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# Comparison of a Thigh-Worn Accelerometer Algorithm With Diary Estimates of Time in Bed and Time Asleep: The 1970 British Cohort Study 

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#### Abstract

Background: Thigh-worn accelerometers have established reliability and validity for measurement of free-living physical activity-related behaviors. However, comparisons of methods for measuring sleep and time in bed using the thigh-worn accelerometer are rare. The authors compared the thigh-worn accelerometer algorithm that estimates time in bed with the output of a sleep diary (time in bed and time asleep). Methods: Participants ( $N=5,498$ ), from the 1970 British Cohort Study, wore an activPAL device on their thigh continuously for 7 days and completed a sleep diary. Bland-Altman plots and Pearson correlation coefficients were used to examine associations between the algorithm derived and diary time in bed and asleep. Results: The algorithm estimated acceptable levels of agreement with time in bed when compared with diary time in bed (mean bias of -11.4 min ; limits of agreement -264.6 to 241.8 ). The algorithm-derived time in bed overestimated diary sleep time (mean bias of 55.2 min ; limits of agreement -204.5 to 314.8 min ). Algorithm and sleep diary are reasonably correlated ( $\rho=.48,95 \%$ confidence interval [.45,.52] for women and $\rho=.51,95 \%$ confidence interval [.47,.55] for men) and provide broadly comparable estimates of time in bed but not for sleep time. Conclusions: The algorithm showed acceptable estimates of time in bed compared with diary at the group level. However, about half of the participants were outside of the $\pm 30 \mathrm{~min}$ difference of a clinically relevant limit at an individual level.


Keywords: activPAL, sleep, sleep diary

Lifestyle behaviors are associated with a multitude of health outcomes, including cardiovascular diseases and mortality (HoevenaarBlom, Spijkerman, Kromhout, \& Verschuren, 2014; Xiao, Keadle, Hollenbeck, \& Matthews, 2014). Among them, the potential health impacts of sleep, as reflected by sleep duration, quality, and timing, are less well explored (Barbaresko, Rienks, \& Nöthlings, 2018), possibly due to the difficulties with robustly measuring sleep-related

[^0]exposures, including sleep duration. Self-reported sleep duration (short or long sleep duration) is linked to adverse health outcomes including obesity, diabetes, cardiovascular diseases, mood disorders, and mortality (Grandner, 2017). Although laboratory-based polysomnography is the gold standard of objective sleep measurement, it is impractical in free-living epidemiological studies considering the cost, professional monitoring, and large resource demands due to its specialized equipment (Van de Water, Holmes, \& Hurley, 2011). Diaries are common low-cost/low-tech alternatives for sleep monitoring in population research. However, diary-based methods could be burdensome for participants and subject to recall bias (Tonetti, Mingozzi, \& Natale, 2016), among other limitations (Riemann, 2012). A 24-hr device-based measurement methods might be a less burdensome option to estimate sleep duration in large-scale epidemiological studies with the added advantage of not being subject to recall bias.

Wearable devices, noninvasive and inexpensive methods for use in nonlaboratory settings, have been increasingly used to estimate sleep, and several studies have examined the agreement between self-reported measures and accelerometer data in different populations (Arora, Broglia, Pushpakumar, Lodhi, \& Taheri, 2013; Girschik, Fritschi, Heyworth, \& Waters, 2012; McCrae et al.,
2005). Although the thigh-worn accelerometer is considered as the gold standard for free-living measurements of sitting time and posture (Dahlgren, Carlsson, Moorhead, Häger-Ross, \& McDonough, 2010; Lyden, Keadle, Staudenmayer, \& Freedson, 2017; Oliver, Badland, Shepherd, \& Schofield, 2011), their uptake in sleep measurement studies is limited. Winkler et al. (2016) and van der Berg et al. (2016) have recently developed automated algorithms to isolate adults' valid waking wear periods from thighworn activPAL data collected with a continuous wear protocol. In addition to these algorithms, other time in bed estimation algorithms exist, for example, the "CREA" algorithm built into the activPAL software (PAL Technologies, Glasgow, United Kingdom), which considers 24-hr wear time, classifies lying time as primary (e.g., during the night) or secondary (e.g., during the day), and automatically excludes sleeping time. Recent studies have used Winkler et al.'s (2016) algorithm to calculate sleep duration (Biddle et al., 2018; Ezeugwu \& Manns, 2017). Biddle et al. (2018) have suggested an agreement between results of algorithm-derived and diary-based sleep duration in their study; for example, the algo-rithm-derived and diary-based sleep time association estimates with fasting glucose were nearly identical ( $1.01,95 \%$ confidence interval [CI] [0.95, 1.07] and $1.02,95 \%$ CI [0.96, 1.08], respectively).

Despite the increasingly frequent (Biddle et al., 2018; Ezeugwu \& Manns, 2017) use of this algorithm for estimating time in bed, very few studies have compared algorithm-derived time in bed with other common measures such as diaries (van der Berg et al., 2016; Winkler et al., 2016) of sleep time. These studies generally show a correlation between algorithm-derived time in bed and sleep diary-derived time in bed (van der Berg et al., 2016; Winkler et al., 2016), although none of them made direct comparisons with sleep time. The aim of this study was to compare Winkler et al.'s (2016) algorithm-based method that uses the thigh-worn accelerometer data with diary estimates of time in bed and time asleep in a large and established population birth cohort from Britain.

## Methods

## Participants and Design

These secondary analyses of available aggregate data have been conducted using the 1970 British Cohort Study (BCS70) data. The BCS70 is an observational prospective population-based cohort study, following the lives of 17,287 people born in a single week of 1970 in England, Scotland, and Wales. In 2016-18, a new wave of data collection was conducted when participants were aged 46-48 years. This comprised of computer-assisted personal interviewing to collect the self-reported information via interviews during the home visit (1970 British Cohort Study, 2019). Nurses conducted physical examinations and placed the activity monitor on participants. The rationale and sampling methods used in the BCS70 are described in detail elsewhere (1970 British Cohort Study, 2019; Elliott \& Shepherd, 2006). All participants gave written informed consent, and the age-46 biomedical survey received ethics from National Research Ethics Service Committee South East CoastBrighton and Sussex (Ref 15/LO/1446).

## Measurements

Computer-assisted personal interviews collected data on participants' self-rated general health, disability/limitations, smoking, and occupation. The disability/physical limitation was assessed
using the European Statistics on Income and Living Conditions (Arora et al., 2015). During the home visit, a nurse took participant's anthropometric measurements including height and weight. Body mass index was calculated as weight (in kilogram) divided by height squared (in meter square).

Participants were asked to wear an activPAL3 device (PAL Technologies) on their thigh for the 7 days following their nurse visit. At the end of the visit, nurses placed and attached the devices to the thigh using a medical dressing. The device is a triaxial accelerometer that provides estimated body posture (sitting/reclining/ lying and standing) and stepping speed (cadence) based on 3Dacceleration information with a sampling frequency of 20 Hz . Devices were waterproofed to allow for continuous wear $24 \mathrm{hr} / \mathrm{day}$. Participants were asked to wear the device for seven consecutive days without removing it at any time. After the device was returned, data were downloaded and processed using an open-source program that incorporates the Winkler et al. (2016) algorithm to quantify valid waking wear times by the custodians (Winkler et al., 2016). The Winkler et al. (2016) algorithm was setup to identify time as either (a) time in bed or nonwear on a valid day, (b) waking wear time on a valid day, and (c) any time on an invalid day. This algorithm was developed for use with 24-hr wear protocols in adults to classify activity bouts recorded in activPAL "Events" files as "sleep"/nonwear (or not) and on a valid day (or not). This automated approach excludes long periods without posture change/movement, adjacent low-active periods, and days with minimal movement and wear based on a simple algorithm. Briefly, development of an algorithm to estimate valid waking wear protocols has four steps including identifying bouts, examining surrounding bouts, identifying other invalid data, and quality control such as checking and error correction. The algorithm was validated based on a minimum of four valid wear days with at least 10 hr of waking wear data and $>500$ steps (Winkler et al., 2016). The algorithm aimed to measure in bed and nonwear time versus waking wear time. We used in bed and nonwear time together in our analysis. We excluded the first day of data and defined subsequent days as the 24 hr between consecutive midnights. Participants providing at least one valid day, defined as waking wear time of more than $10 \mathrm{hr} /$ day were included in the core analysis (van der Velde et al., 2018). Figure 1 illustrates each stage of the algorithm.

Participants were also asked to complete a sleep diary for each day that they wore the monitor. The diary recorded some key information including the exact times (in hours: minutes) they went to bed, fell asleep, woke up, and got out of bed. There were also separate entries on how many times participants got up during the night and self-rated sleep quality. The full diary is shown in Supplemental Material 1 (available online).

## Data Handling

As the algorithm was designed to distinguish waking wear time from time in bed (Winkler et al., 2016), the algorithm-derived time in bed is computed by subtracting valid waking wear time from 24 hr (Biddle et al., 2018). We made both day to day comparisons and mean value comparisons of valid days for sleep diary time in bed and sleep time data as well as algorithm-derived time in bed data. As polysomnography can measure the sleep accurately, we defined diary-reported sleep time as the time participants' wake-up minus the time they fall asleep. Diary time in bed was defined as the time participants get out of bed minus the time they go to bed. Both algorithm data and sleep diary data were calculated as minutes.


Figure 1 - Flow chart for the steps of algorithm.

## Statistical Analysis

Statistical analysis was performed using SPSS (version 26.0; IBM Corp., Chicago, IL) and MedCalc software (MedCalc Software Ltd., Ostend, Belgium). The accelerometer and sleep diary variables were analyzed as continuous variables. We ran the $\chi^{2}$ test and analysis of variance to examine differences by sex for categorical and continuous variables, respectively. Descriptive statistics were calculated for demographic characteristics of participants. We compared algorithm-derived time in bed versus bed time and sleep duration of mean minute/day from diary using the paired sample $t$ test. We also used Schuirmann's (1987) two one-sided tests approach to test equivalence with a specified confidence level between observations. We defined a priori differences between algorithm and diary of $\pm 30 \mathrm{~min}$ as satisfactory for time in bed and sleep time and calculated $90 \%$ CI. If the entire range of $90 \%$ CI of the mean difference lay within the rage of $\pm 30 \mathrm{~min}$, we concluded that the two observations were equivalent. Pearson correlation coefficients were calculated to test the association between the algorithm derived and diary time in bed and sleep time. We used bootstrapping methods to calculate $95 \%$ CIs. Differences in correlations across subgroups were tested using Fisher's $z$ test. In
addition to Pearson correlation coefficients, we calculated absolute intraclass correlation coefficients to assess reliability of repeated measurements among different days as a sensitivity analysis. In stratified analyses, we examined the correlation (Pearson coefficients) between the algorithm derived and diary time in bed and asleep across different education groups and health statuses. We conducted Bland-Altman plot with multiple measurements per subject for daily data to examine the agreement of the algorithmand diary-derived times in bed and times asleep. Limits of agreement (LoAs) were calculated as bias $\pm 1.96 S D$ of the difference. A positive value of the mean difference between algorithm and diary indicates that algorithm overestimates diary data, whereas a negative value indicates that algorithm underestimates diary data. Similar to previous studies (de Zambotti, Baker, \& Colrain, 2015; Short, Gradisar, Lack, Wright, \& Carskadon, 2012), we performed additional Bland-Altman plots, where we defined a priori differences between algorithm and diary of $\pm 30 \mathrm{~min}$ as satisfactory for time in bed and sleep time. The percentage of participants falling within this range is provided. We also performed Bland-Altman plot to examine the agreement of the algorithm- and diary-derived times in bed and times asleep for each day separately as sensitivity analysis. In addition, we used the Bland-Altman plot to examine the agreement of the algorithm- and diary-derived times in bed and times asleep. We performed linear regression analysis to evaluate proportional bias. We specified the difference between algorithm and diary as the dependent variable, and the mean of the algorithm and diary as the independent variable. In this analysis, a $p<.05$ model coefficient value indicated the presence of proportional bias. In a sensitivity analysis, we repeated the above Bland-Altman plots but included participants with at least $>4$ day of valid data and at least $20 \mathrm{hr} /$ day wear. We also calculated Pearson correlation coefficients for each day. All statistical tests were two-tailed, and values are reported as mean and $95 \%$ CIs.

## Results

Table 1 shows participants' demographic, health status, and lifestyle health behaviors characteristics. There were no appreciable differences in the accelerometer $24-\mathrm{hr}$ waking wear time between men and women (mean 24-hr waking wear time $16.0 \mathrm{hr} /$ day, $S D$ $1.3 \mathrm{hr} /$ day and mean $24-\mathrm{hr}$ waking wear time $15.7 \mathrm{hr} /$ day, $S D$ $1.3 \mathrm{hr} /$ day, respectively). The mean nonwear time for valid days was $8.1 \mathrm{hr} /$ day.

Table 2 compares absolute accelerometer time in bed with the diary-reported time in bed and asleep. The differences between algorithm-derived and diary time in bed by sex were statistically significant but practically small (mean $-15.5 \mathrm{~min} /$ day for women and -3.5 min for men). The differences between algorithm-derived time in bed and diary sleep time were larger and also statistically significant (mean 56.0 min for women and 57.4 min for men). According to the two one-sided tests approach, we found that algorithm-derived and diary time in bed was equivalent for total, women and men ( $90 \%$ CI $[-11.3,-8.2]$; $90 \%$ CI [-17.6, -13.3$]$; and $90 \% \mathrm{CI}[-5.7,-1.2]$, respectively), whereas the entire range of $90 \% \mathrm{CI}$ of difference for algorithm-derived time in bed and diary sleep time was not in the a priori defined limits of $\pm 30 \mathrm{~min}$. Table 3 presents Pearson's correlation coefficient between algorithmderived time in bed and diary time in bed and sleep time (see Supplementary Figure S1 [available online]). The correlation coefficients between algorithm-derived time in bed and diary time in bed were .48 in women ( $95 \%$ CI $[.45, .52]$ ) and .51 in men ( $95 \%$ CI $[.47, .55])$. The correlation coefficients between
Table 1 Characteristics of Participants

| Characteristics | Total ${ }^{\text {a }}$ ( $\mathrm{N}=5,498$ ) |  |  |  | Women ( $n=2,879$ ) |  |  |  | Men ( $n=2,619$ ) |  |  |  |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: |
|  | \% | 95\% CI | Mean | 95\% Cl | \% | 95\% CI | Mean | 95\% CI | \% | 95\% CI | Mean | 95\% CI |
| Employed | 84.0 | [83.0, 85.0] |  |  | 79.2 | [77.7, 80.6] |  |  | 89.3 | [88.1, 90.6] |  |  |
| Self-employed | 2.4 | [2.0, 2.8] |  |  | 2.6 | [2.1, 3.3] |  |  | 2.1 | [1.6, 2.7] |  |  |
| Shift workers | 15.3 | [14.2, 16.3] |  |  | 13.9 | [12.6, 15.3] |  |  | 16.7 | [15.2, 18.2] |  |  |
| BMI ${ }^{\text {b }}$ |  |  | 28.2 | [28.02, 28.30] |  |  | 27.9 | [27.67, 28.09] |  |  | 28.5 | [28.29, 28.66] |
| Current smoker | 13.3 | [12.3, 14.2] |  |  | 12.9 | [11.7, 14.0] |  |  | 13.7 | [12.4, 15.0] |  |  |
| General health score |  |  | 68.9 | [68.6, 69.9] |  |  | 69.6 | [68.94, 70.72] |  |  | 68.2 | [67.81, 69.42] |
| No long-standing health condition | 84.4 | [83.4, 85.4] |  |  | 82.1 | [80.7, 83.5] |  |  | 87.0 | [85.6, 88.3] |  |  |
| Total time to fall asleep ( $0-15 \mathrm{~min}$ ) | 51.5 | [50.3, 52.9] |  |  | 47.6 | [45.6, 49.5] |  |  | 55.8 | [53.7, 57.6] |  |  |
| Getting enough sleep (most of the time) | 33.5 | [32.3, 34.8] |  |  | 32.5 | [30.9, 34.1] |  |  | 34.6 | [32.8, 36.6] |  |  |
| Times out of bed during night |  |  | 0.7 | [0.71, 0.76] |  |  | 0.8 | 0.70, 0.76 |  |  | 0.7 | [0.71, 0.77] |
| Self-rated sleep quality (1-10) |  |  | 6.9 | [6.91, 7.00] |  |  | 6.9 | 6.90, 7.01 |  |  | 6.9 | [6.88, 7.01] |
| Sleep hours over the last 4 weeks |  |  | 6.8 | [6.78, 6.84] |  |  | 6.9 | 6.86, 6.96 |  |  | 6.7 | [6.67, 6.76] |
| Number of valid days for sleep time (diary) |  |  | 6.5 | [6.47, 6.54] |  |  | 6.5 | 6.47, 6.56 |  |  | 6.5 | [6.45, 6.54] |
| Number of valid days for time in bed (diary) |  |  | 6.5 | [6.51, 6.58] |  |  | 6.6 | 6.52, 6.61 |  |  | 6.5 | [6.48, 6.57] |
| Number of valid days (accelerometer) |  |  | 6.2 | [6.12, 6.20] |  |  | 6.2 | 6.15, 6.25 |  |  | 6.1 | [6.05, 6.18] |
| Accelerometer wear time (hr/day) ${ }^{\text {c }}$ |  |  | 15.8 | [15.80, 15.88] |  |  | 15.7 | 15.65, 15.75 |  |  | 16.0 | [15.94, 16.05] |
| Note. $\mathrm{CI}=$ confidence interval; BMI = body mass i ${ }^{a}$ Age is identical for the whole sample. ${ }^{\text {b }}$ Weight (in k allowance for up to two consecutive minutes of 1-1 | dex. gram) 00 coun | height (in meter s per minute. | quare). ${ }^{\text {c }}$ | erage accelerom | er wea | me per day, w | ere nonw | ar was defined by |  | f at least 60 m | of zero | vity counts, with |

Table 2 Absolute Differences Between Mean Amounts of Time in Bed From The Sleep Diary and Accelerometer Data, by Sex

algorithm-derived time in bed and diary sleep time were lower for both women ( $\rho=.34,95 \%$ CI $[.30, .38]$ ) and men ( $\rho=.39,95 \%$ CI [.35, .43]). Pearson's correlation coefficient for the association between algorithm-derived time in bed and diary time in bed and asleep for each day also produced similar results to the main analysis (see Supplementary Table S1 [available online]). The intraclass correlation coefficients were low for both women and men (see Supplementary Table S2 [available online]). We also compared absolute accelerometer time in bed with the diaryreported time in bed and time asleep by health status (see

Table 3 Correlation Between Algorithm and Diary for Time in Bed and Sleep Time, by Sex

| Algorithm, diary | $\begin{aligned} & \text { Women } \\ & (n=2,812) \end{aligned}$ |  | Men ( $n=2,544$ ) |  | $p$ value ${ }^{\text {a }}$ |
| :---: | :---: | :---: | :---: | :---: | :---: |
|  | $\rho^{\text {b }}$ | 95\% CI ${ }^{\text {c }}$ | $\rho^{\text {b }}$ | 95\% CI ${ }^{\text {c }}$ |  |
| Time in bed | .48* | [.45, 0.52] | .51* | [.47, 0.55] | . 207 |
| Sleep time | .34* | [.30, 0.38] | . $39^{*}$ | [.35, 0.43] | . 023 |

Note. CIs = confidence intervals.
${ }^{\text {a }} p$ value for the difference between Pearson's $\rho$ for women and men, calculated using Fisher's $z$ test. ${ }^{\text {b }}$ Pearson's correlation coefficient. ${ }^{\text {c }} \mathrm{CIs}$ were computed using a bootstrapping procedure.

* $p<.001$.

Supplementary Table S3 [available online]). The mean difference between algorithm- and diary-derived time in bed was lowest for healthy participants ( -8.3 min ), whereas it was the highest in participants who were severely hampered in activities because of health problems ( -28.6 min ). We presented correlations between algorithm and diary time in bed and asleep by health status in Supplementary Table S4 (available online). We also presented absolute differences between mean amounts of time in bed from the sleep diary and the accelerometer data by education level in Supplementary Table S5 (available online) and correlation between algorithm and diary for time in bed and asleep by education level in Supplementary Table S6 (available online). The correlations coefficient between algorithm-derived time in bed and diary time in bed were .51 in the lowest education level and .55 in the highest education level.

The LoAs between algorithm-derived time in bed and diary time in bed are shown in the repeated measures of Bland-Altman plots (Figure 2), which depicts a systematic error (with a mean bias of -6.1 min ; LoA -260.4 to 248.2 min for men and with a mean bias of -16.1 min ; LoA -268.0 to 235.8 min for women). Assuming the diary is the reference method, the algorithm underestimated the time spent in bed for both women and men. Furthermore, linear regression analysis showed that this underestimation was statistically significant ( $95 \%$ CI [0.398, 0.426], $p<.001$; Table 4). According to a priori defined limits, $36.9 \%$ of the measurements were


Figure 2 - (a-c) The repeated measures of Bland-Altman agreement between algorithm and diary for the duration of time in bed. Mean of the differences between algorithm and diary time in bed and lower and upper agreement limits (mean difference $\pm 1.96 S D$ ) are displayed for each BlandAltman plot. The bold lines represent the upper and lower a priori-set clinically satisfactory limits ( $\pm 30 \mathrm{~min}$ from the zero line).

Table 4 Linear Regression Coefficients Between the Mean of the Algorithm- and Diary-Derived Time, and the Difference Between the Algorithm- and Diary-Derived Time

| Participants | Coefficient | 95\% confidence interval | $\boldsymbol{p}$ |
| :--- | :--- | :--- | :--- |
| Women |  |  |  |
| Time in bed (algorithm and diary) | 0.341 | $[0.442,0.481]$ | $<.001$ |
| Time in bed (algorithm) and sleep time (diary) | 0.357 | $[0.517,0.560]$ | $<.001$ |
| Men | 0.294 | $[0.371,0.412]$ | $<.001$ |
| Time in bed (algorithm and diary) | 0.327 | $[0.454,0.499]$ | $<.001$ |
| Time in bed (algorithm) and sleep time (diary) |  | $[0.398,0.426]$ | $<.001$ |
| Total | 0.310 | $[0.487,0.518]$ | $<.001$ |
| Time in bed (algorithm and diary) | 0.341 |  |  |
| Time in bed (algorithm) and sleep time (diary) |  |  |  |

in the range of $\pm 30 \mathrm{~min}$ difference. The repeated measures of Bland-Altman method for comparison between algorithm-derived time in bed and diary sleep time showed a mean bias of 55.0 min ( $\mathrm{LoA}-205.0$ to 315.1 min ) for men and a mean bias of 55.3 min (LoA -204.0 to 314.6 min ) for women, indicating that algorithmderived time in bed overestimated sleep time in both sexes (Figure 3). The proportion of the total measurements in the range of clinically acceptable limits ( $\pm 30$ min difference) was $23.5 \%$. Linear regression analysis also demonstrated the presence of proportional bias between algorithm-derived and diary for both sexes indicating that algorithm-derived time in bed underestimated the diary time in bed, whereas algorithm-derived time in bed overestimated the diary sleep time. Overall, based on the observed magnitude of the regression coefficients, proportional bias was greater in women than men for all variables (Table 4). The sensitivity analysis of day to day Bland-Altman method for comparison between algorithm-derived time in bed with diary sleep time and time in bed also produced similar results with the main analysis of repeated measures of Bland-Altman plots (see Supplementary Table S7 [available online]). In addition, Bland-Altman agreement between algorithm time in bed and diary time in bed and sleep time showed similar results with the main analysis (see Supplementary Figures S2 and S3 [available online]). For instance, Bland-Altman method for comparison between algorithm-derived time in bed and diary time in bed showed a mean bias of $-3.5 \mathrm{~min}(\mathrm{LoA}-139.1$ to 132.1 min ) for men and a mean bias of -15.5 min (LoA -152.7 to 121.8 min ) for women indicating an underestimation of time spent in bed for both men and women (see Supplementary Figure S2 [available online]). Algorithm-derived time in bed also overestimated the diary sleep time in the Bland-Altman plot with a mean bias of $57.4 \mathrm{~min}(\mathrm{LoA}-90.1$ to 204.8 min ) for men and 56.0 min (LoA -96.1 to 208.0 min ) for women (see Supplementary Figure S3 [available online]).

In sensitivity analyses, we separately examined participants with high ( $>4$ day and $>20 \mathrm{hr}$ ) and low ( $<4$ day and $<20 \mathrm{hr}$ ) wear compliance; Bland-Altman plots are shown in Supplementary Figure S4 (available online). We also reported participants' time in bed and sleep time according to valid wear days and valid hours in Supplementary Tables S8 and S9 (available online). According to Bland-Altman plots, algorithm-derived time in bed overestimated the diary sleep time for both in participants who had more
than 4-day activPAL wearing days (a mean bias of 55.3 min , LoA -82.1 to 192.6 min ) and $<4$ day activPAL wearing days (a mean bias of 69.9 min , LoA -169.3 to 309.1 min ).

## Discussion

To our knowledge, this study is the largest population cohort to compare the thigh-worn accelerometer algorithm that estimates time in bed with a sleep diary. The findings suggest that the algorithm estimates acceptable diary time in bed on a group level. However, about $36.9 \%$ of the measurements and about half of the participants were in the range of $\pm 30 \mathrm{~min}$ difference of a clinically relevant limit at individual level. As expected, the correlations with diary estimated sleep time data were lower concluding that the algorithm estimates longer sleep time on a group level compared with diary.

Average absolute differences in time in bed between the two methods were generally small, for example, the algorithm-derived time in bed was 9.8 min less than diary time in bed, which was within the clinically acceptable range of $\leq 30 \mathrm{~min}$ difference. Although Winkler et al. (2016) found a good correlation (Pearson correlation coefficient $=.67$ ) between the algorithm and sleep diary waking times, the algorithm overestimated waking wear time relative to the diary thus resulting in underestimation of diary time in bed. van der Berg et al. (2016) developed another algorithm for the assessment of time in bed from activPAL data, which was based on the number and duration of sedentary periods to identify time in bed, and on the number and duration of active periods (standing or stepping) to identify wake times. They showed that the algorithm estimates of time in bed differed on average by $<25 \mathrm{~min}$ compared with the self-reported bedtimes. Their algorithm was strongly associated with self-reported wake and time in bed (intraclass correlation coefficient $=.79$ ). We also found an acceptable agreement on estimation of algorithm-derived time in bed and diary time in bed on a group level although the LoAs were relatively wide.

The main potential use of a future activPAL algorithm will be to evaluate associations between sleep duration and health outcomes. It is therefore important to evaluate the capacity of the algorithm to produce consistent results. For instance, Biddle et al. (2018) examined the association between physical behaviors (sleep, sitting, standing, and stepping) and markers of metabolic


Figure 3 - (a-c) The repeated measures of Bland-Altman agreement between algorithm and diary for the duration of time in bed and sleep time. Mean of the differences between algorithm time in bed and diary sleep time and lower and upper agreement limits (mean difference $\pm 1.96 S D$ ) are displayed for each Bland-Altman plot. The bold lines represent the upper and lower a priori-set clinically satisfactory limits ( $\pm 30 \mathrm{~min}$ from the zero line).
health including fasting glucose and insulin, 2-hr glucose and insulin. Sleep time was estimated with both the Winkler et al.'s (2016) algorithm and sleep diary. It is encouraging that Biddle et al. (2018) found that the results were materially the same when associations of self-reported sleep time and cardiometabolic outcomes were compared with those of algorithm-derived time in bed. In our recent BCS70 analysis on the associations between different sleep indicators and a range of cardiometabolic outcomes, we found that there was no material difference between the algo-rithm-derived time in bed and diary time in bed or sleep time (Huang, Inan-Eroglu, Hamer, \& Stamatakis, 2020). We found that algorithm-derived time in bed was higher than diary sleep time by approximately 1 hr in both men and women. Further development in algorithms to estimate sleep duration from the thigh-worn accelerometer data is needed. Studies that determine the time in bed and sleep differences between diary and wrist actigraphy produce different results. For instance, while some studies showed that diary overestimated the total sleep time compared with actigraphy (Campanini et al., 2017), other studies showed an underestimation (Liu, Wong, Zwetsloot, Hsu, \& Tsui, 2019). Yet, the conclusion from these studies were that the levels of disagreement are reasonable for the devices to be used interchangeably (Campanini et al., 2017; Liu et al., 2019).

We showed that $23.5 \%$ of the participants were in the clinically acceptable range ( $\pm 30 \mathrm{~min}$ difference) for sleep time. Unlike our study, the wrist-worn accelerometer study showed that $88 \%$ of the participants were in the clinically satisfactory ranges for total sleep time (de Zambotti, Rosas, Colrain, \& Baker, 2019). The reason for these different findings can be attributed to properties of the devices. The thigh-worn accelerometer can detect sitting/lying time, upright time, sitting/lying to upright transitions, and reduction in sitting as well as distinguish standing from stepping (Edwardson et al., 2017). However, the wrist-worn accelerometer measures cannot use postural information when estimating sleep or waking state, habitual physical activity, and energy expenditure (Doherty et al., 2017).

Although wrist actigraphy has excellent concordance with polysomnography in the measurement of sleep time in healthy people (Martin \& Hakim, 2011), wrist actigraphy is prone to overestimating sleep time in different health conditions compared with polysomnography (Blackwell, Ancoli-Israel, Redline, Stone, \& Osteoporotic Fractures in Men (MrOS) Study Group, 2011) and is prone to underestimating sleep time compared with diary (Moore, Schmiege, \& Matthews, 2015). We also found that the health status of participants influenced the comparisons of time in bed and sleep time assessed by the thigh-worn accelerometer and diary. We showed that the differences between algorithm and diary for both time in bed and sleep time were higher in participants with a long-standing health condition compared with those who did not have a long-standing health condition. Theoretically at least, this observation opens up the possibility that either healthy people report sleep time more accurately or the algorithm works better for healthy people. This finding requires further attention in future research.

Our study has several notable strengths, including the large sample size and the population-based sample that increases generalizability of our findings. Another strength was that $63.5 \%$ of participants provided at least 6 valid days of sleep diary and the accelerometer data. Also, it is a strength that our participants were asked for bedtime and wake-up time rather than for the number of hours slept. The latter would entail a calculation by the respondents and thus an increased risk of reporting error of sleeping times.

Our study has limitations also. The sleep diary as a method to measure time in bed and sleep time may be subject to recall limitations or incompleteness. Because of the way participants were instructed to complete the diary (on the following day), we expect that recall bias is less pronounced than recall questionnaires utilizing a specific time frame or inquire about "usual" sleep duration. There is a need for studies that compare the algorithm we used with the gold standard polysomnography. In addition, because we only had the accelerometer data for Winkler et al. (2016)'s algorithm, we could not make any comparison with other algorithms. As we were only able to look at the agreement in total time in bed, we could not test instance-level agreement. Therefore, we were not able to shed light whether the correct portions of the day were identified as in bed. Another limitation is that we had algorithm data for duration of sleep and time in bed, not for the time participants go to bed and the time they wake up.

## Conclusions

In summary, the algorithm we tested showed acceptable estimates of time in bed compared with diary at the group level. As such, the algorithm is appropriate for use in large-scale population studies to estimate time in bed at a group level. However, despite the limited bias between algorithm and diary, the broad $95 \%$ LoAs suggest that there may still be disparities between these measurement modalities at individual participant levels in estimating time in bed and sleep time. This was especially true for sleep time; as the average value for sleep time increased, there appeared to be less agreement between the measurements. The limited research to date suggests that such disagreement has limited impact on estimates of association between sleep and health outcomes. With the increasing use of thigh-worn monitors in the field of physical activity, sedentary behavior and sleep, automated estimation of sleep behavior parameters has several practical advantages and can maximize use of the accelerometer data. More research is required to further refine the different algorithms that estimate sleep duration from the thighworn accelerometer data.

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