies only performed unilateral tissue oxygenation measurements. In the current study, tissue oxygen saturation (StO₂) is monitored simultaneously in the DIEP-flap and native breast (personalised reference value). The present study aims to gain insight in whether non-invasive tissue oximetry is suitable for assessment of tissue perfusion following reconstructive breast surgery with a DIEP-flap and if bilateral tissue oximetry values can potentially serve as an early marker for vascular compromise.

Materials and methods

Patients

Female patients undergoing unilateral secondary DIEP-flap surgery were included in this prospective explorative study. A prerequisite was a DIEP-flap

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dimension of at least 50 mm x 85 mm, to allow proper sensor placement. Primary DIEP-flap procedures were not included because the abdominal skin island on the breast is smaller following a primary procedure as compared to a secondary procedure. An exclusion criterion for this study was objection in the patient hospital records against consultation of patient and surgery-related information for research or educational purposes. Data acquisition and analyses for this explorative study were performed anonymously and in accordance with the Dutch law for approving medical research.

Measurements

Non-invasive tissue oximetry uses NIRS based on the Lambert-Beer law. In short, light of several wavelengths within the near-infrared spectrum is absorbed by chromophores in an oxygen-dependent manner.^{5,11} Characteristic absorption spectra of the chromophores oxyhaemoglobin and deoxyhaemoglobin allow estimation of their concentrations after measuring the optical signals exiting the tissue.¹² The ratio of oxygenated haemoglobin relative to the total local concentration of deoxygenated haemoglobin is then used to quantify the oxygen content in local tissue.^{5,11,12}

In our study, non-invasive tissue oxygenation monitoring was performed using the INVOS 5000C Oximeter (Somanetics Corporation, Troy, Michigan, USA). One self-adhesive disposable NIRS sensor (INVOS SAFB-SM Adult SomaSensor) was positioned on the DIEP-flap below the staple markings and served to measure the Doppler flow on the lower medial site of the flap. The other sensor was positioned on the lower side of the native breast right below the areola and served as a personalised reference value. Since revisions of the anastomoses are mostly performed in the first critical hours following surgery^{3,13}, tissue oximetry readings were initiated directly after completion of the surgical procedure and continued until 24 hours postoperatively at the ward. Protocolled transfer of the patient from the operating theater to the recovery room was accommodated after adequate blood flow identification by Doppler ultrasonography.

Flap weight, ischaemia time and postoperative complications emerging before hospital discharge were recorded. Post-operative complications were defined as circulatory failure at the recipient site (DIEP-flap) requiring immediate return to the operating room for re-exploration.

Statistical analysis

For the a priori sample size calculation a 10% difference in StO₂ was considered a relevant change, considering the inaccuracy of the INVOS 5000C clinical oximeter of 4.7%. With an α set at 0.05, a statistical power ($1-\beta$) of 0.95, and σ

of 13.75 (maximum - minimum divided by 4, i.e., 99-44/4), the estimated sample size amounted to 28 patients.

Data were analysed according to the absolute tissue oxygen saturation difference (ΔStO_2 , depicted in %) between the DIEP-flap and the native breast. Numerical values are expressed as mean $\pm$ standard deviation. Depending on data distribution, either a paired t-test or Wilcoxon signed-rank test was used for comparison of DIEP and native breast StO_2 .

Results

From a practical point of view, a total of 29 patients were included in the study. The mean age and body mass index were 50 ± 10 years and 26.3 ± 3.3 kg/m², respectively. The ischaemia time varied from 23 to 75 min (mean 48 ± 12 min) and the weight of the transplant varied from 250 to 1324 g (mean 645 ± 237 g). On average, StO_2 of the native breast amounted to $85 \pm 3\%$ in the first 24 h post-operatively, whereas StO_2 measured in the DIEP-flap was significantly lower, amounting to $81 \pm 4\%$ (Wilcoxon signed-rank test, $P=0.043$) (Table 1).

Table 1. Study population characteristics.

	n=29	case 1	case 2
age (y)	50 ± 10	52	61
BMI (kg/m ²)	26.4 ± 3.3	30.0	23.5
weight DIEP-flap (g)	649 ± 240	1000	688
ischemia time DIEP-flap (min)	48 ± 12	60	37
mean StO_2 DIEP-flap (%)*	81 ± 4	43 ± 0	44 ± 1
mean StO_2 native breast (%)	85 ± 3	86 ± 4	82 ± 2

BMI: body mass index, DIEP flap: deep inferior epigastric perforator-flap, StO_2 : tissue oxygen saturation. *P-value for comparison of the mean StO_2 DIEP-flap and mean StO_2 native breast: $P=0.043$ (Wilcoxon signed-rank test).

In the majority of patients, a rapid post-surgical tissue oxygenation response was noted in the native breast, amounting to 11.9%/hour for 84 min (mean values for 28 patients). One patient lacked an identifiable tissue response, showing stable StO_2 values throughout the entire measurement duration. Following tissue oxygenation recovery, native breast StO_2 values remained constant ($85.9 \pm 7\%$). The DIEP-flap, on the other hand, showed a more extended tissue oxygenation response of 7.5%/h for 6 h (mean value for 23 patients). In some of

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these patients (n=14), an acute and second more prolonged tissue response could be identified (Graph 1). In those cases, a slope of 12.8%/h was observed in the DIEP-flap immediately after initiation of the measurement for 71 min (mean value), while the second and more prolonged recovery slope amounted to 6.9%/h for 165 min (mean value). After tissue oxygenation recovery, DIEP-flap StO_2 values remained stable ($81.8 \pm 12\%$). In one individual patient with the shortest ischaemia time observed (23 minutes), DIEP-flap and native breast StO_2 showed very similar values throughout the entire measurement (Graph 2). In 6 of 29 patients, no clear tissue oxygenation recovery could be identified as tissue oximetry values obtained from the DIEP-flap remained relatively similar throughout the measurement. In three of these patients, DIEP-flap and native breast StO_2 also consistently showed comparable values (absolute $\Delta\text{StO}_2 \leq 10\%$ throughout the entire measurement duration).

Graph 1. Tissue oximetry readings of an individual patient with an uncomplicated postoperative recovery. 1. Acute tissue oxygenation recovery phase, 2. Second prolonged tissue oxygenation recovery phase. DIEP: deep inferior epigastric perforator, REF: internal reference measurement, StO_2 : tissue oxygen saturation.

Graph 2. Tissue oximetry readings from a patient with the shortest observed ischemia time (23 minutes). DIEP: deep inferior epigastric perforator, REF: internal reference measurement, StO₂: tissue oxygen saturation.

Most patients showed an uncomplicated postoperative course and were discharged from the hospital after 5 days. In two patients (7%), however, re-exploration of the DIEP-flap was performed within 24 h following clinical signs of vascular compromise and aberrant results obtained by Doppler ultrasonography. An immediate and constant enlarged ΔStO_2 (on average 43%) and decreased DIEP-flap StO₂ (43%) was observed in case 1 (Table 1, Graph 3), which could be explained by a non-patent anastomosis. In this particular patient, the epigastric perforators were anastomosed to the thoracodorsal vessels after failure to locate the internal mammary vessels. A second anastomosis was performed to ensure sufficient tissue perfusion and DIEP-flap salvage. In another patient experiencing postoperative re-exploration, similar ΔStO_2 values (on average 38%) and decreased DIEP-flap StO₂ (44%) were noted (Table 1, Graph 4). In case 2, re-exploration of the DIEP-flap was performed within 24 h because of vascular compromise that was suspected based on flap discolouration; however, an evident circulatory defect could not be identified. On the fifth postoperative day, partial necrosis on one side of the DIEP-flap was sensed as palpable firmness identified by physical examination.

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Graph 3. Case 1: Tissue oximetry readings from a patient with a non-patent anastomosis. DIEP: deep inferior epigastric perforator, REF: internal reference measurement, StO₂: tissue oxygen saturation.

Graph 4. Case 2: Tissue oximetry readings from a patient complicated with partial fat necrosis of the DIEP-flap observed on the fifth postoperative day. DIEP: deep inferior epigastric perforator, REF: internal reference measurement, StO₂: tissue oxygen saturation. Due to dislodgement of measurement probes, data was lost between the 3rd and 20th postoperative hour.

Discussion

This explorative clinical study identified several patterns of tissue oximetry readings in the first 24 h following unilateral secondary DIEP-flap surgery. Most patients showed a gradual recovery of DIEP-flap tissue oxygenation. To the best of our knowledge, this is the first study linking tissue oximetry readings including a personalised reference value to clinical outcome following DIEP-flap surgery.

Although most patients showed a subtle or more pronounced tissue response in the DIEP-flap, some patients showed relatively stable tissue oxygenation values throughout the measurement. Possibly in the latter group of patients (n=6) the tissue response did not exceed the threshold of a detectable StO_2 change. In three of these patients, DIEP-flap StO_2 did not only lack an identifiable recovery slope but also showed comparable values to the native breast StO_2 throughout the entire measurement ($\leq 10\%$ absolute difference). A possible explanation for these findings is that in this group of patients, DIEP-flap StO_2 recovery had already occurred prior to initiation of the measurement.

Following flap elevation, primary ischaemia begins whenever the vascular pedicle is transected - in this case, the vessel responsible for perfusion of the DIEP-flap. When the anastomosis is completed and vascular clamps are removed, the initial reperfusion phase starts. Generally, an increased ischaemia time leads to a decreased survival rate of free skin flaps; therefore, one may expect the chance of vascular compromise to be increased with a prolonged ischaemia time.¹⁴ However, our results do not reflect this statement, as the re-explored DIEP-flaps underwent an ischaemia time of 37 and 60 min, which is within the range of the mean value $\pm$ one standard deviation (36-60 min, Table 1). One could therefore hypothesise that in the studied cases, the ischaemia time was too short to contribute to impaired postoperative tissue recovery.

In total, 2 out of 29 studied patients underwent re-exploration of the DIEP-flap. In case 1, the anastomosis was insufficient to adequately perfuse the entire DIEP-flap, which was reflected by a ΔStO_2 of 43% and a DIEP-flap StO_2 of 43%. More specifically, an inadequate venous outflow resulted in venous congestion of the DIEP-flap. In contrast, in case 2 no evident cause for impaired tissue perfusion could be identified. Preceding partial necrosis noted on the fifth postoperative day, a consistently lowered StO_2 concomitant with an increased ΔStO_2 was measured in the DIEP-flap of this particular patient. These results imply that both an enlarged ΔStO_2 ($\geq 38\%$) and decreased StO_2 measured in the DIEP-flap ($\leq 43\%$) are indicative of inadequate flap perfusion. In both patients, an increased ΔStO_2 as well as a decreased DIEP-flap StO_2 were observed im-

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mediately after initiation of the measurement, suggesting that tissue oximetry was capable of providing an early warning of impaired tissue perfusion.

Nevertheless, when determining a clear StO_2 or ΔStO_2 threshold necessitating prompt intervention, it is important to consider the limitations of tissue oximetry. Clinical oximeter devices are destined for either trend or absolute StO_2 monitoring, as they use an algorithm which requires the assumption of a fixed ratio of arterial to venous blood in the vascular bed. This algorithm, however, cannot adapt to all possible applications of tissue oximetry. Hence, one must be cautious when interpreting absolute StO_2 values derived from measurements performed in different areas. When interpreting the current results, it is important to consider the fact that DIEP-flap and personalized reference StO_2 reflect the oxygen balance in different types of tissue. Therefore, it can be expected that absolute values derived from both measurements (native breast tissue and abdominal wall tissue) differ to a certain extent, although in the vast majority of patients, the absolute ΔStO_2 was $\leq 10\%$ after tissue oxygenation recovery. This latter suggests that comparison of DIEP-flap and native breast StO_2 is of added value in patients with vascular compromise.

Additional factors to take into account when establishing StO_2 thresholds are the clinical oximeter device and type of sensor used. Previous studies used different oximeter devices and NIRS sensors, which makes comparison of study results challenging. In a study by Hyttel-Sorensen and colleagues, three different oximeters were compared.¹⁵ They found differences in median absolute values, repeatability and dynamic measurements across the different devices, underlining the importance of standardised application of tissue oximetry. Additionally, tissue oxygen saturation values are not only dependent on sensor positioning but are also affected by near-infrared transmitter-receiver spacing, which may vary between sensor types.¹⁶ The current study used sensors with an estimated depth of measurement of 20 mm, while other studies used oximeters with varying measurement depths of 0-5 mm¹³, 4-6 mm⁸, or more similar to our study, up to approximately 23 mm.³ Different monitoring devices also use varying numbers and wavelengths of near-infrared light, which also affects estimation and calculation of StO_2 .¹⁷

Conclusion

Continuous non-invasive tissue oxygen saturation patterns may aid in early identification of vascular compromise following DIEP-flap surgery. Future studies should aim at establishing clinically relevant tissue oxygenation thresholds.

Conflict of interest statement

None declared.

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General discussion

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A number of different technologies have been developed to measure tissue oxygenation with the goal of identifying tissue hypoxia and guiding therapy to optimize end-organ tissue oxygenation, to ultimately, prevent ischemic tissue damage. In specific cases, tissue oximetry may indicate decreased tissue oxygenation such as that occurring during acute brain ischemia. However, the causation between tissue hemoglobin-oxygen desaturation in one organ (e.g., brain or muscle) and global outcomes such as mortality, intensive care unit length of stay, and remote organ dysfunction remains speculative. In this thesis, the current state of evidence for predicting clinical outcomes from tissue oximetry is described and several issues that need to be addressed to clarify the link between tissue oxygenation and outcomes are identified. The analysis finds that despite the increasing amount of literature focusing on the application of tissue oximetry, the association between desaturation episodes and clinical outcomes remains assumptive. Major lacunae include clinically relevant threshold or prediction values for tissue desaturation-related injury in specific organs. Furthermore, defining the types of required interventions to correct changes in tissue oxygenation and defining the effect of these interventions on clinical outcomes is warranted.

Tissue oximetry for brain monitoring

Neurological complications following cardiac surgical interventions are among the most detrimental adverse outcomes, affecting 1.5-11% of the patient population.¹⁻³ Several studies elaborated on the factors that play a role in the obviously multifactorial development of neurological complications. Regional tissue oxygen saturation (rSO_2) reflects the balance between arterial oxygen supply and demand in real-time, thus a decrease in oxygen supply or increase in oxygen extraction by metabolic demand in tissue results in a decrease in tissue oximetry readings.⁴ In essence, rSO_2 is thought to reflect the local venous oxygen reserve, indicating that any factor that modulates either oxygen supply, oxygen extraction ratio, or both (e.g., anesthetics or cerebrovascular dysfunction) directly affects cerebral rSO_2 . Cerebral oximetry, however, does not provide any information regarding the cause of a changing rSO_2 , thus it remains unknown whether the rSO_2 changes are attributable to modifiable factors or not. Although several observational and few experimental studies conclude that continuous brain monitoring using near-infrared spectroscopy (NIRS) is a viable method for early detection of cerebral hypoxia, proof for a clear link between cerebral rSO_2 and postoperative neurologic complications (PNC) is still lacking. As discussed in Chapter 2, this can be partially explained by the fact that tissue oximetry, due to its measurement principle, is unable to take the intrinsic auto-

regulatory activity of the cerebral vasculature into account. This is illustrated by the observation of seemingly normal cerebral rSO_2 values during cerebral hyperperfusion (i.e., “brain luxury perfusion”), while the cerebral autoregulatory activity is impeded.⁵ Cerebral autoregulation (CA) is known to be intact within a certain range of physiologic cerebral perfusion pressures, and prevents both hypoxia and hyperoxia. The autonomous cerebral protective system prevents hyper- and hypoperfusion by continuous control and modification of cerebrovascular resistance, assuring constant cerebral blood flow. Consequently, impaired CA permits fluctuations in cerebral perfusion pressure which may result in either brain hyper- or hypoperfusion, predisposing the patient to an increased PNC risk. Rather than solely focusing on preserving cerebral rSO_2 within certain predefined limits, maintaining intact CA should be of primary importance in minimizing PNC risk. The clinical relevance of statistically significant decreasing rSO_2 values requires further elucidation, therefore it remains of utmost importance to take all available clinical information into account when interpreting rSO_2 readings.

One factor contributing to the lack of evidence on the association between cerebral rSO_2 and PNC may be the different perfusion protocols applied across studies. As indicated by Ganushchak et al.⁶, the cardiopulmonary bypass (CPB) technique affects PNC risk through variations in hemodynamic parameters such as mean arterial pressure, systemic vascular resistance, and arterial pulse pressure. Moreover, a prospective study by Ševerdija et al. clearly illustrated that the levels of arterial carbon dioxide level and the extent of hemodilution need to be controlled within a certain range to enable optimal cerebrovascular reactivity and thus intact CA.⁷ The primary requisite for intact CA is a mean arterial blood pressure (ABP) within the lower and upper autoregulatory limit, which are reported to lie around 60 and 150 mmHg, respectively.⁸ These values, however, are subject to interpersonal variations, for example differences in sympathetic nervous activity, as is the case in chronic hypertension.⁹ In clinical practice, this may pose a challenge to warrant CA integrity based on preoperative measurements. Besides intraoperative ABP, arterial partial gas pressure of carbon dioxide also needs to be maintained at predetermined levels to enable sufficient autoregulatory activity (Chapter 3). Moreover, maintaining stable hemodynamics during CPB will contribute to lowering the PNC risk.⁶ Therefore, standardization in the form of strictly regulating patients’ hemodynamics between the anticipated autoregulatory limits will contribute to preservation of CA (Chapter 4). Ultimately, this will aid in decreasing the PNC incidence in surgical patients by avoiding unnecessary exposure to CA disturbances.

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Despite the shortcomings of cerebral oximetry inherent to its measurement technique, rSO_2 readings can still serve as an additional source of information regarding the current balance between oxygen delivery and consumption. In Chapter 5, we showed that cerebral oximetry effectively reflects tissue oxygenation changes resulting from several iatrogenic events in cardiac surgical patients. Onset of CPB and placement and removal of the aortic cross-clamp were events that resulted in a decreased rSO_2 , whereas anesthetic induction, placement of the sternal retractor and termination of CPB were associated with an increase in rSO_2 . We also illustrated that phenylephrine administration has no relevant effects on cerebral oxygen saturation. This observation is in contrast with the findings of an interventional study by Moerman et al., who concluded that cerebral rSO_2 decreases following phenylephrine infusion.¹⁰ The authors hypothesized that this effect was a functional myogenic response, part of cerebral autoregulatory activity. The reported changes in rSO_2 in their publication were statistically significant, but only very small in magnitude (on average 1.8%). It is therefore unlikely that vasopressor (e.g., phenylephrine) administration has clinically relevant effects with regards to cerebral tissue perfusion. A previous study by Brassard and colleagues¹¹ did show a decrease in cerebral tissue oxygenation following phenylephrine administration, however, this effect was exclusively observed in a specific subset of patients (diabetics) included in the study. The proposed negative effect of phenylephrine on cerebral rSO_2 is, therefore, probably not of any clinical importance in non-diabetic patients. In addition, Chapter 5 illustrates that cerebral oximetry using NIRS is sensitive enough to detect subtle and potentially relevant changes in rSO_2 through several stages of CPB. Nonetheless, further clinical studies are warranted to investigate the relationship between subtle and pronounced cerebral desaturations identified by cerebral oximetry and PNC.

Tissue oximetry may also be helpful in continuous assessment of tissue perfusion in patients undergoing long-term cardiopulmonary support, such as veno-arterial extracorporeal life support (VA-ECLS). Maintaining adequate cardiac output is especially important in VA-ECLS patients in order to prevent ischemic episodes which can potentially result in cerebral and microvascular malperfusion, contributing to the risk of complications including PNC, congestive heart failure, renal dysfunction, infections, and irreversible multi-organ failure.^{6,12-15} Hemodynamic instability is reflected by fluctuations in oxygen saturation and could thus be identified by tissue oximetry. In a retrospective study, we identified several events which were related to significant changes in cerebral rSO_2 (Chapter 6). The analysis showed that cardiac arrhythmias (i.e., atrial fibrillation or ventricular fibrillation) cause a decrease in bi-frontal cerebral rSO_2 (both the

left and the right cerebral hemisphere), most probably as a result of hemodynamic instability.

Another event that manifested in a clear rSO_2 decrease was the occurrence of a presumably sudden change in cardiac output without timely adjustment of the ventilator settings. These results indicate that tissue oximetry can aid in timely recognition of hemodynamic instability, contributing to early detection of impaired cerebral perfusion.

Surprisingly, administration of packed red blood cells (PRBC) did not cause a significant change in cerebral rSO_2 readings. One might expect that allogeneic blood transfusion would cause an increase in rSO_2 values due to its effect on oxygen carrying capacity and cardiac output. Part of the explanation for this seemingly contradictory finding can be found in the critical hemodynamic conditions of the patients receiving PRBC transfusion. In our study, some patients suffered from severe bleeding, which most likely caused blood transfusion to have had a compensatory effect on the decreased cardiac output. This, in turn, resulted in restoration of cardiac output, and thereby preservation of cerebral rSO_2 rather than an increased value.

The study results advocate for the application of non-invasive tissue oximetry as a viable monitoring method for assessing cerebral tissue oxygenation during ECLS. Although direct interpretation of measurement values continues to be challenging due to the lack of application-specific rSO_2 thresholds, inclusion of tissue oximetry in routine bedside monitoring could aid in early recognition of threats to hemodynamic stability.

Tissue oximetry for somatic monitoring

Besides the originally intended use of tissue oximetry (brain monitoring), several other clinical applications have been described in the literature. The two most commonly used oximeter devices (Fore-Sight Elite, CAS Medical Systems, Inc., Branford, CT, USA and INVOS 5100C, Medtronic, Minneapolis, MN, USA) provide the option to simultaneously measure cerebral and somatic tissue oxygen saturation with an adapted algorithm for the calculation of local oxygen content in muscle tissue.

Patients undergoing long-term cardiopulmonary support (e.g., VA-ECLS) specifically may benefit from somatic tissue oximetry. In VA-ECLS, femoral artery cannulation is a commonly used technique, however this access technique often compromises perfusion of the lower limbs, causing limb ischemia and concomitant tissue damage. In some cases, placement of a distal cannula is required to prevent fasciotomy or even limb amputation. Chapter 6 shows that tissue oximetry aids in early recognition of compromised limb perfusion and

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contributes to timely intervention by identifying the need for a distal cannula. Moreover, tissue oximetry even appeared superior in terms of early detection of malperfusion as compared to repeated bedside evaluation of limb temperature. In case of clotting in the distal femoral cannula, our analysis showed clear changes in limb rSO_2 values before a decrease in limb temperature became evident.

Another potential target for somatic tissue monitoring are free skin transplants. The use of autologous skin and fat tissue supplied by an isolated perforator vessel has gained popularity over the recent years in plastic reconstructive surgery. Free skin-fat transplants, in the literature referred to as a flaps, are increasingly used for autologous breast reconstructive surgery. In the late eighties and early nineties, the deep inferior epigastric perforator (DIEP)-flap was introduced as an alternative to the transverse rectus abdominis myocutaneous (TRAM)-flap. While the latter involves rectus abdominis muscle and fascia excision, the abdominal muscles remain intact in DIEP-flap surgery.

Maintaining abdominal wall integrity contributes to decreased postoperative pain and risk of complications by minimizing donor-site morbidity as compared to TRAM-flap surgery.¹⁶ The DIEP-flap, however, is particularly susceptible to ischemia in which the quality of the microsurgical anastomoses determines flap perfusion and thereby its viability. Circulatory failure in a DIEP-flap is a detrimental complication that can cause partial or even complete flap loss. While previous reports suggest that non-invasive tissue oximetry might be of added value in perioperative DIEP-flap monitoring, these studies only performed unilateral measurements. In this specific application of tissue oximetry, the direct comparison with an internal or personalized reference value is crucial. Rather than aiming at maintaining stable rSO_2 values, which is the commonly used strategy in brain monitoring during cardiac surgery, the intended use of tissue oximetry in free skin transplants is to assess tissue reoxygenation or tissue recovery.

In a prospective explorative study, we identified several patterns of tissue oximetry readings in the first 24 hours following unilateral secondary DIEP-flap breast reconstructive surgery (Chapter 8). Most patients showed a gradual recovery of DIEP-flap tissue oxygenation and an uncomplicated postoperative course. Two of the studied patients, however, underwent re-exploration of the DIEP-flap due to a non-patent anastomosis. This was reflected by an enlarged ΔrSO_2 (absolute difference in regional tissue oxygen saturation values between DIEP-flap and native breast), as well as a decreased rSO_2 measured in the DIEP-flap as observed in both complicated cases. These aberrant rSO_2 values were apparent immediately following initiation of the measurement. In this explorative study, we used tissue oximetry readings in the native breast as a per-

sonalized reference value. Although the DIEP-flap concerns a different tissue type than the native breast, this personalized reference measurement enabled direct discrimination between cases with apparent circulatory failure of the perforator vessels and uncomplicated cases. These results suggest that the native breast can serve as an internal reference measurement and that non-invasive tissue oximetry values provide an early marker for impaired DIEP-flap perfusion. Nevertheless, in order to enable prompt intervention, further studies are needed to identify optimal ΔrSO_2 thresholds.

Microvascular reactivity

Apart from cerebral and/or somatic tissue oximetry, NIRS can also be used to gain insight in dynamic parameters, such as microvascular reactivity. Intraoperative monitoring of peripheral microvascular reactivity enables early detection of alterations in microcirculatory function and may contribute to preventing impaired tissue perfusion and adverse patient outcome. Combining continuous non-invasive tissue oxygenation monitoring with a reproducible ischemia-reperfusion challenge allows assessment of vascular reactivity and potentially early recognition of altered vascular reactivity and function (Chapter 7). Through a prospective study, 34 adult patients undergoing cardiac surgery with CPB were studied. A vascular occlusion test (VOT) was performed by occluding the brachial artery using a pneumatic tourniquet inflated 30 mmHg above the patient's systolic blood pressure for a fixed time frame of 3 minutes. Somatic rSO_2 was continuously monitored at the internal surface of the proximal third of the forearm to assess the rate of tissue deoxygenated and reperfusion following the VOT. One of the studied parameters included the occlusion slope, which describes the decrease in rSO_2 directly following occlusion of the brachial artery. According to previous studies, this parameter represents the rate of mitochondrial oxygen consumption and local tissue metabolism.¹⁷ The results showed an increased occlusion slope during and following CPB as compared to prior to CPB, indicating increased oxygen consumption during and after CPB. This change has been described previously, and is explained by the effect of general anesthesia with propofol on oxygen delivery and extraction as well as capillary blood flow. Another VOT-derived parameter which showed significant changes throughout the cardiac surgical procedure is the lowest rSO_2 value measured during the ischemic period. This parameter in particular provides information regarding the absolute oxygen reserve in the microcirculatory system. During CPB, this value was lowered as compared to prior to and following CPB, suggesting an effect of CPB on the absolute oxygen reserve. Supported by the decreased hemoglobin values during bypass, part of this effect could be ex-

plained by hemodilution. Interestingly, the time necessary for rSO_2 recovery did not change through the different phases of cardiac surgery. Therefore, one can speculate that reperfusion or tissue oxygenation recovery occurred in a more efficient manner during CPB. A possible explanation can be found in the increased blood flow velocity in minor hemodilution by a decrease in systemic vascular resistance in combination with a reduced blood viscosity. In this case, the increased blood flow in the capillaries compensated for the effects of hemodilution with regards to local rSO_2 values.

Another parameter that provides information regarding microcirculatory function is the reperfusion slope or recovery slope. This VOT-parameter reflects the time required to wash out stagnant blood as well as the local reperfusion reserve. In our study, an increased reperfusion slope was seen after termination of CPB compared to prior to CPB, suggesting altered peripheral microvascular reactivity. The duration of reperfusion remained unchanged, which may be indicative of enhanced reperfusion efficiency. Contrastingly, a previous interventional study concluded that CPB worsened microvascular reactivity with decreased microcirculatory function, as illustrated by a successive decline in reperfusion slopes with increasing CPB duration.¹⁸ Possible factors contributing to this discrepancy include differences across studies with regards to CPB protocol, measurement site, tissue oximetry probe, and ischemic challenge protocol. Besides interindividual variations, VOT-derived measurements are obviously affected by the duration of occlusion as well as the algorithm used to calculate the occlusion and reperfusion slopes, amongst other factors. In addition, the clinical relevance of alterations identified by dynamic measurements of peripheral tissue oxygenation remains to be further explored. Since the current literature describes a variety of measurement protocols and calculation methods, further studies are warranted to determine the optimal approach in performing the VOT.

Considerations of tissue oximetry application

Despite the need for superior continuous and non-invasive monitoring methods in patient care, tissue oximetry is not yet part of standard routine practice. A multitude of anecdotal reports and recent reviews have tempered the enthusiasm for routine use of rSO_2 by questioning whether it leads to improved patient outcomes or not.¹⁹ One of the causative factors is the lack of intervention-guided trials linking disturbances in tissue oxygen saturation to adverse clinical outcome. Although multiple studies reported an association between tissue oxygen desaturation and post-surgical complications, it remains unclear if this is part of a causal relationship or just a reflection of overall morbidity. In addition, some studies elaborated that intraoperative optimization of rSO_2 will result in

fewer complications, however, these studies were mostly observational or underpowered to detect any significant effects. Moreover, in a systematic review conducted by Zheng et al., it was concluded that intraoperative correction of cerebral rSO_2 is not associated with improved neurologic outcome.²⁰ The role of intrinsic autoregulatory activity was most probably neglected when previous studies attempted to link decreased rSO_2 to clinical outcome.

Another factor precluding routine use of tissue oximetry is the lack of clear application-specific rSO_2 thresholds requiring immediate intervention. When determining a clear threshold rSO_2 or change in rSO_2 necessitating prompt intervention, it is important to take the limitations of the tissue oxygenation measurement into account. Clinical oximeter devices are destined for either trend or absolute rSO_2 monitoring, utilizing an algorithm that requires the assumption of a fixed ratio of arterial to venous blood in the vascular bed in the area of interest. This algorithm, however, cannot adapt to all possible applications of tissue oximetry. Hence, one must be cautious when interpreting absolute rSO_2 values derived from measurements performed in different areas.

To date, there are no clear indications when intervention to correct rSO_2 is warranted. One may argue that this is partially due to the fact that studies up until now failed to demonstrate a causal relationship between tissue oxygen desaturations identified by tissue oximetry and adverse clinical outcome.

Additionally, the use of different monitoring devices used across studies makes standardised application of cerebral oximetry even more challenging. Oximeter devices from different manufacturers each use different algorithms for estimation of local oxygen content, and utilize varying numbers and wavelengths of near-infrared light. Furthermore, since every single device differs in terms of hardware as well as software (data acquisition, filtering and processing), each device should be used in concordance with a device-specific and application-specific set of desaturation thresholds.

Not only the specific measurement device but also the different applications in tissue oximetry directly affect the measurement and derived rSO_2 values. While originally developed for cerebral tissue monitoring, tissue oximetry has been increasingly applied in different clinical settings, including somatic tissue monitoring in autologous tissue transplants²¹ or peripheral tissue, including muscle,²²⁻²⁴ as well as monitoring of the central nervous system by assessing spinal perfusion.²⁵ Development of standardized desaturation thresholds for the different applications will aid in interpretation of rSO_2 values and thereby establish routine use of tissue oximetry.

The main goal of continuous rSO_2 measurement is to prevent or minimize hypoxemia by early detection of decreased oxygen delivery. The relationship between clinical outcome and changes in rSO_2 readings remains doubtful, de-

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spite the large amount of literature describing the application of tissue oximetry in surgical patients. Nonetheless, it is clear that the measurement technique is capable of identifying hemodynamic fluctuations. In general, microvascular alterations associated with microcirculatory dysfunction are predominant factors in the process of tissue hypoxia. Microcirculatory dysfunction is known to precede tissue hypoxia, and if left untreated results in ischemic tissue damage. Adopting microcirculatory monitoring as the standard of care may prove to be the next big frontier in critical care management. Monitoring microcirculation at the bedside, however, poses several practical challenges, nor is it easy to estimate tissue perfusion from standard physiological monitoring modalities. Now the limitations inherent to using NIRS in non-invasive tissue oximetry are identified, the focus should be on determining the optimal measurement protocol for bedside microvascular monitoring and interpretation of measurement values.

Physiologic knowledge, including definition of thresholds for tissue damage that are associated with adverse outcomes

This is a critical issue that remains unresolved to date. In previous studies, mostly arbitrary cut-offs are used for analysis of rSO_2 values. One difficulty is that injury thresholds may vary among individuals because of differences in age, cerebral metabolism, anaesthetic and sedative regimen, body temperature, and other factors. However, if the technology accounts for changes in oxygenation because of changes in flow and blood volume in the sensor field, then autoregulation of cerebral blood flow should not be a confounder in establishing threshold values, since autoregulation affects vessel diameter and thereby blood flow. The other issue is the “area under the curve” problem: is 3 hours at a 10% reduced cerebral saturation equivalent in injury to a 1 hour interval at 30%? Greater knowledge in this area is critical for study designs because interventions need to be assigned to an appropriate threshold and duration for potential tissue injury. Without appropriate thresholds, interventions will be initiated that are either unnecessary or it may be too late to successfully alter the chance of adverse patient outcome. Furthermore, interventions have their own risks; for example vasopressors may decrease blood flow in unintended ways, and transfusion of blood products expose patients to a variety of risks.

Conclusion

Many studies have been conducted implicating a link between changes in regional tissue oxygen saturation observed by tissue oximetry and clinical out-

comes. Despite this fact, the evidence for a causal relationship between tissue oximetry readings and outcome remains questionable. Well-designed prospective studies testing the hypothesis that monitoring oxygenation status in one organ is predictive for more general patient outcomes still needs to be conducted. Application-specific variables as well as measurement technique-related factors play a role in the failure of studies to demonstrate a clear relationship between tissue oximetry readings and complications resulting from tissue ischemia.

Moreover, there is a lack of intervention-guided studies identifying organ-specific thresholds associated with concomitant ischemic tissue damage. Therefore, more work that defines regional variations in tissue oxygenation in critical organs is warranted. Such studies will contribute to the inclusion of monitoring and imaging of tissue oxygenation in routine practice in the care of high-risk patients because the monitors will provide outputs that direct therapy to improve clinical outcomes.

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Summary

The introduction of near-infrared spectroscopy for assessment of regional tissue oxygenation was an important landmark in the history of tissue perfusion monitoring. Since then, non-invasive tissue oximetry gained wide interest with subsequent studies addressing the clinical importance of continuous monitoring of tissue perfusion. An increasing amount of literature including many observational and few intervention-guided studies elucidated on the added value of primarily regional cerebral oximetry in terms of predicting neurologic outcome following cardiopulmonary bypass. Some studies even suggested that cerebral oximetry can be used as an organ index, meaning that maintaining adequate tissue oximetry levels is beneficial for all vital organs. Furthermore, continuous tissue oximetry proved to be a valuable addition in various clinical applications (short-term and prolonged cardiopulmonary support, and monitoring graft viability ensuing transplant surgery), as it effectively identifies changes in tissue oxygenation following several iatrogenic events.

Despite these proposed benefits, routine use of tissue oximetry in the clinical setting is, as of now, far from evident. For a compelling part this is due to the lack of well-designed interventional studies showing a clear association between tissue oximetry values and outcome, as well as discordance regarding clinically relevant and application-specific tissue oxygenation thresholds predictive for adverse outcome. Moreover, different applications of tissue oximetry require different interpretation strategies due to the absence or presence of regional vascular autoregulatory activity. Especially during cerebral oximetry, intact or any extent of temporary or permanently disturbed cerebral autoregulation directly affects oxygen delivery. In this case, assumptions as part of the algorithm used for calculation of oxygenated and deoxygenated hemoglobin may contribute to interpretation errors in apparent normal tissue oxygenation. Therefore, it remains of utmost importance to include all available clinical information when performing tissue oximetry.

Taking the aforementioned into account, non-invasive tissue oximetry aids in prompt assessment of tissue oxygenation and may thereby contribute to prevention of complications associated with hypoxia. The latter catalyzes indivertible developments for various prospective clinical applications.

Samenvatting

De introductie van nabij-infrarood spectroscopie voor het regionaal monitoren van weefseloxygenatie was een belangrijke mijlpaal in de geschiedenis van weefselperfusie monitoring. Sindsdien is non-invasieve weefseloxymentrie meer onder de aandacht gekomen en richten studies zich op het klinische belang van continue weefselsonitoring. Een toenemende hoeveelheid literatuur waarvan enkele interventionele en vele observationele studies focust op voornamelijk regionale cerebrale oxymentrie in de context van het voorspellen van neurologische complicaties na cardiopulmonale bypass. Sommige studies suggereren zelfs dat cerebrale oxymentrie als een orgaanindex kan worden toegepast, hetgeen betekent dat behoud van adequate weefseloxymentrie waarden gunstig zou zijn voor alle vitale organen. Continue weefseloxymentrie is een bewezen waardevolle aanvulling in verscheidene klinische toepassingen (kort- en langdurige cardiopulmonale ondersteuning en monitoren van de levensvatbaarheid van een transplantaat), daar het effectief blijkt in identificatie van veranderingen in weefseloxygenatie ten gevolge van verschillende iatrogene gebeurtenissen.

Ondanks deze voorgestelde voordelen is routinematig gebruik van weefseloxymentrie in de klinische setting bij lange na niet vanzelfsprekend. De oorzaak hiervan kan deels gezocht worden in het gebrek aan correct opgezette interventionele studies die een duidelijke associatie tussen weefseloxymentrie waarden en relevante uitkomsten aantonen. Daarbij bestaat ook tegenstrijdigheid in klinisch relevante en applicatie-specifieke grenswaarden voor weefseloxygenatiewaarden die gelinkt zijn aan nadelige gezondheidseffecten. Tevens behoeven de verschillende afzonderlijke toepassingen van weefseloxymentrie verschillende interpretatiestrategieën vanwege de aan- of afwezigheid van regionale autoregulatorische vasculaire activiteit. Vooral bij cerebrale oxymentrie is intacte cerebrale autoregulatie, of een verstoring hiervan, direct van invloed op de zuurstofvoorziening van het brein. In beide gevallen dragen aannames, welke onderdeel uitmaken van het algoritme dat gebruikt wordt voor de berekening van geoxygeneerd en gedeoxygeneerd hemoglobine, bij aan interpretatiefouten bij ogenschijnlijk normale weefseloxygenatie waarden. Het is daarom van groot belang om rekening te houden met alle beschikbare klinische informatie bij het toepassen van weefseloxymentrie.

Met inachtneming van de voorgenoemde zaken kan gesteld worden dat non-invasieve weefseloxymentrie bijdraagt in directe beoordeling van weefseloxygenatie en daarbij preventie van complicaties ten gevolge van hypoxie. Laatsgenoemde katalyseert de onvermijdbare ontwikkeling van nieuwe klinische toepassingen.

Valorization

Non-invasive tissue oximetry – an integral puzzle piece

Inadequate tissue oxygen delivery is known to result in complications, contributing to morbidity and mortality following or during medical procedures. In order to minimize the risk of adverse outcome, close monitoring of patient's hemodynamic status at all times is indispensable. Non-invasive tissue oximetry is a monitoring method for continuous assessment of tissue oxygenation, which may aid in detection of hemodynamic instability and otherwise unnoticed hypoxia.

To date, numerous studies (of which mostly observational) focused on the use of non-invasive tissue oximetry in surgical patients, proposing its predictive value in relation to clinical outcome. Cerebral oximetry in particular has been the focus in the context of preventing neurological complications following cardiac surgery. These complications, including stroke which appears to be the most detrimental, are complex in nature and elicited by a multitude of preoperative and perioperative factors. Intraoperative cerebral hypoxia resulting from hypoperfusion is generally accepted as a factor contributing to the risk of adverse neurologic outcome.^{1,2} Although the exact etiology is not yet completely understood, continuous assessment of tissue perfusion may aid to a better understanding of the role of tissue hypoxia in the development of postoperative cognitive complications.

While the incidence of neurological complications may seem relatively low, the effects on the patient's physical and psychological health are tremendous with serious implications for the quality of life.³ The reported incidence of stroke following cardiac surgery varies around 4.2%, meaning that every year 33 patients are affected based on 800 procedures annually.⁴ Postoperative stroke entails prolonged hospital stays of on average seven days with an incremental increase of hospital resources.^{5,6} In the United States, for each affected patient the estimated added costs make up to \$18,552, of which \$1,000 are attributable to each additional day of hospitalization.⁷

Another type of neurological complication that may emerge following cardiac surgery is delirium, which is characterized by a state of confusion and inattention. Although often seen as a reversible condition, delirium contributes to persistent functional decline and significant morbidity and mortality risk.⁸ Postoperative delirium is associated with only four extra hospitalization days, but is far more common as compared to stroke, with incidence rates varying around 55%.^{9,10} If non-invasive tissue oximetry could help to prevent part of the neurologic complications, such as hypoxia-related stroke or delirium^{2,11}, the odds of an uncomplicated prosperous recovery would increase and a substantial pro-

portion of hospital costs could be saved. The costs of performing the measurement include the purchase of disposable self-adhesive sensors (usually two, for bilateral measurement of tissue oxygenation), which in the United States cost around \$200 per patient¹², and a one-time investment for purchasing the oximeter device. The costs for routine application of clinical oximetry, however, are only marginal compared to the major additional expenses associated with ischemic-related stroke and delirium¹³, let alone the deleterious long-term effects of these complications, i.e. the quality of life.

The pathophysiology of neurologic postoperative complications is complex and multifactorial in nature. Therefore, some neurologic complications are nearly impossible to prevent due to unforeseen events occurring in the perioperative period (e.g. embolism originated from the cardiopulmonary bypass circuit) and the role of certain patient characteristics is not subject to change (pre-existing co-morbidities and positive family history of adverse neurovascular events). Another substantial proportion with less of a complex etiology is caused by modifiable factors and therefore theoretically concerns preventable cases. For example, hemodynamic instability is known to affect the risk of hypoxia. Moreover, hypercapnia and excessive hemodilution are thought to alter the risk of neurologic complication (chapter 3).¹⁴ The cardiopulmonary bypass protocol is, therefore, an important factor in enabling and maintaining adequate tissue perfusion and should be critically evaluated in order to minimize the risk of neurologic complications. Strict monitoring routines concern another factor of importance in preserving hemodynamic integrity, specifically monitoring at the tissue level since general hemodynamic factors may not adequately represent local tissue oxygenation status.¹⁵

With non-invasive tissue oximetry on the rise and being increasingly applied as a brain monitor, the technique appears to be a viable assessment method for diverting adverse neurologic outcome. On that note, cerebral oximetry showed to adequately reflect real-time changes in tissue oxygenation readings following several iatrogenic events. Despite the abundance of studies implying that oxygen desaturations detected by cerebral oximetry predict neurological outcome, evidence for a causal relationship remains scarce. Part of the explanation can be found in the fact that the development of neurological complications is a complex process, as mentioned beforehand, which is still not entirely understood. Deoxygenation episodes detected by cerebral oximetry should probably be considered as a contributor, rather than an independent causative factor for clinical neurologic damage and evident changes in neurocognitive function (chapter 2).

In addition to the latter, when performing cerebral oximetry it is important to consider the intrinsic system of cerebral autoregulation. When intact, reactive vasoconstriction and vasodilatation ensures adequate tissue oxygenation, providing cerebral protection. Although often unacknowledged, disturbances in autoregulatory function have shown to result in neurologic complications and thus should be avoided at all times. In this thesis, several modifiable factors requiring strict regulation in order to maintain intact cerebral autoregulation are identified. In turn, a perfusion protocol that includes maintaining these factors within the physiologic range confers to the observed low incidence of neurological complications by enabling intact autoregulatory function.

Taking these practical considerations into account, one may conclude that tissue oximetry, inherently due to its measurement technique and thus non-invasive nature, cannot independently predict the occurrence of complications with a multifactorial nature such as ischemic stroke or delirium. Similar to most non-invasive monitoring tools and methods, tissue oximetry readings should be interpreted in the context of all clinical information available. The scientific value of this thesis is that non-invasive tissue oximetry derived measurement values should be viewed as an integral piece of information rather than a superior monitoring method.

Besides its original intended use (i.e. brain monitoring), non-invasive tissue oximetry is increasingly applied in somatic tissue monitoring. One example is assessment of distal limb perfusion in patients supported by veno-arterial extracorporeal life support (VA-ECLS). Femoral access techniques often used in VA-ECLS may compromise limb perfusion, therefore predisposing the patient to concomitant tissue damage with potential disastrous effects. Tissue oximetry performed at the calf muscle proved effective for identification of endangered limb perfusion by showcasing aberrant tissue oximetry readings before any other clinical parameters showed any evident change (chapter 6).

Another example of somatic tissue oximetry applies to monitoring autologous breast reconstructive surgery, in which abdominal wall tissue is transplanted to the chest area using microsurgical anastomoses. Graft failure, in the worst case, could lead to loss of the entire tissue flap with a major additional risk of physical and psychological burden for the patient. By immediately depicting deviant measurement values as compared to the expected physiologic tissue response, tissue oximetry appears superior to other applied monitoring techniques, which solely provide delayed timing of alarm signals. Tissue oximetry could aid in timely detection of circulatory compromise and thereby lower the rate of complications resulting from ischemic tissue damage. Successively,

avoiding complications contributes to minimizing postoperative morbidity and mitigating health care costs. As is the case in brain monitoring, the costs for performing tissue oximetry are only marginal compared to the costs associated with postoperative complications. In case of arterial or venous thrombosis, surgical re-intervention is necessary to increase the chance of successful flap salvage. This will add around \$76,000 per hour spent in the operating room to the hospital costs. Also, patients experiencing complications generally consume two extra hospital days, leading to another \$7,000 in added costs per patient operated in the United States.¹⁶ In uncomplicated cases, tissue oximetry eliminates the need for prolonged intensive monitoring with savings of \$1,337 (or 6.3%¹⁷) that far outweigh the costs associated with routine use of tissue oximetry.^{17,18}

The relationship between aberrant tissue oximetry readings and clinical outcome appears to be more clear in the somatic applications of tissue oximetry. Complications arising from peripheral tissue ischemia (e.g. the distal limb and autologous breast flaps) are elementary in nature due to the absence of an intrinsic homeostatic autoregulatory system. In cerebral oximetry, one attempts assessing an entire organ system that is only represented by a regional assessment of tissue oxygenation in the prefrontal cortex. In somatic tissue oximetry on the other hand, the readings appear more representative for clinical outcome.

The versatility of tissue oximetry in the clinical setting may broaden the scope for future studies to focus on new potential applications. One prospective application is assessment of the microcirculatory function. Since microcirculatory dysfunction precedes tissue hypoxia, adopting tissue oximetry as a part of standard microcirculatory monitoring may prove to be the next big frontier in critical care management.

With the limitations of non-invasive assessment of tissue oxygenation being identified, future studies should focus on interpretation of measured data and aim at determining clinically relevant and application-specific threshold values for tissue desaturation-related injury. Furthermore, the types of interventions necessary for correcting tissue oxygenation values and its effects on clinical outcome require further clarification.

Overall, non-invasive tissue oximetry is a promising tool for (regional) assessment of tissue oxygenation. Its measurement readings should be considered as an integral source of information, a puzzle piece that together with all clinical information can aid in decision making and minimizing the risk of postoperative complications.

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Curriculum vitae

Nousjka Vranken is geboren op 28 september 1991 te Geleen. In 2008 behaalde zij haar Havo diploma aan de Scholengemeenschap Groenewald te Stein. In hetzelfde jaar startte zij haar opleiding Biometrie aan de Zuyd Hogeschool in Heerlen. In 2013 startte zij met de opleiding Gezondheidswetenschappen aan de Universiteit Maastricht en tegelijkertijd haar functie als promovendus bij het Maastricht Universitair Medisch Centrum. In 2016 behaalde zij haar bachelordiploma Gezondheidswetenschappen met Cum Laude onderscheiding in de richting Biologie en Gezondheid. Later dat jaar in september 2016 startte zij met de masteropleiding Arts-Klinisch Onderzoeker aan de Universiteit Maastricht.

Nousjka Vranken was born in Geleen, the Netherlands, on September 28th 1991. In 2008 she graduated from Scholengemeenschap Groenewald in Stein. Immediately thereafter she started studying Biometrics at Zuyd Hogeschool. After graduating from Biometrics she initiated her studies Health Sciences at Maastricht University with as field of expertise Biology and Health. At the same time, she started her work as a PhD student at the Maastricht University Medical Center. In 2016 she received her bachelor diploma from Health Sciences with Cum Laude distinction. Later that year, in September 2016, she started the master's study Physician-Clinical Investigator at Maastricht University.

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